

**Analysis of Interactions between Finite-Sized Particles and Terminally
Attached Polymer using Numerical Self-Consistent-Field Theory**

by

BRADLEY MICHAEL STEELS

B.Eng., Royal Military College of Canada, 1995

A THESIS SUBMITTED IN PARTIAL FULFILLMENT OF
THE REQUIREMENTS FOR THE DEGREE OF
MASTERS OF APPLIED SCIENCE

in

THE FACULTY OF GRADUATE STUDIES

Department of Chemical and Bio-Resource Engineering
and
The Biotechnology Laboratory

We accept this thesis as conforming
to the required standard

THE UNIVERSITY OF BRITISH COLUMBIA

December 1997

© Bradley Michael Steels, 1997

In presenting this thesis in partial fulfilment of the requirements for an advanced degree at the University of British Columbia, I agree that the Library shall make it freely available for reference and study. I further agree that permission for extensive copying of this thesis for scholarly purposes may be granted by the head of my department or by his or her representatives. It is understood that copying or publication of this thesis for financial gain shall not be allowed without my written permission.

Department of Chemical and Bioresource Engineering
The University of British Columbia
Vancouver, Canada

Date 14 Jan 1998

ABSTRACT

Non-specific protein adsorption is known to influence many processes. For example, fouling of food processing equipment or fouling of biomedical implants often occurs because of strong protein adsorption. Protein adsorption on these and other surfaces, such as biomaterials, can however be reduced by attaching polymer chains by one end to the surface. Terminally attached polymer chains have also found application in size-based chromatographic separations.

The goal of this thesis is to improve our understanding of the way in which solute molecules interact with terminally attached polymer chains, and to use this knowledge to predict optimum system conditions for minimizing protein adsorption. We develop a numerical self-consistent-field lattice model, based on an earlier model of Scheutjens and Fleer [1979; 1980], to calculate theoretical results for the polymer density distribution of isolated and interacting chains around a solute particle positioned at a fixed distance from a surface. In addition, the excess energy required to move the particle into the polymer chains (interaction energy) is calculated using a statistical mechanical treatment of the lattice model. The effect of system variables such as particle size, chain length, surface density and interaction parameters on density distributions and interaction energies is also studied.

The model is first applied to the compression of a single polymer chain by a disc of finite radius. Results are compared to predictions of a previous scaling thermodynamic model by Subramanian *et al.* [1995]. We see no first order partial-escape transition as reported by Subramanian *et al.* Instead, we find that the energy required to compress the chain increases monotonically, becoming independent of chain length at very close compression.

Calculations for the interaction of a solute particle with a surface covered by many polymer chains (a brush) shows that the polymer segments will fill in behind the particle quite rapidly as it moves toward the surface. When there is no strong energetic attraction between the polymer and solute we predict that the interaction energy will be purely repulsive upon compression due to losses in conformational entropy of the polymer chains. Above a critical chain length, which depends upon particle size, a maximum in the force required to move the particle toward the surface is observed due to an engulfment of the particle as chains attempt to access the free volume behind the particle.

If an attraction exists between the polymer and solute, such that a minimum in the interaction energy is seen, the optimum conditions for solute repulsion occur at the highest surface density attainable. Long chain length can lead to increased solute concentration within the polymer layer due to the fact that more favourable polymer-solute contacts are able to occur than with short chains at a similar entropic penalty.

Table of Contents

ABSTRACT	II
TABLE OF CONTENTS.....	IV
TABLE OF FIGURES	VI
LIST OF TABLES	XI
ACKNOWLEDGEMENTS.....	XII
1 INTRODUCTION.....	1
1.1 Overview	1
1.2 Non-Specific Protein-Surface Interactions.....	4
1.3 Thesis Objective.....	6
1.4 Terminally Attached Polymers at Interfaces	7
1.4.1 Distributions of Terminally Attached Chains.....	10
1.4.1.1 Experimental Measurements and Scaling Predictions.....	10
1.4.1.2 Advanced Brush Models	16
1.4.1.3 Brushes with Free Polymer in Solution.....	19
1.4.1.4 Brush Distributions – Summary.....	20
1.4.2 Compression of Terminally Attached Polymers.....	22
1.4.3 Particle Interactions with Terminally Attached Polymers.....	28
1.4.3.1 Experimental Studies	28
1.4.3.2 Modeling of Brush-Particle Interactions	30
2 MODEL OUTLINE.....	33
2.1 Origins of Nonideal Mixing in Liquid Solutions.....	33
2.1.1 Entropy of Mixing Polymer in Solvent.....	34
2.1.2 Enthalpy and Gibbs Energy of Mixing	36
2.2 Self-Consistent Mean-Field Theory of Scheutjens and Fleer.....	38
2.2.1 Cylindrical Lattice Geometry	41
2.2.2 Combinatorial Entropy.....	43
2.2.3 Internal Energy	45
2.2.4 Equilibrium Segment Density Distribution.....	46

2.2.5	Chain Grafting.....	48
2.2.6	Interaction Energy	51
2.2.7	Numerical Solution.....	52
2.3	Evaluation of Model Parameters.....	57
2.3.1	Scaling the Lattice Model	57
2.3.1.1	Lattice Unit and Chain Length.....	58
2.3.1.2	Polymer Surface Concentration	61
2.3.1.3	Particle Size.....	62
2.3.2	Measuring Interaction Parameters	64
2.3.2.1	Differential-Vapour-Pressure and Osmometry	65
2.3.2.2	Low-Angle Laser-Light-Scattering (LALLS).....	66
3	ISOLATED TERMINALLY-ATTACHED CHAINS.....	71
3.1	Motivation.....	71
3.2	Scaling Theory of Mushroom Compression	72
3.3	Analysis of Mushroom Compression using Numerical SCF Theory	73
3.4	Summary.....	83
4	BRUSHES AND BRUSH-PARTICLE INTERACTIONS	84
4.1	Outline of Calculations	84
4.2	Brush Density Distributions	85
4.3	Brush-Particle Interactions	89
4.3.1	2D Brush Density Distributions	89
4.3.2	Brush-Particle Interaction Energy.....	94
4.3.3	Surface Mobile Brushes.....	101
4.3.4	Brush-Particle Attraction	104
	NOMENCLATURE.....	113
	REFERENCES.....	117
	APPENDIX A	127

Table of Figures

Figure 1.1 Several possible polymer density profiles are shown for terminally attached polymer chains. (a) The Alexander-de Gennes brush assumes a step profile. (b) Analytical SCF theory predicts a parabolic brush. (c) Real terminally attached polymer will exhibit a maximum slightly away from the surface, which advanced numerical models also predict. (d) A strongly adsorbing surface can lead to a pancake structure.....	14
Figure 2.1: Comparison between ideal entropy of mixing and combinatorial entropy of mixing given by Flory-Huggins theory for a polymer chain of 1000 segments.....	36
Figure 2.2: Cartesian (a) and cylindrical (b) lattice geometries used in the self-consistent-field model. Areas treated with mean-field averaging are shown in grey as well as the grafting surface in (b).	39
Figure 2.3: The probability that segment s ends in radial (r,z) is found by combining the probability of two shorter chains ending in that radial. This involves combining two step-weighted walks, one for $1,2,...s$ segments and one for $N,N-1,...s$	49
Figure 2.4: Non-linear curve fit of data taken from Tyn and Gusek [1990] for use scaling particle size to protein molecular weight.....	64
Figure 3.1 Schematic diagram of a single end-grafted chain in (a) uncompressed (b) compressed, and (c) escaped states. The chain grafting point indicated by ● is at lattice position $(z=0,r=0)$. Characteristic dimensions include: (i) disc position, Z_{disc} , (ii) disc radius, R_{disc} (iii) r.m.s. radius of segments from cylinder axis, R_{rms} and, (iv) Flory radius, R_F .	
71	
Figure 3.2 Fractional segment distribution of a single end-grafted chain in the radial (r) (dash-dot line) and normal (z) (solid line) directions with $N=100$ segments. Dashed line shows the root mean squared (rms) distance of segments from the center axis, R_{rms} , and dotted line shows the Flory radius, R_F	75

Figure 3.3 Segment density distribution of a single end-grafted chain with $N=100$. The chain is shown in (a) with no disc and in (b) with a disc of radius, $R_{\text{disc}}=20$, sitting in layer 2 compressing the mushroom.	76
Figure 3.4 Root mean squared distance of segments from the center of the cylinder, R_{rms} , is shown as the disc compresses a mushroom with $N=100$. $R_{\text{disc}}=20$ (solid), $R_{\text{disc}}=30$ (dashed)	77
Figure 3.5 Fractional segment distribution in the radial direction as a mushroom with $N=75$ is compressed by a disc with $R_{\text{disc}}=20$. The curves represent the disc in positions of $z=16, 8, 5, 4, 3$, and 2	78
Figure 3.6 Root mean squared distance of segments from the center of the cylinder, R_{rms} , is shown as the disc of $R_{\text{disc}}=20$ compresses a mushroom with $N=75$	79
Figure 3.7 Energy required to compress a mushroom with a disc of radius, $R_{\text{disc}}=20$, for several chain lengths: $N=20$ (dashed), $N=50$ (dotted), $N=100$ (dot-dash), $N=200$ (solid).	80
Figure 3.8 Fraction of segments covered (dotted) and escaped (solid) from under a stationary disc of radius 20, extending from $z=3$ to the end of the cylinder (Z_{max}), as chain length is varied.	81
Figure 3.9 Chemical potential of a single end-grafted chain under a stationary disc of radius 20, that extends from $z=3$ to the end of the cylinder (Z_{max}), as a function of the number of grafted chains.	82
Figure 3.10 The change in chemical potential with respect to the number of grafted chains (at $n_{\text{chain}} = 1$) as a function of chain length. This value always remains positive indicating stability against phase separation.	82
Figure 4.1 Schematic diagram showing a solute molecule interacting with polymer chains end-grafted to a surface. The centerline represents the axis of a cylindrical coordinate system, and the rings on the surface represent spatial increments in the radial direction.	84

Figure 4.2 Brush density distributions for various polymer-solvent interaction parameters. $N = 50$ segments, $\sigma = 5\%$, $\chi_{os} = \chi_{bs} = 0$.	85
Figure 4.3 Brush density profiles for various polymer-surface interactions are shown. $N = 50$ segments, $\sigma = 5\%$, $\chi_{os} = \chi_{bo} = 0$.	87
Figure 4.4 Segment density profiles for brushes of different lengths. Surface density is 10% and the polymer-solvent interaction parameter χ_{bo} is 0.5. All other interactions are athermal.	88
Figure 4.5 Brush density profiles for various surface densities. Chain length is 100 segments and $\chi_{bo} = 0.5$.	88
Figure 4.6 Polymer segment density distributions in the cylindrical lattice are indexed in both the z and r directions. The chains of length $N=50$ with a grafting density of $\sigma=0.1$ are interacting with a particle of dimensions $R_p=3$ and $L_p=3$ (3 by 3). Interaction parameters are set as $\chi_{bo}=0.4$ and $\chi_{po}=0.4$ (unspecified interaction parameters are always zero). The density distribution is shown for a particle position (a) outside the brush, (b) at layer $z_p = 10$, (c) $z_p = 7$, and (d) $z_p = 5$.	90
Figure 4.7 The 2-dimensional segment density distributions for four different chain lengths are shown around a 3 by 3 particle placed with the leading edge at $z_p = 5$. Interaction parameters are specified as $\chi_{bo}=0.4$ and $\chi_{po}=0.4$. Chain lengths are (a) $N = 15$, (b) $N = 25$, (c) $N = 40$ and (d) $N = 60$ segments.	92
Figure 4.8 The brush distribution of $N=50$ segment chains is shown around a 5 by 5 particle at four different grafting densities. Interaction parameters are $\chi_{bo}=0.4$ and $\chi_{po}=0.4$. Grafting densities are (a) $\sigma=0.05$, (b) $\sigma=0.1$, (c) $\sigma=0.2$ and (d) $\sigma=0.3$.	93
Figure 4.9 Brush-particle interaction energy curves are shown for chains of $N=50$ with a graft density of $\sigma=0.1$ interacting with various sized particles. Interaction parameters are specified as $\chi_{bo}=0.4$ and $\chi_{po}=0.4$. Particle size has been varied from $R_p=1$, $L_p=1$ up to $R_p=7$, $L_p=7$. The dashed line shows the inflection point of each curve that shows one.	94

- Figure 4.10 Interaction energy curves are shown for a particle of $R_p=3$, $L_p=3$ interacting with different length polymer chains of constant grafting density $\sigma = 0.1$. Interaction parameters are $\chi_{bo}=0.4$ and $\chi_{po}=0.4$. The dashed line shows the inflection point of each curve.....95
- Figure 4.11 The critical chain length $N_{critical}$ for which an inflection point is observed is shown as a function of R_p for the system with $\sigma = 0.1$, the previous interaction parameters, and particles with a cylindrical geometry where $L_p = R_p$96
- Figure 4.12 F and the rate of segment displacement from the total volume the particle moves through are shown as a function of z_p for a 3 by 3 particle moving into a brush with $N = 50$ and $\sigma = 0.1$98
- Figure 4.13 F_{max} is shown as a function of particle size for a brush with $N = 50$ and a 10% graft density. The maximum force appears to scale closely with particle volume.....100
- Figure 4.14 Interaction energy curves are shown for a particle of $R_p=3$, $L_p=3$ interacting with 50 segment polymer chains of varied grafting density. Interaction parameters are $\chi_{bo}=0.4$ and $\chi_{po}=0.4$. The dashed line shows the inflection point of each curve.....101
- Figure 4.15 Brush distribution around a 3 by 3 particle is shown for surface non-mobile and mobile brushes. Brushes consist of $N=40$ segment chains at 10% surface density and interaction parameters used were $\chi_{bo}=0.4$ and $\chi_{po}=0.4$. The distributions for non-mobile chains around a particle in (a) layer $z_p = 4$ and (b) $z_p = 2$ are shown; distributions of mobile chains around a particle in (c) $z_p = 4$ and (d) $z_p = 2$ are also shown.....102
- Figure 4.16 Interaction energy curves are shown for a 3 by 3 particle interacting with 40 segment polymer chains that are surface mobile (dashed) and non-mobile (solid). Interaction parameters are $\chi_{bo}=0.4$ and $\chi_{po}=0.4$103
- Figure 4.17 Brush-particle interaction energy curves are shown for five different sized particles interacting with chains of length $N=50$ and grafting density $\sigma=0.1$. Interaction parameters are $\chi_{bo}=0.5$, $\chi_{po}=0.5$ and $\chi_{bp} = -0.5$105

Figure 4.18 Brush-particle interaction energy curves are shown for a 5 by 5 particle penetrating chains of length $N=50$ at four different grafting densities. Interaction parameters are $\chi_{bo}=0.5$, $\chi_{po}=0.5$ and $\chi_{bp}=-0.5$ 106

Figure 4.19 Brush-particle interaction energy curves are shown for a 3 by 3 particle penetrating brushes of varied chain length, each at 10% grafting density. Interaction parameters are $\chi_{bo}=0.5$, $\chi_{po}=0.5$ and $\chi_{bp}=-0.5$ 108

Figure 4.20 Layer partition coefficient $K_p(z_p)$ for various particle sizes interacting with 50 segment chains at 10% surface density. Interaction parameters are $\chi_{bo}=0.5$, $\chi_{po}=0.5$ and $\chi_{bp}=-0.5$. 110

List of Tables

Table 1.1	Several polymers with their monomers and repeat units.	8
Table 1.2	Schematic of different copolymer structures.....	8
Table 2.1:	Experimental properties that require direct comparison with lattice values.	58
Table 2.2:	Polymer-solvent interaction parameters for PEG and Dextran in water at 25 °C calculated from light-scattering data of Haynes et al. [1993].	69
Table 2.3:	Protein-solvent interaction parameters calculated from light-scattering data for bovine serum albumin (BSA) in water at 25 °C.....	69
Table 2.4:	Protein-solvent interaction parameters calculated from light-scattering data for lysozyme in water at 25 °C.	69
Table 2.5:	Protein-solvent interaction parameters calculated from light-scattering data for α - chymotrypsin in water at 25 °C.....	70
Table 2.6:	Protein-polymer interaction parameters χ_{23} calculated from light-scattering data in potassium phosphate buffer at 25 °C.	70

Acknowledgements

Above all, I would like to thank my thesis supervisor Dr. Charles Haynes, for offering me this very interesting project. His enthusiasm and expertise have made this work possible.

I am very grateful to Dr. Don Brooks and Dr. Bruce Bowen, whose courses in biophysical chemistry and numerical programming methods provided me a framework upon which this work was built. I would also like to thank Dr. Frans Leermakers for his expert help with the modeling and I am indebted to Jurgen Koska for his help with computer code and math.

I must also thank all of the people that I have had the pleasure of knowing and working with in the Biotechnology Laboratory at UBC, especially those in the Bioprocess Engineering Group. This very outgoing group of people has been inspirational and supportive. I am thankful for the many wonderful friendships I have made during this work.

I am also very grateful to NSERC and the Canadian Forces, whose support made this work possible.

1 Introduction

1.1 Overview

Properties of a solution at an interface are different from those in bulk solution. This is especially true for solutions containing globular proteins, since the solubility and solution structure of proteins is determined by a delicate balance of intermolecular and intramolecular interactions. Introduction of an interface can disrupt this balance of forces, leading to adsorption and the possibility of a change in protein conformation. Protein adsorption is a complex process, which remains only partially understood [Haynes and Norde, 1994; Andrade, 1986]. Increasing our knowledge of protein-surface interactions is motivated by a desire to understand how these interactions may be controlled. Therapeutically effective contact of foreign surfaces with the human biosystem usually requires careful design of the sorbent properties. In some applications, it may be desirable for proteins to interact strongly with a surface, while in others adsorption must be moderate and controllable.

Often, when a material is engineered for use in a biological system, protein adsorption is undesirable. When a foreign material contacts blood, plasma proteins such as serum albumin and fibrinogen form an adsorbed layer through a process called opsonization. It has been shown that nonspecific adsorption of proteins can lead to structural changes in the protein molecules [Haynes and Norde, 1994]. It is believed that these changes in conformation of serum proteins then trigger proteolytic cascades or activate platelet receptors, which leads to thrombus formation [Elbert and Hubbel, 1996; Bamford and Al-Lamee, 1992]. This has practical implications in design of all biomaterials, such as dialysis tubing, vascular grafts or artificial heart valves, since thrombus formation can lead to occlusion or embolus formation.

Protein adsorption in biosystems also has implications in site-directed drug delivery or gene therapy [Davis, 1997]. Adsorption of plasma proteins on the surface of a foreign material may lead to targeting of the material by the immune system, or more specifically by the mononuclear phagocytic system (MPS) [Woodle and Lasic, 1992]. Drug delivery vessels, such as liposomes or polymer microspheres, may be rapidly cleared from circulation without having time to reach the desired target within the host. This is especially significant in cases where a therapeutic is designed for second or third-order targeting, where it must reach a specific cell type or specific location within a cell, respectively.

Unwanted protein adsorption is also observed in more general situations. Plaque formation on teeth and fouling of surfaces such as contact lenses, food processing equipment and naval equipment results from strong protein-surface interactions. The nonspecific adsorption of protein can also interfere with results in high-sensitivity bioassays in which fluids contact glass or polymeric surfaces [Malmsten and Van Alstine, 1996].

In some cases, protein adsorption can be a desired event. Because of their amphiphilic nature, proteins may be used as surfactant-like molecules to stabilize creams or emulsions at a liquid-liquid interface. Separation or purification of proteins may also be carried out using controlled protein-surface interactions. Hydrophobic interaction chromatography (HIC) makes use of hydrophobic interactions between protein surfaces and a solid support matrix. Under the correct solution conditions it is possible to adsorb target proteins preferentially from a mixture and then elute them under different solution conditions (*i.e.* lower salt concentration). Similarly, ion exchange chromatography makes use of electrostatic interactions between proteins and the support matrix. Protein purification processes are very important since therapeutic proteins are

often produced in biological fermentations, where the product concentration is typically quite low and the number and levels of impurities relatively high.

A common step in protein purification is precipitation, which may be initiated by addition of water-soluble polymer to a protein-containing solution. Polyethylene glycol (PEG), dextran and polyvinyl alcohol (PVA) are often used as precipitating agents because they do not interact strongly with most proteins and are approved for biological applications by the FDA. The weak interaction of these water-soluble polymers with globular proteins has motivated their application in surface modifications for improved biocompatibility. Attaching PEG or dextran to synthetic surfaces has been shown to reduce significantly the adsorption of proteins and the adhesion of platelets and cells [Schroën *et al.*, 1995; Llanos and Sefton, 1993; Merrill, 1992; Bergström *et al.*, 1992; Gombotz *et al.*, 1992; Desai and Hubbel, 1991]. Presentation of PEG on the surfaces of polystyrene microspheres or liposomes has also been shown to reduce clearance of the particles from circulation [Dunn *et al.*, 1994; Woodle and Lasic, 1992]. In both cases, the susceptibility of a surface to protein fouling can be controlled by the introduction of a water-soluble polymer to the interface.

A new generation of size-exclusion chromatography, which we call entropic interaction chromatography, is based on end-grafting of water-soluble polymer chains to a solid matrix. Traditional size exclusion chromatography makes use of macroporous particles into whose pores some solute molecules may diffuse while others are excluded. Thus, the effective column volume is smaller for large molecules and they elute more quickly. A similar size-based separation is achieved in entropic interaction chromatography [Brooks and Müller, 1996]. In this case, smaller solute molecules sample a larger column volume as a result of lower steric repulsion by the polymer chains.

1.2 Non-Specific Protein-Surface Interactions

Protein molecules are copolymers made up of defined sequences of the 21 basic L-amino acids. The specific linear sequence of amino acids defines a protein's primary structure. Amino acid side-chains have various sizes, shapes and chemical properties. Some side-chains are acidic and some basic, meaning a protein molecule may vary in charge with changing solution pH. Some amino acid side-chains are relatively hydrophobic and therefore prefer to be positioned so that contact with water is minimized (*i.e.* within the core of protein). Thus, the primary structure defines a protein's secondary and tertiary structures.

Secondary structure involves the formation of α -helices and β -sheets within a protein, which result from regularly repeating hydrogen-bonding groups in the polypeptide backbone. Association between elements of secondary structure leads to formation of structural domains within the molecule. A three-dimensional tertiary structure then results from association between structural domains, and is stabilized by a complex set of interactions involving hydrophobic forces, electrostatic forces, dispersion forces, and hydrogen bonds [Zubay, 1993]. Tertiary structure is well defined in fibrous proteins (structural proteins) and globular proteins (enzymes, transport proteins). Folding of proteins into these well-ordered structures is entropically unfavourable, and the process occurs spontaneously because of favourable enthalpic interactions. The Gibbs energy of denaturation $\Delta_{N-D}G$ for single domain proteins falls in the range 20-100 kJ/mol, which corresponds roughly to that of 1-8 hydrogen bonds, indicating that the native folded conformation of a protein is only marginally stable [Haynes and Norde, 1994; Privalov, 1979].

Several major driving forces for non-specific protein adsorption have now been identified. Transmission circular dichroism, nuclear magnetic resonance, and microcalorimetry

have shown that a significant proportion of a protein's ordered secondary structure can be lost upon adsorption to a surface [Haynes and Norde, 1994]. This suggests that a gain of conformational entropy helps drive the adsorption process.

Dehydration of sorbent or protein surfaces has also been shown to influence protein adsorption at a surface [Haynes and Norde, 1994]. Differential scanning microcalorimetry has shown that the total heat capacity C_p of a system often decreases sharply when protein is adsorbed to hydrophobic surfaces. This decrease in heat capacity is consistent with the release of water molecules involved in solvating the surface, a signature of the hydrophobic effect. More hydrophobic proteins therefore show higher maximum adsorption values and less tendency to desorb upon dilution. Electrostatic interactions and redistribution of charge in the interfacial layer also contribute to protein adsorption.

Based on these driving forces for protein-surface interactions, neutral, flexible polymer chains attached by one end at the surface should provide resistance to non-specific adsorption. The protective polymer layers are prepared such that long flexible chains extend away from the surface into solution, forming a soft hydrophilic barrier. The hydrophilic nature of the chains can act to reduce any hydrophobic driving force. Also, solute molecules that move into volume that the polymer chains can occupy (excluded volume) decrease the polymer conformational entropy, which is energetically unfavourable. This entropic effect may help to compensate for any gain of protein conformational entropy that adsorption would provide the system. Indeed, it is accepted but not proven in the literature that some combination of these two effects is what leads to reduced protein adsorption on grafted polymer surfaces [Schroën *et al.*, 1995; Gölander *et al.*, 1992; Gombotz *et al.*, 1992; Andrade, 1986].

Indirect studies indicate that entropic repulsion may be the more dominant effect. Schroën *et al.* [1995] studied lipase adsorption on surfaces covered with adsorbed Pluronic block copolymer ($\text{PEO}_m\text{-PPO}_n\text{-PEO}_m$; PEO = polyethylene oxide, PPO = polypropylene oxide). When adsorbed to hydrophobic surfaces by the PPO block, the Pluronic formed a highly extended surface layer of PEO tails, and lipase adsorption was reduced to undetectable levels. If the copolymer was adsorbed onto a hydrophilic surface, the PEO tails collapsed onto the surface. Although the amount of copolymer adsorbed still provided a very hydrophilic surface, lipase adsorption was not reduced as significantly.

1.3 Thesis Objective

Significant experimental data are now available describing solute interactions with terminally attached polymer chains. Most of this work has focused on trial-based correlation of materials and synthesis methods with protein adsorption or cell adhesion experiments [Merril, 1992; Gölander *et al.*, 1992; Gombotz *et al.*, 1992; Desai and Hubbel, 1991, Bergström *et al.*, 1992]. Often, however, incomplete characterization of the experimental system leads to ambiguous or incomplete conclusions. It would be very useful to understand these systems well enough to predict *a priori* how a solute molecule will interact with a particular terminally attached polymer brush. This involves (i) defining how the polymer will change its equilibrium distribution when a solute particle is interacting with it as well as (ii) understanding the energetics accompanying the changes in polymer distribution and changes in contact between different components of the system.

The goal of this work is therefore to develop a general model to study the interaction of a solute particle with polymer that is terminally attached at an interface. The first objective is to calculate the polymer density distribution in the presence of a particle whose position may be

varied. In this way we hope to gain a better understanding of how the polymer will redistribute itself as the particle penetrates toward the surface. The second objective involves calculation of the interaction energy between the polymer and the particle in order to understand better how the polymer repels a particle. The effect of varying polymer chain length and surface density on the polymer distribution and interaction energy will be investigated. Also the effect of varying particle size and interaction parameters between system components will be investigated.

It is hoped that the model will help us to understand how a surface might be protected most effectively from protein adsorption using terminally attached polymer. Also, the effects of system properties on polymer-particle interactions are of interest for other applications such as separations using end-grafted polymer surfaces.

1.4 Terminally Attached Polymers at Interfaces

A polymer is a large molecule composed of a number of small, chemically simple subunits. The subunits from which the polymer is formed are called monomers and they define the type of polymer (see Table 1.1). Polymer molecules are often linear sequences of repeat units (*e.g.* polyethylene), but may also be branched chains and even cross-linked networks of chains forming very large molecules. The degree of polymerization N is defined as the number of repeat units forming a given polymer, and hence the molecular weight of the molecule M is equal to its degree of polymerization multiplied by the repeat unit molecular weight.

If all repeat units are identical, a polymer is called a homopolymer; copolymers on the other hand contain a mixture of different monomers. The different types of copolymer include random, alternating, block, and graft copolymers (see Table 1.2). For example, if one monomer type forms a linear chain, while a second monomer type is coupled to an active site along that

chain (other than the ends), a graft copolymer is formed. Both block and graft copolymers are often used to modify interfacial properties for reducing protein adsorption.

Table 1.1 Several polymers with their monomers and repeat units.

Polymer	Monomer	Repeat Unit
polyethylene	$\text{CH}_2=\text{CH}_2$	$-(\text{CH}_2\text{CH}_2)_N-$
polyvinyl chloride	$\text{CH}_2=\text{CHCl}$	$-(\text{CH}_2\text{CHCl})_N-$
polyethylene glycol	$\text{HOCH}_2\text{CH}_2\text{CH}_2\text{OH}$	$-(\text{CH}_2\text{CH}_2\text{O})_N-$
polyvinyl alcohol	$\text{CH}_2=\text{CHOH}$	$-(\text{CH}_2\text{CHOH})_N-$

Table 1.2 Schematic of different copolymer structures.

<p>(a) Random Copolymer</p> <p>-AAABABBABAABBB-</p>	<p>(c) Block Copolymer</p> <p>-AAAABBBBAAAA-</p>
<p>(b) Alternating Copolymer</p> <p>-ABABABABABABAB-</p>	<p>(d) Graft Copolymer</p> <p>-AAAAAAAAA-</p> <p style="text-align: center;">↓</p> <p style="text-align: center;">-BBB-</p>

When linear polymer molecules are placed in solution they may adopt a great number of conformations whose average is that of a random coil. Although the bond angles between atoms forming the backbone are fixed (*e.g.*, 109.5° for C-C), the energy barrier associated with rotation

about those bonds is often on the same order of magnitude as the thermal energy of the solution. As a result, the path from one end of a long polymer molecule to the other changes over time. Thus, describing geometric properties of polymer molecules in solution requires a statistical analysis. For example, the average path and path length of a chain can be determined using a statistical-mechanics formalism known as the random walk [Kuhn, 1934]. In this manner, the average distance between ends of a polymer molecule can be calculated by considering the chain as a sequence of N randomly oriented bonds each of length l . The well known result is [Flory, 1953]:

$$\langle R^2 \rangle = l^2 N \quad (1.1)$$

From this result, the radius of gyration $\langle R_g^2 \rangle$ of a random coil chain is given by

$$\langle R_g^2 \rangle = \frac{1}{6} l^2 N \quad (1.2)$$

which is defined as the root mean squared distance of monomers from the center of mass.

It has also been noted that a polymer chain will form a somewhat more expanded coil in a very good solvent. de Gennes (1979, 1980) proved that the coil radius in this case may be given by

$$R_g \approx l N^{3/5} \quad (1.3)$$

where numerical constants of order unity are ignored. The central result here is that $R_g \propto N^a$ where a lies in the range from $1/2$ in a theta (poor) solvent to $3/5$ in a good solvent.

Polymer chains are not completely flexible however, due to the fixed bond angles and steric interactions between side groups. Flory was the first to account for this by multiplying the

random walk result (Equation (1.2)) by a stiffness parameter C_∞ , which is determined experimentally. A parameter known as the persistence p may also be used to account for chain stiffness and it is equivalent to $C_\infty/6$. Finally, rescaling of N and l can be used to account for chain stiffness [Kuhn, 1934]. For example, if a statistical segment length l_K (Kuhn length) is chosen such that $l_K = bl$ and the number of segments is chosen as $N_K = N/c$, the average chain dimension becomes $\langle R^2 \rangle = l_K^2 N_K = (b^2/c)l^2 N$. The chain stiffness will be properly accounted for as long as b and c are chosen such that $(b^2/c) = C_\infty = 6p$ [Fleer *et al.*, 1993]. In the following discussion the chain persistence is ignored for simplicity, but can be reintroduced in a straightforward manner without loss of generality.

1.4.1 Distributions of Terminally Attached Chains

1.4.1.1 Experimental Measurements and Scaling Predictions

Graft copolymer synthesis is the most common method used to terminally attach polymer at an interface. For example, polystyrene microspheres onto which PEG chains are grafted are commercially available for various applications including oligopeptide synthesis and chromatography [Bayer and Rapp, 1992]. Polymer chains may also be immobilized at a surface by block copolymer adsorption [Van Alstine and Malmsten, 1997; Kent *et al.*, 1995; Schroën *et al.*, 1995]. If one block of a copolymer has a very strong affinity for the surface it will adsorb preferentially leaving the other block freely extended into solution. In this situation, it is possible for adsorbing molecules to laterally displace molecules already at the interface, giving rise to a surface-mobile adsorbed layer (especially when adsorbed at a liquid-liquid interface). A third technique for preparing surfaces with terminally attached chains involves self-assembly of

monolayers or bilayers using polymer-derivatized lipids [Du *et al.*, 1997; Woodle and Lasic, 1992].

Restriction of one end of a polymer molecule to an interface leads to very distinct chain configurations and energetics. The degree of surface coverage σ (chains/unit area), or distance d between grafting points ($d \approx \sigma^{-1/2}$), in large part determines the grafted chain conformation. A crude picture of chain conformation can therefore be obtained by calculating the reduced surface coverage $\sigma^* = \pi \langle R_g^2 \rangle / \Sigma$, which is approximately the ratio of an undisturbed chain's cross-sectional area to the average surface area per grafted chain, where $\Sigma = 1/\sigma$ (area per chain) [Baranowski and Whitmore, 1995]. If the grafting points are farther apart than the chain radius of gyration, a random coil configuration, commonly termed a "mushroom", is adopted by the chains. In the mushroom regime the reduced surface coverage is less than unity and the thickness of the polymer layer h is independent of surface coverage and will increase with N^ν , where $\nu = 0.5$ to 0.6 in a poor to good solvent respectively (corresponding to Equations (1.2) and (1.3)). Within the mushroom regime, grafted-chain conformations are extremely sensitive to enthalpic interactions, commonly expressed in terms of a binary Flory interaction parameter χ_{ij} . For example, if a favourable energetic interaction exists between chain segments and the surface, coil collapse can occur forming a pancake structure on the surface (see Figure 1.1 (d)) [Fleer *et al.*, 1993].

In regimes of surface coverage where $\sigma^* > 1$, chain overlap occurs and the chains extend away from the surface due to excluded volume interactions with one another. A polymer layer under these conditions is often termed a "brush" due to the physical picture of partially ordered, stretched, linear molecules extending from a surface. This regime was first described by

Alexander [1977] and de Gennes [1976], who predicted that the polymer configuration minimizing entropically unfavourable chain stretching and excluded volume interactions between chains would result in an equilibrium brush with height h . The equilibrium brush height was found by minimizing an approximate expression for the brush energy derived either using polymer scaling theory [Alexander, 1977] or global energy balance arguments [Fleer *et al.*, 1993]:

$$\Delta A \approx kT \left[\frac{3h^2}{2Nl^2} + \nu N \left(\frac{N\sigma l^3}{h} \right) \right] \quad (1.4)$$

Here, the first term in square brackets represents the energetic cost to stretch a polymer from a Gaussian coil having entropy of $3k/2$ per segment or $N3k/2$ per chain, where k is Boltzmann's constant. The stretching energy is proportional to distance squared (*i.e.* Hookian), and the ratio $h^2 / (Nl)^2$ gives the fraction of total chain conformational entropy lost due to stretching, where all entropy is lost at the fully stretched length of Nl [Fleer *et al.*, 1993]. The second term represents the excluded volume interaction energy between polymer segments, where ν represents an excluded volume parameter (equal to $1-2\chi_{12}$: see Section 2.1) and $N\sigma l^3 / h$ is equivalent to the average volume fraction Φ of polymer in the brush.

Ignoring numerical constants of order unity, the equilibrium ($\Delta A = 0$) height is therefore given by [Milner, 1991]

$$h \approx Nl(\nu\sigma l^2)^{1/3} \quad (1.5)$$

which indicates that the brush height scales linearly with N . As suggested by Equation (1.2) the unstretched chain dimension R_g therefore scales with $N^{1/2}$. Equation (1.5) also suggests that brush height increases with $\sigma^{1/3}$, so that the maximum volume fraction increases with $\sigma^{2/3}$.

However, two major assumptions of this model are that (i) all free chain ends lie on the plane at the outer edge of the brush and (ii) the volume fraction of polymer in the brush assumes a constant density step profile (Figure 1.1 (a)). Both assumptions are at best approximate. Thus, the energy expression overestimates both the stretching cost and the excluded volume energy, but cancellation of errors results in the physics of the system being described reasonably well [Milner, 1991].

Following these early model results, experimental brush density distributions have been measured using small angle neutron scattering (SANS) and neutron reflectivity to provide a much clearer picture of chain conformations. Cosgrove *et al.* [1987b] measured the density profiles of PEO grafted on nonadsorbing, deuterated polystyrene using SANS. The polymer density profile exhibited a clear maximum several nanometers from the surface and then decreased slowly (parabolically) away from the surface. At the outer edge of the brush, the polymer volume fraction was seen to decrease very slowly giving rise to a long tail region (Figure 1.1 (c)). Density profiles for PS-PEO adsorbed from d-toluene onto quartz measured by Field *et al.* [1992] using neutron reflectometry were also of the form shown in Figure 1.1 (c). Similar profiles were measured by Cosgrove *et al.* [1991] using neutron reflectivity, for polystyrene-poly(2-vinylpyridine) (PS-P2VP) block copolymer adsorbed onto mica from toluene. In this solvent, the PS forms a highly extended layer, while the P2VP remains strongly adsorbed. Auroy *et al.* [1991a, 1991b] studied the structure of end-grafted polydimethyl siloxane (PDMS) on silica using SANS and found that in a poor solvent the polymer layer was collapsed and gave good agreement with the step-profile model. However, in a good solvent the layer was highly extended such that the volume fraction $\Phi(z)$ decreased very slowly at high z . Auroy *et*

al. [1991a] did not see a depletion layer next to the grafting surface but they suggest that there may be an attractive interaction between the PDMS polymer and the surface (Figure 1.1 (d)).

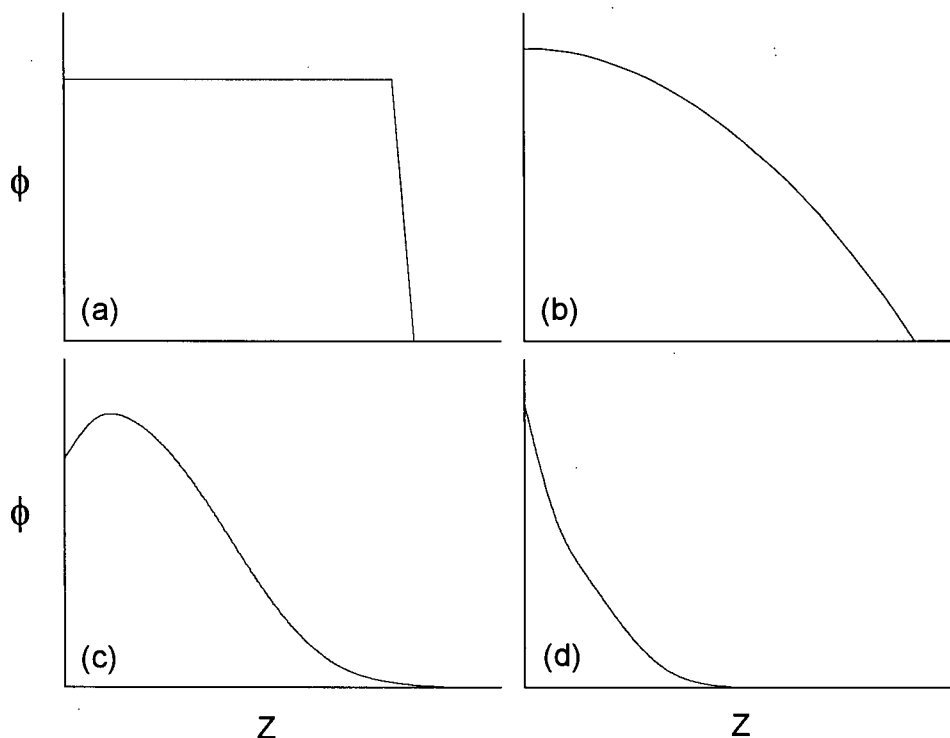


Figure 1.1 Several possible polymer density profiles are shown for terminally attached polymer chains. (a) The Alexander-de Gennes brush assumes a step profile. (b) Analytical SCF theory predicts a parabolic brush. (c) Real terminally attached polymer will exhibit a maximum slightly away from the surface, which advanced numerical models also predict. (d) A strongly adsorbing surface can lead to a pancake structure.

Cosgrove and Ryan [1990b] successfully measured the density profile of end-adsorbed methacrylate-terminated polyethylene glycol methyl ethers ($M_n=5000$ g/mol) on polystyrene microparticles using SANS. They found that the density of polymer was a maximum at the surface and decayed rapidly away from the surface. This was attributed to low surface coverages ($1-4$ mg/m²), and the fact that the surface was strongly charged and an adsorbing surface for the PEG chains. Cosgrove [1990a] also presents data for PS grafted to silica in which there are

different polymer-surface interactions. Here the polymer-surface interaction was characterized by a dimensionless adsorption energy $\chi_s = (u_1^a - u_2^a)/kT$ that represents the difference between the energy of a solvent-surface contact u_1^a and a polymer segment-surface contact u_2^a [Silberberg, 1968]. For high χ_s the segment density was found to be a rapidly decaying function away from the surface (Figure 1.1 (d)); for low χ_s a parabolic-type profile was seen with a depletion region next to the surface (Figure 1.1 (c)). At very high brush densities, however, segment adsorption can result in no depletion layer being observed [Auroy *et al.*, 1991a].

Kent *et al.* [1992; 1995] carried out experiments in which the chain length and surface density of a brush were varied independently over a large range. Langmuir monolayers of polydimethylsiloxane-polystyrene (PDMS-PS) copolymer were prepared at an ethyl benzoate-air interface, and density profiles were measured using neutron reflectivity. By varying the surface pressure Π it was possible to vary the density of chains in the brush and thereby test the accuracy of various analytical models. In contrast to the scaling predictions, Kent *et al.* found that brush height scaled as $h \propto \sigma^{0.22} N^{0.86}$. These results suggest that the analytical models are often limited by their inherent assumptions and are not truly applicable to the majority of experimental brushes.

The distribution of terminally attached polymer chains in a poor solvent is more poorly understood because the system cannot undergo ordinary phase separation. Uchida and Ikada [1997] imaged the surface of poly(2-dimethylamino)ethyl methacrylate (PDMAE-MA) brushes grafted on polyethylene terephthalate films in water using scanning atomic force microscopy. They observed surface inhomogeneities, which were measured reproducibly and attributed to the fact that the polymer was below its lower critical solution temperature in water. They also found that segment clusters would tilt in the direction of the AFM scan due to friction between the

AFM tip and the chains, with less load on the tip being required to induce tilting in longer chains. This suggests that clumping of polymer segments can occur in a very poor solvent along with brush collapse.

1.4.1.2 Advanced Brush Models

Milner, Witten and Cates [1988a, 1988b] and Zhulina, Pryamitsyn and Borisov [1989] independently developed analytical self-consistent-field models to describe brush distributions that provide essentially identical results. The basis of their model is the assumption that the set of all possible chain conformations may be replaced by the average chain trajectory, neglecting fluctuations about this average, when the chains are strongly stretched as in a brush [Semenov, 1985]. The main result is that the brush density profile is found to be a gradually decreasing function in the z -direction (normal to the surface). It is expressed in analytical form as a parabola as shown in Figure 1.1 (b), which is given by

$$\Phi(z) = (B/v)[h^2 - z^2] \quad (1.6)$$

where h is the equilibrium height given by $h = (12v\sigma/\pi^2)^{1/3} N$ and B is a prefactor equal to $\pi^2/8N^2$ [Milner, 1988a]. The brush density profile is predicted by Equation (1.6) to be a maximum at the surface and also to terminate abruptly at distance h from the surface. Similar to the Alexander-de Gennes brush, the equilibrium height is found to scale with N and $\sigma^{1/3}$. In this case, however, the brush is slightly more extended than the step-profile brush ($h/h_{step}=1.3$). Moreover the analytical SCF theory predicts a finite probability to find free end segments throughout the brush. Although many physical systems of interest may not lie in the regime of strong stretching, the analytical result is exact within this assumption and gives simple expressions to describe brush properties. Because of the compact analytical form of the step-

profile brush and parabolic brush models, they have received a great deal of attention [Kenworthy *et al.*, 1995; Baranowski and Whitmore, 1995; Milner, 1991].

More recently, advanced simulation techniques and lattice theories have been applied to the determination of brush distributions. Detailed computer experiments including numerical SCF calculations and Monte Carlo and molecular dynamics simulations have all shown good agreement with measured density profiles [Baranowski and Whitmore, 1995; Lai and Binder, 1991; Chakrabarti and Toral, 1990; Murat and Grest, 1989; Cosgrove *et al.*, 1987a]. Both approaches are able to predict a depletion layer next to the surface leading to a maximum in the density, followed by a region of decreasing density that terminates in a smooth tail region. The brush extension has been found to depend on the solvent conditions and surface adsorption. Computer experiments have also been useful for exploring system conditions that are not easily obtained in experiments, such as dependence of brush conformation on chain length and surface density.

In addition to their use as a test of model accuracy, simulations (both Monte Carlo and molecular dynamics), have also provided an accurate, detailed picture of tethered chain conformations and their influence on segment density distributions. Monte Carlo simulations, for instance, have been used by Chakrabarti and Toral [1990] and Lai and Binder [1991] to determine the true scaling behaviour of brush height and maximum segment density. Molecular dynamics calculations addressing the same questions have also been performed by Murat and Grest [1989]. Simulated chain lengths range from $N = 20$ to 99 and surface fractions from $s = 0.04$ to 0.2, thereby providing an accurate picture of brush structure over the realistic range of brush synthesis conditions.

Wijmans *et al.* [1992] carried out a detailed comparison of brush distributions calculated using an advanced numerical SCF model (Chapter 2), which makes no *a priori* assumptions about chain or brush distributions, with those calculated by the analytical theory of Zhulina *et al.* [1989]. The analytical theory cannot predict a depletion zone next to the surface; it also predicts a sharp end-point of the brush due to the central model result of a parabolic segment-density profile. As a result, important features of real brushes, which are accurately captured by numerical SCF theory, are lost in the analytical model. Nevertheless, the two analytical models have received considerable attention due to their simplicity. Moreover, both analytical models predict the exact behaviour of the brush in the limit $N \rightarrow \infty$ or under fully stretched chain conditions, which should be approached, at least approximately, in an athermal (*i.e.*, a good) solvent.

Lai and Binder [1992] compared scaling prediction from analytical models to results from Monte Carlo simulations for low-molecular-weight brush density profiles in near theta solvent conditions over the surface fraction range of $\sigma = 0.075$ to 0.125 . Simulated density profiles were characterized by a pronounced depletion zone near the grafting surface and a smooth tail region, similar to that shown in Figure 1.1 (c). Thus, even under good solvent conditions, the analytical models fail to predict important brush characteristics. Nevertheless, normalization ($\Phi(z)/\sigma^{1/2}$ vs. $z/N\sigma^{1/2}$) of simulated density profiles yields a universal curve, which is accurately predicted by scaling results except near the brush boundaries.

Under poor solvent conditions, the accuracy of the analytical models is significantly worse. Grest and Murat [1993] carried out molecular dynamics simulations of brushes in poor solvent and found that the parabolic density profile predicted by analytical SCF theory was in significant error. Unlike free chains, the tethered chains in a brush cannot phase separate under

poor solvent conditions. Using Monte Carlo simulations, Lai and binder [1992] were the first to observe lateral phase inhomogeneity of brushes in a poor solvent. The simulated chains formed collapsed clusters of segments when the solvent quality became poor enough to significantly favour polymer-polymer contacts. Grest and Murat [1993] also saw this lateral phase separation in their molecular dynamics simulations. At low enough surface coverage ($\sigma = 0.03$), 50 and 100 segment chains were seen to collapse into clusters leaving bare patches or holes through which the grafting surface was exposed. They saw a decrease in bare surface with increases in chain length and predicted that the holes would disappear with long enough chains, perhaps forming a dimpled brush surface. Yeung *et al.* [1993] studied the effect of solvent quality on brush phase stability using a numerical mean-field model combined with random phase approximation. They also concluded that as solvent quality decreased, the brush became unstable and would form a dimpled surface, in agreement with the AFM work of Uchida and Ikada [1997].

1.4.1.3 Brushes with Free Polymer in Solution

By interacting with the solvent, grafted chains and surface, free polymer in solution can influence brush configuration. Lee and Kent [1997] used neutron reflectivity to measure the density profiles of PDMS-PS copolymers adsorbed at the interface between air and ethyl benzoate solution containing free polystyrene. Selective deuteration of the adsorbed polystyrene ($N = 1625$ repeat units) and free polystyrene ($N = 413$ and 3846) in solution allowed them to measure the density profiles of each component independently. They observed a more compressed brush density distribution in the presence of the free polymer, and the tail region became less pronounced with higher molecular weight free polymer. They also found that there was significant penetration of the free polymer into the brush, even at $\sigma^* = 12$, which increased

with decreasing brush surface density. The degree of penetration was also seen to increase significantly with decreasing free chain length. Comparison of their experimental results to predictions of a modified analytical SCF theory showed that the free polymer penetrated much more than the model predicted [Lee and Kent, 1997].

Numerical SCF models have also been used to study the structure of the brush in the presence of free polymer. Wijmans and Factor [1996] carried out calculations, which simulated the experimental conditions of Lee *et al.* [1994] and found good agreement in terms of both density distributions and brush height. They were also able to reproduce the trends of brush height and penetration with varied surface density and free polymer chain length. They suggest that the decrease in brush height is a result of a shift in the balance between chain stretching and excluded volume interactions between brush chains. Penetration of the free polymer acts to screen excluded volume interactions in the brush, thereby reducing its height. However, the model consistently underestimated the brush height in the presence of free polymer. The model also underpredicts the penetration of the free polymer into the brush, although not as badly as analytical SCF models.

1.4.1.4 Brush Distributions – Summary

From this earlier work, a picture of polymer brushes in solution has emerged, in which long chain molecules stretch away from an interface, forming a partially ordered layer. This results from a balance between the entropic penalty associated with chain stretching and the unfavourable excluded volume interactions between neighbouring chains. Often, a depletion zone is observed near the surface, due to the entropic penalty imposed on chains by the impenetrable grafting surface. Unfavourable interaction between the polymer and solvent may lead to a more compressed layer, since the excluded volume term is less significant. In lower

ranges of surface coverage where the chains form a brush in a good solvent, decreased solvent quality may lead to lateral phase separation and thus exposure of the underlying surface. Also, a favourable segment adsorption energy may lead to absence of the depletion zone in a dense brush, or a rapidly decaying density profile in a less dense brush (pancake). Free polymer in solution will compress the brush, due to the balance between osmotic pressure of the brush and bulk solution, and this compression increases with increasing free polymer concentration. Also, significant free chain penetration into the brush is observed, which is greater for shorter free chains, but decreases with increased brush density.

Numerical and analytical models are also very useful for understanding (visualizing) and predicting behaviour of polymer brushes. Overall, the analytical models have shown value because of their simple form and ability to capture the basic physics of brushes. They do however contain some unrealistic assumptions, such as the step-profile brush model, which yield an unrealistic picture except in the case of a very high density brush. Also the strong stretching assumption for the parabolic brush model has been shown poor in most regimes of brush density and chain length that are experimentally obtainable. More complex computer models, such as numerical SCF, Monte Carlo and molecular dynamics models provide a significantly better picture of brush density profiles. Molecular dynamics simulations give presumably the best representation of a real system. However, due to the large computer capacity necessary for both MD and MC simulations, numerical SCF models have been widely used, showing good agreement with results of experiments and the more complex computer simulations. Typical computing time for SCF calculation of brush distributions is on the order of minutes for a desktop PC, which makes them convenient for investigation of a wide range of brush parameters.

1.4.2 Compression of Terminally Attached Polymers

Adsorbed polymer layers are known to prevent flocculation of colloidal particles in solution [Napper, 1983]. Early attempts to understand this phenomenon and identify conditions that would result in colloid stabilization were carried out by Hesselink [1971], Meier [1967], and Clayfield and Lumb [1966]. They used Monte Carlo simulations and models to calculate interaction potentials between particles on which polymeric stabilizers were adsorbed. Experimental verification of these predictions was provided by Dorozkowski and Lambourne [1971], who measured the repulsive force between colloidal particles experimentally using a surface balance. The repulsion between adsorbed layers of polymer was believed to result from loss of chain configurations and also a change in the free energy of mixing of polymer and solvent [Meier, 1967].

More advanced experimental equipment has allowed the force between two brushes to be measured directly. This has been carried out using the surface force apparatus (SFA) and the atomic force microscope (AFM). Reviews by Luckham [1996] and Claesson *et al.* [1996] discuss recent advances in the technology. The SFA employs two curved mica surfaces (convex) placed such that their cylindrical axes are perpendicular to one another. Polymer may be adsorbed or terminally attached to the mica surfaces, which are then moved together in small increments (nm scale) using a piezoelectric transducer. The force between the mica sheets is measured as a function of separation distance. The AFM uses a small cantilever with a very fine tip, which contacts a surface at positions controlled by a piezoelectric transducer. In very simple terms, the bending of the cantilever, as the surface is raised or lowered, is measured using a laser reflected off the back of the cantilever into a split photodiode. By knowing the spring constant

of the cantilever it is possible to calculate the applied force as a function of distance from the surface.

Hadziioannou *et al.* [1986] measured the force between surfaces of adsorbed poly(2-vinyl pyridine)-polystyrene (P2VP-PS) block copolymers using the SFA. They studied the case of PS in a good solvent (toluene) and found that the onset of repulsion occurred at about ten times the radius of gyration of a free PS chain. This was in contrast to adsorbed homopolymer layers where a repulsion onset was seen to occur at about $3R_g$, suggesting that a highly extended polymer layer was formed by the block copolymer under good solvent conditions. They also found that the force between surfaces increased monotonically with decreased separation, with the onset of repulsion occurring at higher separations for longer PS chains. Similar results showing a monotonically increasing repulsive force with compression have been shown by others [Kenworthy *et al.*, 1995; Taunton *et al.*, 1990; Taunton *et al.*, 1988; Patel *et al.*, 1988].

Hadziioannou *et al.* [1986] also observed a weak attraction between brushes in a less-than-theta solvent (cyclohexane at 26 C). This was attributed to net favourable polymer-polymer contacts in the poor solvent. Upon higher compression, the repulsive force increased more rapidly than in a good solvent, due to the more collapsed nature of the brush. Numerical SCF calculations by Van Lent *et al.* [1990] suggest that an attraction between brushes will be felt if the solvent does not meet theoretical theta conditions ($\chi_{12} = 0.5$). They attribute this attraction to the fact that terminally attached chains have essentially zero translational entropy and thus their phase behaviour is similar to that of infinite molecular weight chains.

Various attempts have been made to correlate experimental brush height data with scaling behaviour. This is difficult for two reasons. First, surface density and chain length are difficult to vary independently during brush synthesis. As a result, a clear dependence of brush height on

N at constant σ does not emerge from experiment, making theoretical comparisons difficult. Second, brush height cannot be measured directly, but instead is generally taken as the separation distance where the onset of brush repulsion occurs. It is unclear how this measured property relates to the actual brush height, and if the two properties scale linearly. This latter point has generated much confusion in the literature. Hadziioannou *et al.* [1986], for instance, report that brush height h scales linearly with N , while Ansarifard and Luckham [1988] and Taunton *et al.* [1990] reported a dependence of $N^{0.7}$ and $N^{0.6}$, respectively.

Scaling theory [de Gennes, 1985], which assumes a step-profile in density, predicts that the force to compress two layers of terminally-attached polymer whose surface coverage lies in the mushroom regime is given by

$$F \approx \frac{kT}{d^3 2h} \left(\frac{2h}{D} \right)^{8/3} \quad (1.7)$$

and that the compression force between two brushes on planar surfaces is given by:

$$F \approx \frac{kT}{d^3} \left\{ \left(\frac{2h}{D} \right)^{9/4} - \left(\frac{D}{2h} \right)^{3/4} \right\} \quad (1.8)$$

In Equations (1.7) and (1.8) numerical prefactors are ignored, and D represents the distance between the two grafting surfaces. In Equation (1.8) the first term in brackets gives the repulsive force due to the increase in osmotic pressure in the brush (higher excluded volume), while the second term accounts for the energetically favourable decrease in chain stretching. In the limit of close compression, where $D \ll h$, the osmotic term dominates and the force is predicted to scale with $D^{-9/4}$.

The energy to compress a brush with a parabolic segment density profile has also been determined and is given by [Milner, 1988a]:

$$A(u) = N(\sigma v)^{2/3} (\pi^2 / 12)^{1/3} \left[\frac{1}{2u} + \frac{1}{2} u^2 - \frac{1}{10} u^5 \right] \quad (1.9)$$

Here u is given by h'/h , where h' is the new brush height due to compression. Due to the "softer" parabolic density profile, the brush is predicted to have a lower compression energy at small compressions. Both models assume complete compression of the terminally attached chains, which excludes (experimentally relevant) cases where there is interpenetration of brushes.

Ansifar and Luckham [1988] compared scaling-theory predictions to their experimental results for the compression force of poly(2-vinylpyridine)-poly(*t*-butylstyrene) (P2VP-PBS) brushes adsorbed in toluene. They found that scaling theory underestimated the rate of increase in force with compression, which was found to be proportional to D^{-4} . In contrast, Taunton *et al.* [1990, 1988] measured the force between two brushes of PS in toluene under compression and found that the de Gennes scaling dependence of force provided a good representation of the data. Since the scaling results ignore numerical prefactors, it was necessary to adjust the curve with a single constant whose value was found to be about 1.5. Taunton *et al.* [1990] also compared the measured compression force with predictions of the model of Milner *et al.* [1988a]. The force calculated from the model was in very good agreement with experiment if the surface density was set to a value slightly higher than the experimental value.

Patel *et al.* [1988] have derived a more general expression for the brush compression energy, based on the de Gennes result, which introduces a parameter describing the solvent quality and numerical prefactors (k_1 and k_2) describing the contribution of the osmotic and

stretching terms to the energy, respectively. Although their expression is more complex, similar results are obtained.

A detailed study by Kenworthy *et al.* [1995] investigated the pressure-distance relationships of lipid bilayers containing PEG-derivatized lipids. The distance between liposome bilayers as a function of osmotic pressure was measured using X-ray diffraction. Bilayers with different PEG chain lengths and different mole fractions of derivatized lipid were constructed and used to study the effect of varied chain length and surface density on brush-brush interactions. They characterized the different regimes of surface coverage as (i) interdigitating mushrooms (where mushrooms could fit into gaps between mushrooms on the opposite surface), (ii) mushrooms and (iii) brushes. For all cases, they observed a monotonic increase in osmotic pressure with decreased separation. They also observed an earlier onset of repulsion and higher repulsive pressures with increased N or σ .

By comparing various models to their result, Kenworthy *et al.* [1995] found that compression of mushrooms in the interdigitating regime was best modeled assuming compression with no interdigitation, since pressure was underestimated by all models at large separations. They reached this conclusion even though at higher compressions it appeared that some interdigitation did occur. In the brush regime, Kenworthy *et al.* found that the de Gennes and Milner results gave good agreement at strong compression where the osmotic term dominates, but both models underestimated the repulsive pressure at weak compressions. They gave no explanation for the discrepancy, but the most likely explanation is that the analytical models underestimated the brush height, due to the sharp termination of the step or parabolic density profiles.

The analytical models of de Gennes and Milner also suffer from the assumption that no interpenetration occurs between the opposing layers as they move toward one another. Moreover, all molecular detail is lost in these models since they are based on energy balance arguments. Both of these limitations can be removed through more powerful computer simulation techniques. Murat and Grest [1991], for example, investigated the interaction of two brushes using molecular dynamics simulations and found that a significant degree of interpenetration occurs. They were able to show good agreement between their calculated force-distance curves and experimental results. Chakrabarti *et al.* [1994] confirmed that significant interpenetration occurs using Monte Carlo simulations.

Brush-brush interactions have also been investigated using numerical SCF models. Wijmans *et al.* [1994a] used numerical SCF theory to accurately calculate force-distance curves at weak compression and showed that the analytical model of Zhulina *et al.* [1989] underestimated the force at weak compression due to the absence of the tail region in the parabolic density profile. Martin and Wang [1995], also using numerical SCF, confirmed the importance of the tail region for the onset of repulsion. A more advanced numerical SCF model, which takes bond neighbour correlations into account, has recently been developed by Ruckenstein and Li [1997]. Calculated force-distance curves are in good agreement with experiment, in contrast to analytical models, which show large deviations in the regime of low compression. The numerical model required no adjustable parameters, although one could adjust the polymer-solvent interaction parameter. Ruckenstein and Li [1997] investigated the importance of chain interpenetration between the brushes and showed that the compression force was overestimated by up to an order of magnitude when interpenetration was not allowed.

1.4.3 Particle Interactions with Terminally Attached Polymers

The interaction of finite-sized particles with terminally attached polymers has received considerably less attention than the interaction between two end-grafted polymer surfaces, at least on the fundamental level. This is due to the difficulty of making experimentally meaningful measurements and the difficulty in modeling these systems. The majority of experimental work in this area involves protein adsorption experiments on surfaces modified with terminally attached polymers [Du *et al.*, 1997; Gombotz, 1992; Gölander, 1992]. Some useful information is also now being provided by chromatographic separation of proteins using terminally attached polymer [Brooks and Müller, 1996].

1.4.3.1 Experimental Studies

Experimental work describing the interaction of proteins with end-grafted polymer does not generally provide solid conclusions about how polymer properties influence the interactions. Different optimum chain lengths of end-grafted PEG have been reported for minimizing protein adsorption on PEG-modified surfaces. For PEG hydrogels, Gölander *et al.* [1992] reported that adsorption decreased with increasing polymer molecular weights up to 1.5 kDa, above which only a marginal decrease is observed. In attempting to minimize adsorption of fibrinogen and bovine serum albumin on polyethylene terephthalate films, Gombotz *et al.* [1991] reported an optimum PEG graft length of 3.5 kDa, above which little decrease in adsorption was seen. Desai and Hubbel [1991] reported that adsorption of albumin and fibrinogen onto PEG-grafted polyethylene terephthalate surfaces was minimized when PEG chains of molecular weight 18 500 g/mol or higher were used.

The difficulty in drawing solid conclusions about the optimum properties of grafted chains is due in large part to the interplay between surface density and degree of polymerization. Characterization of surfaces using electron spectroscopy for chemical analysis (ESCA) [Gombotz *et al.*, 1991; Desai and Hubbel, 1991] showed that higher molecular weight PEG was present on the surfaces in lower quantities. It is believed that the experimentally achieved surface densities are often lower for large polymer chains since they have a higher excluded volume and lower diffusion to the interface during synthesis. Thus, a given chain length may appear to give optimum protection because it resulted by chance in the best combination of chain length and surface density for protein exclusion after experimental synthesis.

Du *et al.* [1997] studied the behaviour of PEG derivatized lipid bilayers with respect to protein adsorption and cell adhesion. Like the work of Kenworthy *et al.* [1995], they were able to vary the PEG chain length ($M = 750 - 5000$) and surface density (0-5 mol% PEG-lipid) independently. For the range of PEG-lipid substitution used, the longest chains were seen to give the best reduction in protein and cell adhesion. They also observed a lower degree of protein adsorption and cell adhesion with increasing surface density of the PEG chains. For $M = 5000$ chains, the most significant decrease in adsorption and adhesion was seen up to about 1 mol% PEG-lipid, which is just above what they calculated as the theoretical point where complete surface coverage is achieved (0.7 mol%). Due to the fact that some protein still adsorbed after theoretically complete surface coverage, however, they concluded that complete surface coverage was never truly obtained. It appeared that the PEG chains were not randomly distributed, but instead arranged in denser and less dense regions of coverage.

Yang and Yu [1997] prepared self-assembled monolayers of end-functionalized PEG chains on glass slides and studied the adsorption and translational diffusion of bovine serum

albumin (BSA) on the surfaces. Using a fluorescent dye, they found that the level of adsorption decreased to about 6% of that on the bare glass surface. They also found that the surface diffusion coefficient measured using fluorescence recovery after photobleaching (FRAP) increased by almost an order of magnitude on the coated surfaces. Complete recovery of fluorescence was not observed, suggesting that some of the BSA was not surface-mobile. In contrast to adsorption on bare silica, however, adsorption was completely reversibly.

Yang and Yu [1997] also imaged protein sorbates on PEG covered and bare surfaces using an AFM. They observed regular ellipsoid patterns on the PEG-covered surface, which had the correct dimensions of BSA molecules, while the bare surfaces showed no regular patterns. From this information, they speculated that PEG reduced the magnitude of interactions between the protein and surface to a level where native-state conformations were retained.

1.4.3.2 Modeling of Brush-Particle Interactions

The empirical model of Joen *et al.* [1991a; 1991b] represents the first attempt to analyze the interaction of a spherical solute with a brush, in this case end-grafted polyethylene oxide (PEO). Interaction energies were calculated as the sum of a steric repulsion term, a van der Waals attraction term and a hydrophobic interaction term. The steric repulsion term is based on the brush model of de Gennes and makes use of the compression energy expression derived by Patel *et al.* [1988]. Thus, the model assumes the brush is completely compressed with no splaying as the particle approaches. It predicts that solute repulsion increases with increasing particle penetration and with increasing chain length at a given chain density. It also predicts, somewhat surprisingly, that the optimum chain density for solute repulsion depends upon the particle size. For larger proteins of radius $R = 60\text{-}80\text{\AA}$, the optimum distance between grafting

points d was found to be slightly more than that for small proteins of radius $R = 20\text{\AA}$ ($d = 13\text{-}17\text{\AA}$ vs. $9\text{-}11\text{\AA}$).

A molecular dynamics simulation of interactions between lysozyme and end-grafted PEG chains by Lim and Herron [1992] showed that the mobility of the chains may be important for reducing protein adsorption. Their simulations assumed a weak attraction between the polymer and some surface regions of the protein. In the simulations, the protein always diffused away from the surface although weak attachment of polymer segments to the protein sometimes occurred. The polymer chains were able to move with the protein until the contacts were broken. Lim and Herron [1992] also calculated the energy required for the protein to move into the surface of the brush and found a slight attraction at very weak penetration (4\AA) followed by strong repulsion. In some cases there was a maximum in repulsion energy at very weak penetration that they attribute to the protein squeezing through a small opening in the PEG chains.

In order to treat brush interactions with a small particle, Subramanian *et al.* [1995] have modeled the interaction of a finite-sized cylinder with a brush using the equation for brush compression of Milner *et al.* [1988a]. In this way, they consider the case where only brush compression occurs and show that the repulsive force is always increasing with approach of the particle. They ignore the case where polymer chains may spread around the particle, although they acknowledge that this would be important for small particles. One clue as to the importance of particle size is offered by the numerical SCF work of Wijmans *et al.* [1994b] who studied the interaction potential of two spherical particles of radius ranging from 2 to 10 lattice units (on the size scale of proteins) whose surfaces were covered with grafted chains. They found that the repulsion between particles was much lower than that predicted using the Derjaguin

approximation for repulsion between two flat surfaces. This was attributed to the ability of polymer chains ($N = 50$) to move out of the gap between the approaching particles. This kind of molecular detail is required to see the correct interactions between polymer and very small particles.

Recently, Murat and Grest [1996] reported MD simulation results for an AFM tip interacting with a brush, from which some insights for an interacting particle can be inferred. The simulations show that the applied force required increases with brush compression. The increase in force is less than that predicted by the simple model of Subramanian *et al.* because the chain segments are in fact able to escape from under the AFM tip. Larger tip sizes lead to a more rapid increase in compression force since it is more difficult for the chains to escape. However, since the chain segments are able to rearrange themselves around the tip, the segment density between the tip and the surface was found to remain approximately constant (the same as that of the undisturbed brush), in sharp contrast to predictions of analytical models.

2 Model Outline

2.1 Origins of Nonideal Mixing in Liquid Solutions

In order to understand the properties of a solution, it is often useful to compare behaviour of a mixture to that of an ideal solution as defined by Raoult's law. The activity a_i of any component i is then equal to its mole fraction x_i . Deviations from Raoult's law are observed when this condition is not met and mixing therefore results in a nonzero change in enthalpy ($\Delta H_m \neq 0$) or nonzero excess entropy ($S^E \neq 0$). Under such conditions, the ratio a_i/x_i is no longer equal to unity, but is instead set equal to γ_i , the activity coefficient of i .

Mixing nonidealities are known to result from asymmetries in the energetics of the molecular interactions occurring in the mixture. For instance, water must break energetically favourable hydrogen bonds with itself in order to solvate a non-hydrogen-bonding solute. As a result, ΔH_m is nonzero and γ_i is often far from unity for the dilute solute component. In polymer solutions, mixing leads to large negative values of S^E due to the connected nature of the polymer chain, which severely limits the number of ways in which the polymer can be arranged in the mixture. As a result, nonideality is observed even though ΔH_m is near zero. Moreover, nonidealities occur at extremely small mole fractions of polymer. This latter effect arises because of the large size difference between polymer and solvent. Thus, the mole fraction of polymer remains small even as its weight fraction approaches 0.5.

The unusual mixing properties of polymer solutions were first recognized in a formal way by Flory [1953; 1942] and Huggins [1942], whose combined theory has served as a basis for understanding polymer-mixing thermodynamics for over 50 years.

2.1.1 Entropy of Mixing Polymer in Solvent

In order to conform to ideal solution behaviour, a solution must meet two requirements [Flory, 1953]. The first is that the entropy of mixing is equal to

$$\Delta S_m^{id} = -R \sum_i x_i \ln x_i \quad (2.1)$$

where R (J/K-mol) is the gas constant and x_i is the mole fraction of component i . The second is that all mixing is athermal or the heat of mixing ΔH_m is zero.

Since the mole fraction of each component must be less than unity, Equation (2.1) is always positive. The increase in entropy is due to the increased number of possible arrangements of the molecules in the system. Modeling a binary mixture using a simple lattice allows the number of different possible arrangements of the molecules to be counted, at least approximately. Flory [1953] showed for a lattice of n_0 sites, which contain n_1 solvent and n_2 solute molecules, the number of ways of arranging them is

$$\Omega = \frac{n_0!}{n_1!n_2!} \quad (2.2)$$

which is simply the number of ways of arranging n_0 things n_1 at a time. Through Boltzmann theory

$$\Delta S = -k \ln \Omega \quad (2.3)$$

which reduces to Equation (2.1) after substitution of Equation (2.2).

For the case of a polymer solution, Equation (2.1) greatly overestimates the entropy of mixing. This is due to the fact that n_2 polymer molecules of degree of polymerization N will have less possible mixing arrangements with n_1 solvent molecules than an equal volume of

solvent-sized solute molecules (*i.e.* Nn_2) would. Flory-Huggins theory treats the polymer molecules as a series of connected segments, and calculates the number of possible ways of inserting the adjacent (connected) segments into the lattice. For example, the number of sites available for placement of molecule $i+1$ is given by

$$v_{i+1} = (n_0 - Ni)z(z-1)^{N-2}(1-f_i)^{N-1} \quad (2.4)$$

where i is the number of previously placed molecules, z is the lattice coordination number (*i.e.* the number of nearest neighbours), and f_i is the probability that a site adjacent to the previously vacant one (where the previous segment was placed) is occupied. This probability of occupancy f_i in the mean field approximation is simply given by Ni/n_0 . The total number of possible ways of arranging n_2 sets of N consecutively adjacent lattice sites correcting for the fact that the molecules are identical is:

$$\Omega = \frac{1}{n_2!} \prod_{i=1}^{n_2} v_i = \left[\frac{n_0!}{(n_0 - Nn_2)!n_2!} \right] \left(\frac{z-1}{n_0} \right)^{n_2(N-1)} \quad (2.5)$$

Substituting this expression into Equation (2.3) and subtracting the reference state of unmixed, amorphous components gives the surprisingly simple expression

$$\Delta S_m = -n_0 R \sum_i \frac{\Phi_i}{N_i} \ln \Phi_i \quad (2.6)$$

for a mixture of i different components. For very large molecules, Equation (2.6) states the entropy of mixing no longer depends directly upon the mole fraction, but rather on the volume fraction Φ_i ($= N_i n_i / n_0$) of each component. Figure 2.1 shows a comparison of the entropy of mixing calculated using Equations (2.1) and (2.6). The Flory-Huggins ΔS_m is approximately

half ΔS_m^{id} . It should be noted, however, that Flory Huggins theory slightly overestimate the decrease in mixing entropy of polymer solutions. Thus the true entropy of mixing lies somewhere between the two curves shown in Figure 2.1 [Johansson *et al.*, 1997].

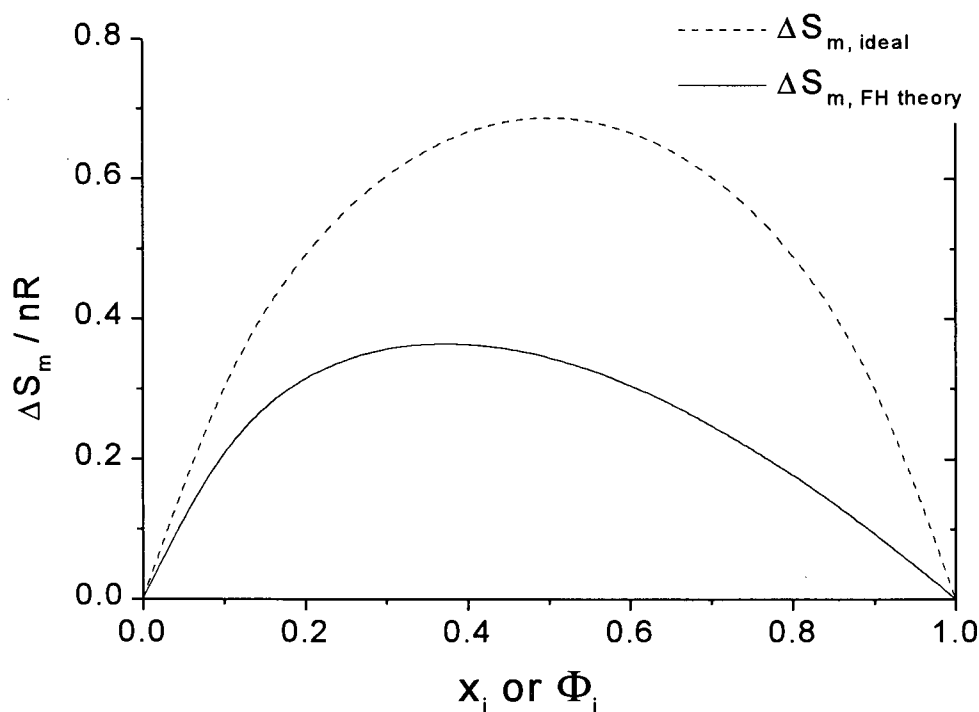


Figure 2.1: Comparison between ideal entropy of mixing and combinatorial entropy of mixing given by Flory-Huggins theory for a polymer chain of 1000 segments.

2.1.2 Enthalpy and Gibbs Energy of Mixing

In order to account for enthalpic interactions between components in solution, Flory assumed that only nearest neighbour contacts are significant. Thus, interactions between components that are not immediate neighbours are viewed as being sufficiently weak to make a negligible contribution to the total mixing energy. As with the entropy, a change in energy with

mixing is calculated using the unmixed components as a reference state. This is carried out by considering the difference in energy between the like contacts, [1,1] and [2,2], and the unlike contact [1,2] (for the simple case of a binary mixture).

Let ω_{11} , ω_{22} and ω_{12} be the energy values associated with the respective contacts. It is then possible to write an interchange energy, which is defined by statistical mechanics, as

$$\Delta\omega_{12} = \omega_{12} - \frac{\omega_{11} + \omega_{22}}{2} \quad (2.7)$$

based on the stoichiometry of $\frac{1}{2}[1,1] + \frac{1}{2}[2,2] = [1,2]$. The heat of mixing is then given by

$$\Delta H_m = z\Delta\omega_{12}n_1\Phi_2 \quad (2.8)$$

where component 1 is assumed to be a monomeric solvent. This result is often further simplified by defining a dimensionless parameter χ_{12} , which incorporates the interchange energy and changes its basis from the energy change with respect to one contact, to that for interchange of one lattice site. This parameter, called the Flory-Huggins interaction parameter, is defined as

$$\chi_{12} = z\Delta\omega_{12} / kT \quad (2.9)$$

and can be measured experimentally; typical values lie in the range of -1 to 1 kT [*Polymer Handbook*].

Flory's expressions for the entropy and enthalpy of mixing provide a simple, general expression for the Gibbs energy of mixing polymer and solvent

$$\Delta G_m = n_0 RT \sum_i \left[\frac{\Phi_i}{N_i} \ln \Phi_i + \sum_{j=i+1}^m \chi_{ij} \Phi_i \Phi_j \right] \quad (2.10)$$

where m is the total number of components. Equation (2.10) can be used to calculate any thermodynamic property of a polymer solution, such as the chemical potential of the solvent or polymer.

2.2 Self-Consistent Mean-Field Theory of Scheutjens and Fleer

Flory-Huggins theory deals with an entire solution volume using the mean-field approximation. It is possible to get more detailed information from a lattice model by defining smaller regions in which properties are averaged. In order to study the adsorption of polymer at an interface, Scheutjens and Fleer [1979;1980] treated each layer of a Cartesian lattice with mean-field averaging as shown in Figure 2.2 (a). They developed a self-consistent mean-field (SCF) model, which allowed calculation of the polymer concentration profile in the direction normal (z) to the sorbent surface. We will refer to the original SCF model with concentration variation in one dimension as the 1D model.

An extension of the Scheutjens and Fleer model by Cosgrove *et al.* [1987a] gives the density distribution of end-grafted chains away from the grafting surface (normal to the interface). This work was shown to give very good quantitative agreement with experimentally measured density profiles [Cosgrove and Ryan, 1990b]. Leermakers *et al.* [1990] extended this model to a cylindrical lattice (Figure 2.2 (b)) to allow calculation of the segment density distribution in two dimensions (2D model). This allowed Leermakers *et al.* [1990] to study the energetics of membrane formation and the distribution of chains in inhomogeneous membranes.

Our goal is to model a particle interacting with end-grafted polymer chains, which requires both of the above extensions to the original 1D self-consistent-field model of Scheutjens and Fleer. In particular, the cylindrical coordinate system of Leermakers *et al.* [1990] allows the distribution of end-grafted polymer around a particle to be monitored in the direction normal (z)

to the grafting surface and in the radial (r) direction (parallel to the grafting surface). In addition, by combining step-weighted walk statistics with a statistical mechanical treatment of the lattice, important thermodynamic information about the system can be calculated such as how much energy it takes to move the particle into the grafted polymer.

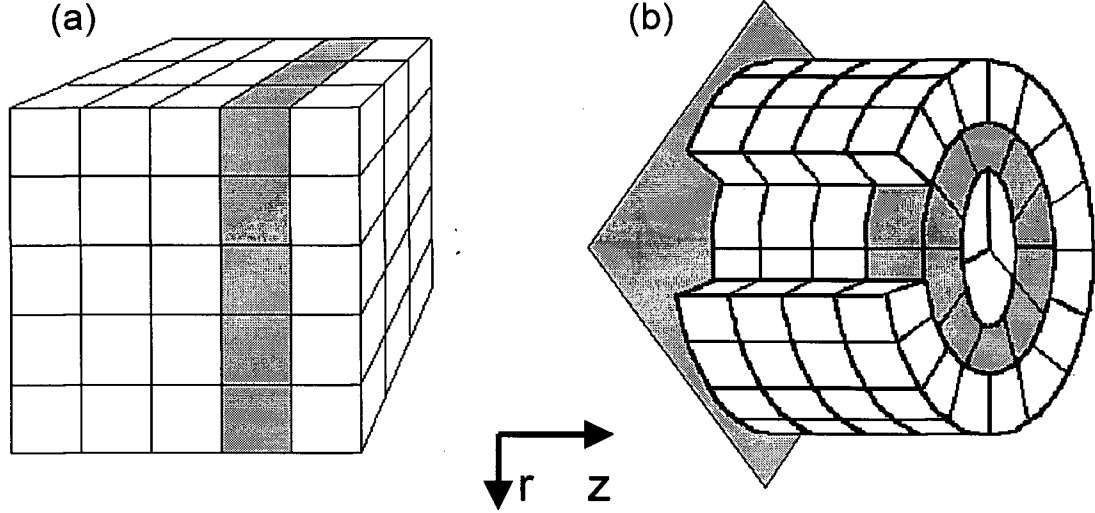


Figure 2.2: Cartesian (a) and cylindrical (b) lattice geometries used in the self-consistent-field model. Areas treated with mean-field averaging are shown in grey as well as the grafting surface in (b).

The derivation of our model equations follows that for the original 1D model [Fleer et al., 1993; pp.171-180]. However, due to the addition of an extra dimension there are some important differences, which will be outlined in the following sections. Moreover, all model equations related to the movement of a particle into the grafted chain volume are new.

The grand canonical partition function Ξ can be written as a summation of canonical partition functions Q weighted with the appropriate Boltzmann factors:

$$\Xi(\mu_i, V, T) = \sum_N Q(N, V, T) e^{\frac{N\mu}{kT}} \quad (2.11)$$

The equilibrium distribution of polymer corresponds to the maximum term of Equation (2.11), taken with respect to the number of chains in various conformation distributions $\{n_i^c\}$. This is found from the total differential

$$\sum_i \sum_c \left\{ \frac{\partial \ln \Xi}{\partial n_i^c} \right\}_{V,T} dn_i^c = 0 \quad (2.12)$$

where n_i^c is the number of molecules of component i adopting a conformation denoted by c . The lattice and polymer conformations in it are further constrained by the requirement that all lattice sites be occupied, which is given by

$$\sum_i \sum_c \{n_i^c r_i^c(z, r) - L(r)\} = 0 \quad (2.13)$$

where $r_i^c(z, r)$ is the number of segments of the chain of type i in conformation c that are in the radial of the cylinder in position (z, r) . $L(r)$ is the number of lattice sites in radial r .

The maximum of a constrained function can be found using the method of Lagrange multipliers. A new function is therefore written

$$f = \ln \Xi - \sum_z \sum_r \alpha(z, r) \left\{ \sum_i \sum_c n_i^c r_i^c(z, r) - L(r) \right\} \quad (2.14)$$

where $\alpha(z, r)$ represents the Lagrange multiplier for each mean-field radial position in the lattice. Taking the derivative of this expression with respect to one molecule of type k in conformation d gives:

$$\frac{\partial \ln \Xi}{\partial n_k^d} - \sum_z \sum_r \alpha(z, r) r_k^d(z, r) = 0 \quad (2.15)$$

The grand partition function Ξ is then expanded into its individual terms and evaluated with respect to a reference state denoted by $*$. The most convenient reference state is that of pure, unmixed, amorphous components, where $\Xi^* = \prod_i \Xi_i^*$, $\Omega^* = \prod_i \Omega_i^*$ and $U^* = \sum_i U_i^*$. The expansion gives:

$$\frac{\partial \ln \Omega / \Omega^*}{\partial n_k^d} - \frac{\partial (U - U^*) / kT}{\partial n_k^d} + \frac{\mu_k - \mu_k^*}{kT} - \sum_z \sum_r \alpha(z, r) r_k^d(z, r) = 0 \quad (2.16)$$

Here Ω represents the multiplicity, or the number of ways that a specific set of molecules with fixed internal energy U can be placed on the lattice, and μ is the chemical potential. It is now necessary to develop expressions for Ω/Ω^* , $U-U^*$ and $\mu-\mu^*$ based on the lattice model.

2.2.1 Cylindrical Lattice Geometry

In the cylindrical lattice (Figure 2.2 (b)), cylinder axis layers are numbered $z = 1, \dots, Z_{max}$ in the direction normal to the grafting surface and rings in the radial direction are numbered $r = 1, \dots, R_{max}$. In each ring, within a given layer z , the lattice sites are considered to be indistinguishable and treated by mean-field averaging. The grafting surface at $z = 0$ is treated as impenetrable and all other surfaces are treated as reflecting boundaries. In all calculations, the lattice is large enough that boundary effects on the chains are negligible.

The area of a given radial, specified in lattice units, is given by:

$$L(r) = \pi \{ r^2 - (r-1)^2 \} \quad (2.17)$$

The circumference $S(r)$ is then given by:

$$S(r) = 2\pi r \quad (2.18)$$

Evaluation of the step-weighted random-walk chain configurations requires knowledge of the step probability for a move from a given lattice site to any adjacent site. We follow the same rules as Leermakers *et al.* [1990], and allow steps up (higher z), steps down or steps in the same layer. We also allow steps inward (lower r), steps outward, or steps in the same radial shell, and any combination of these two steps simultaneously (*i.e.* in and down).

Physically the lattice step probabilities are a consequence of the assumed geometry and are thus constants. In the normal direction, if a hexagonal lattice is assumed (12 nearest neighbors), the probability to step up or down a layer is $\lambda_1(z) = \lambda_{-1}(z) = 3/12$, corresponding to the number of nearest neighbors in the layers adjacent to layer z . The probability to stay in the same layer z is then $\lambda_0(z) = 6/12$. For steps inward and outward the probabilities are made proportional to the lattice site surface area on the face that is crossed so that:

$$\begin{aligned}\lambda_{-1}(r) &= \frac{1}{4} S(r-1)/L(r) \\ \lambda_0(r) &= 1 - \lambda_{-1}(r) - \lambda_1(r) \\ \lambda_1(r) &= \frac{1}{4} S(r)/L(r)\end{aligned}\tag{2.19}$$

Thus, the probability to step down and outward simultaneously is given by

$$\lambda_{-1,1}(z, r) = \lambda_{-1}(z) \lambda_1(r)\tag{2.20}$$

and likewise for all other step directions.

2.2.2 Combinatorial Entropy

The multiplicity Ω can be calculated from the number of ways of placing volumeless chains in the lattice corrected in a mean-field approximation to account for chain volume. The number of ways ω_i^c of placing a single volumeless chain i with conformation c (which may include a number of degenerate states) is given by

$$\omega_i^c = L_i^c \prod_{s=2}^{N_i} Z \lambda^c(z_s - z_{s-1}, r_s - r_{s-1}) \quad (2.21)$$

where Z is the lattice coordination number, L_i^c is the number of sites available for placement of the first segment of the chain, and $\lambda^c(z_s - z_{s-1}, r_s - r_{s-1})$ is the step probability for insertion of the next segment in the chain. The product is over all segment positions, denoted by a ranking number s up to the full chain length N_i . The number of ways of placing all n_i^c chains can be generalized in the following way to account for all components in all possible conformations:

$$\Omega' = \prod_i \prod_c \frac{(\omega_i^c)^{n_i^c}}{n_i^c!} \quad (2.22)$$

The numerator of Equation (2.22) accounts for the ways of placing all chains of type i in conformation c , and the denominator corrects for the fact that each chain of type i is indistinguishable.

What remains is to reintroduce chain volume into the "volumeless" multiplicity function Ω' defined by Equation (2.22). This is achieved by multiplying Ω' with the fraction of vacant sites available to each new segment added to the chain. The correction factor for the first segment placed in radial (z, r) is $L(r)/L(r) = 1$. For the second segment placed in the same

radial, the correction factor is $(L(r)-1)/L(r)$. The total correction for filling all the lattice sites in a given radial (z,r) is then $L(r)!/L(r)^{L(r)}$. Thus, the total correction to Ω' for occupancy of all possible radials R_{max} and all layers Z_{max} is:

$$\prod_{z=1}^{Z_{max}} \prod_{r=1}^{R_{max}} \frac{L(r)!}{L(r)^{L(r)}} = \prod_{r=1}^{R_{max}} \left[\frac{L(r)!}{L(r)^{L(r)}} \right]^{Z_{max}} \quad (2.23)$$

Combination of Equations (2.22) and (2.23), which is our next step, can be greatly simplified by subtracting the multiplicity of the reference state (the result being the total increase in the number of possible molecular arrangements due to mixing). According to Flory [1953], the multiplicity of the pure amorphous polymer chain (see Equation (2.5)) is given by:

$$\Omega_i^* = \frac{(N_i n_i)!}{n_i!} \left(\frac{Z}{N_i n_i} \right)^{n_i(N_i-1)} \quad (2.24)$$

Combining Equations (2.22) to (2.24) and application of Stirling's approximation then leads to

$$\ln \left(\frac{\Omega}{\Omega^*} \right) = \sum_i \sum_c n_i^c \ln \frac{L_i^c \lambda^c}{N_i n_i^c} \quad (2.25)$$

after careful rearrangement of terms. Here λ^c is the product of step probabilities for placing all of the segments in a chain defined by the conformation c . This expression represents the entropic part of the partition function. Taking the derivative of Equation (2.25) with respect to n_k^d gives the following expression

$$\frac{\partial \ln \Omega / \Omega^*}{\partial n_k^d} = \ln \left(\frac{L_k^d \lambda^d}{N_k n_k^d} \right) - 1 \quad (2.26)$$

which provides the first term of Equation (2.16).

2.2.3 Internal Energy

In this work, we assume that all energetic interactions are adequately described by the Flory interaction parameter χ_{ij} . Thus, the change in energy, with respect to the reference state, for one segment of i to be placed in radial (z,r) is given by

$$\frac{u_i - u_i^*}{kT} = \sum_j \chi_{ij} \langle \Phi_j(z,r) \rangle \quad (2.27)$$

where the summation on j excludes component i , and the angular brackets represent a layer average. The layer average is needed in SCF theory because all lattice radials adjacent to a given radial (z,r) contain different volume fractions of each component. Thus, the result differs from Flory-Huggins theory, in which the whole solution is assumed to have a uniform distribution of each segment type. The layer average is given by

$$\langle \Phi_j(z,r) \rangle = \sum_{z'} \sum_{r'} \lambda_{z'-z, r'-r} \Phi_j(z', r') \quad (2.28)$$

where the summations are over all lattice positions adjacent to radial (z,r) , and $\lambda_{z'-z, r'-r}$ is the fraction of surface area a site in radial (z,r) has in contact with a site in radial (z',r') .

The total energy expression $(U-U^*)/kT$ can be obtained by multiplying Equation (2.27) with the number of segments of i in a lattice radial $L(r)\Phi_i(z,r)$ and summing over all components

$$\frac{U - U^*}{kT} = \frac{1}{2} \sum_z \sum_r L(r) \sum_i \sum_j \Phi_i(z,r) \chi_{ij} \langle \Phi_j(z,r) \rangle \quad (2.29)$$

where the factor of $\frac{1}{2}$ is needed to account for double counting of pair interactions. An adsorbing interface can be accounted for in the model by including the surface in the summation

over all components. Adsorption then occurs if a segment is in a layer next to a surface, such as a segment in layer 1 next to an impenetrable surface at $z=0$. The surface is treated as a component with $\Phi=1$ in layer $z=0$.

Finally, the derivative of Equation (2.29) with respect to n_k^d can be taken in order to generate the second term of Equation (2.16). The result is:

$$\frac{\partial \{U - U^*/kT\}}{\partial n_k^d} = \sum_z \sum_r \sum_i r_k^d(z, r) \chi_{ki} \langle \Phi_i(z, r) \rangle \quad (2.30)$$

2.2.4 Equilibrium Segment Density Distribution

In order to complete Equation (2.16), we need an expression for the chemical potential of component k . Evers et al. [1990] have noted that μ_k for a multicomponent mixture is most easily derived using the relation $A - A^* = -kT \ln \Omega/\Omega^* + (U - U^*)$. When this is applied to the bulk solution, we find

$$\frac{(\mu_k - \mu_k^*)}{kT} = 1 + \ln \Phi_k^b - N_k \sum_i \frac{\Phi_i^b}{N_i} - \frac{N_k}{2} \sum_i \sum_j \Phi_i^b \chi_{ij} \Phi_j^b + N_k \sum_i \chi_{ik} \Phi_i^b \quad (2.31)$$

where the superscript b denotes a bulk volume fraction. This result may also be obtained using the Flory-Huggins expression generalized to i components, since the more complex combinatorial and energy terms derived above reduce to those of Flory-Huggins theory when applied to a homogeneous bulk solution.

Substituting Equations (2.26), (2.30) and (2.31) into Equation (2.16) allows one to write an expression that satisfies the condition of equilibrium

$$\ln\left(\frac{L_k^d \lambda^d \Phi_k^b}{N_k n_k^d}\right) - \sum_z \sum_r r_k^d(z, r) \frac{u_k(z, r)}{kT} = 0 \quad (2.32)$$

where

$$\frac{u_k(z, r)}{kT} = \alpha(z, r) + \sum_i \frac{\Phi_i^b}{N_i} + \frac{1}{2} \sum_i \sum_j \Phi_i^b \chi_{ij} \Phi_j^b + \sum_i \chi_{ki} (\langle \Phi_i(z, r) \rangle - \Phi_i^b) \quad (2.33)$$

and $u_i(z, r)$, defined by Scheutjens and Fleer [1979, 1980], is the mean segment potential, which consists of two separate contributions:

$$u_k(z, r) = u'(z, r) + u_k^{\text{int}}(z, r) \quad (2.34)$$

The first term in Equation (2.34) represents a hard core potential that is independent of segment type

$$\frac{u'(z, r)}{kT} = \alpha(z, r) + \sum_i \frac{\Phi_i^b}{N_i} + \frac{1}{2} \sum_i \sum_j \Phi_i^b \chi_{ij} \Phi_j^b \quad (2.35)$$

and the second term defines an interaction potential

$$\frac{u_k^{\text{int}}(z, r)}{kT} = \sum_i \chi_{ki} (\langle \Phi_i(z, r) \rangle - \Phi_i^b) \quad (2.36)$$

that depends on the energetic interactions between segments in the lattice.

By careful rearrangement of Equation (2.32), we can determine the number of chains i in a conformation c

$$n_i^c = \frac{\Phi_i^b L_i^c \lambda^c}{N_i} \prod_z \prod_r G_i(z, r)^{r_i^c(z, r)} \quad (2.37)$$

where $G_i(z, r)$ is a Boltzmann factor given by:

$$G_i(z, r) = \exp\left(-u_i(z, r)/kT\right) \quad (2.38)$$

$G_i(z, r)$ is also called the free segment weighting factor and represents the preference a free segment of component i has for being in radial (z, r) with respect to the bulk solution. The free segment weighting factors G_i and the step probabilities λ allow one to calculate the statistical weight of any conformation.

In practice, it is not efficient to generate the weighting for individual conformations since it does not provide an average distribution over all possible conformations. Scheutjens and Fleer [1979] used a matrix formalism developed by Dimarzio and Rubin [1971] to generate simultaneously the statistical weighting of all possible conformations. This method has taken the form of a generalized recurrence relation [Evers, 1990; Leermakers, 1990] that gives the chain-end distribution function as

$$G_i(z, r, s+1|1) = G_i(z, r) \langle G_i(z, r, s|1) \rangle \quad (2.39)$$

where $G_i(z, r, s+1|1)$ is the statistical weighting factor (chain end weighting factor) for a chain of $s+1$ segments to end in radial (z, r) after starting from an end segment with ranking 1. For the case of grafted chains, the chain-end distribution function must be generated from each end of the chain (fixed and free) since inversion symmetry does not apply to end-grafted chains [Cosgrove et al., 1987a].

2.2.5 Chain Grafting

Grafting chains to the end of the lattice at layer 1, is achieved by applying the recurrence formula in Equation (2.39), started from segment 1 with the restriction that:

$$G_i(z, r, 1|1) = G_i(z, r) \quad ; \quad z=1, \text{ all } r \quad (2.40)$$

$$G_i(z, r, 1|1) = 0 \quad ; \quad \text{all other } z \text{ and } r \quad (2.41)$$

Grafting positions are specified through different restrictions on Equation (2.40). It is possible, for example, to graft a single chain to the center radial of the cylinder by specifying the only nonzero starting value in Equation (2.40) at $(z=1, r=1)$. The complementary chain-end distribution function is then generated (starting at the other end of the chain) with no restrictions on the location of the free end. This is done using Equation (2.39) from the starting point $G_i(z, r, N|N) = G_i(z, r)$ for all z and r .

Scheutjens and Fleer showed that the statistical weight of an inner chain segment can be generated using the chain-end weighting factors for a shorter chain of length s and a second chain of length $N - s$. This approach follows from the "composition law", which is shown schematically in Figure 2.3.

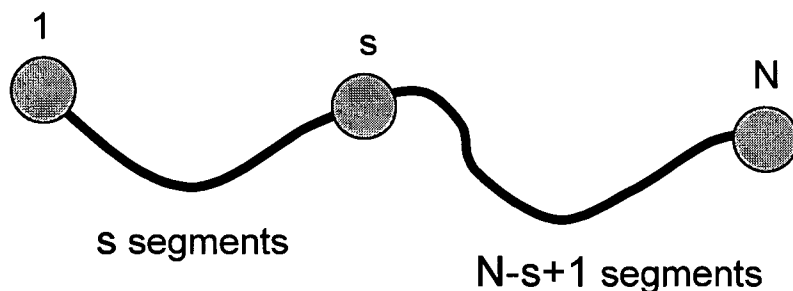


Figure 2.3: The probability that segment s ends in radial (r, z) is found by combining the probability of two shorter chains ending in that radial. This involves combining two step-weighted walks, one for $1, 2, \dots, s$ segments and one for $N, N-1, \dots, s$.

To calculate the volume fraction $\Phi_i(z, r)$ of a component i in radial (z, r) in our model, the chain-end weighting factors for all chain conformations are computed and combined according to the composition law to give:

$$\Phi_i(z, r) = C_i \sum_s \frac{G_i(z, r, s|1)G_i(z, r, s|N)}{G_i(z, r)} \quad (2.42)$$

The summation s is over all segment positions in the chain and a normalization constant C_i is needed to transform the weighting factors to volume fraction. The normalization constant for free chains is then given by $C_i = \Phi_i^b / N_i$.

For components, which are free to move in or out of the system, Φ^b must be specified. If however, one component is restricted to remain within a certain area of the lattice, such as end-grafted chains, the true bulk volume fraction Φ^b will be zero for that component. It then becomes necessary to have a different way of specifying the amount of that component in the system. Scheutjens and Fleer [1985] therefore introduced the idea of restricted equilibrium. Under restricted equilibrium conditions, one can replace Φ^b with a pseudo-equilibrium bulk volume fraction calculated using the chain end weighting factors.

Summing the equilibrium expression (Equation (2.37)) over all possible conformations n_i^c gives n_i . Substitution of $C_i = \Phi_i^b / N_i$ then allows one to write the normalization constant as:

$$C_i = \frac{n_i}{\sum_z \sum_r L(r)G_i(z, r, N|1)} \quad (2.43)$$

This expression can be used with Equation (2.42) for molecules in restricted equilibrium, where n_i is the number of molecules of i , which must be specified for the calculation. The denominator of the expression gives the total statistical weight to find a set of chains containing all possible conformations in the cylindrical lattice.

The combination of Equations (2.38), (2.34), (2.36) and (2.42) constitutes a set of self-consistent equations that must be solved using numerical techniques. This is because the volume fraction $\Phi_i(z,r)$ of each component is calculated from the free segment weighting factors $G_i(z,r)$ based on the mean segment potentials $u_i(z,r)$. The mean segment potentials in turn depend on the volume fraction distribution of the components through the functional dependence of the interaction potential $u_i^{\text{int}}(z,r)$.

2.2.6 Interaction Energy

The partition function Q is related to the change in Helmholtz energy of the system to by

$$\ln(Q/Q^*) = \frac{-(A - A^*)}{kT} = \ln(\Omega/\Omega^*) - \frac{(U - U^*)}{kT} \quad (2.44)$$

where the second equality separates the Helmholtz energy into its energetic and entropic component:

$$S - S^* = -k \ln(\Omega/\Omega^*) \quad (2.45)$$

Equation (2.45) allows one to define the mixing entropy in terms of the free segment weighting factors and volume fractions by substitution of the equilibrium expression (Equation (2.37)) into the combinatorial expression (Equation (2.25)). Taking the summation over all conformations gives:

$$(S - S^*)/k = \sum_i \sum_z \sum_r L(r) \Phi_i(z,r) \left[\frac{\ln \Phi_i^b}{N_i} + \ln G_i(z,r) \right] \quad (2.46)$$

By adding the energy term to this expression the complete expression for the change in Helmholtz energy is obtained:

$$\frac{(A - A^*)}{kT} = \sum_z \sum_r \sum_i L(r) \Phi_i(z, r) \left[\frac{\ln \Phi_i^b}{N_i} + \ln G_i(z, r) + \frac{1}{2} \sum_j \chi_{ij} \langle \Phi_j(z, r) \rangle \right] \quad (2.47)$$

The restricted equilibrium criteria then allow one to make a useful substitution in Equation (2.47) for the bulk volume fraction of grafted components:

$$\Phi_i^b = \frac{N_i n_i}{\sum_z \sum_r L(r) G_i(z, r, N|1)} \quad (2.48)$$

Finally the energy change due to the movement of a particle into the grafted polymer chains is calculated by

$$A^{\text{int}}(z) = \{A - A^*\}(z) - \{A - A^*\}(\infty) \quad (2.49)$$

where the coordinate z represents the layer position of the leading edge of the particle. The particle is moved in the z -direction toward the surface one layer at a time and the brush distribution and Helmholtz energy are calculated at each position.

2.2.7 Numerical Solution

The set of self-consistent equations may be solved numerically by writing a set of non-linear functions [Leermakers, 1988] of the form:

$$f_i(z, r) = 1 - \frac{1}{\sum_i \Phi_i(z, r)} + \frac{\sum_i u_i'(z, r)}{\sum_i 1} - u_i'(z, r) = 0 \quad (2.50)$$

The set includes an equation for each component in each mean-field radial of the lattice. The first two terms of Equation (2.50) require that the volume fractions of all components add up to unity in each lattice site, and the second two terms are only satisfied when the hard core potential

becomes independent of segment type. An example of the computer code written for the calculations is provided in Appendix A.

The problem could be solved using a global minimization method, where the root of the sum of squares $F = \left[\sum_z \sum_r \sum_i f_i^2(z, r) \right]^{1/2}$ is minimized, but a non-linear equation method has been chosen, since the functions are fairly well behaved, and the need for second-order derivatives is avoided. No conditions have been observed where the Jacobian J

$$J = \begin{bmatrix} \frac{\partial f_1}{\partial u_1}, \frac{\partial f_1}{\partial u_2}, \frac{\partial f_1}{\partial u_3}, \dots \\ \frac{\partial f_2}{\partial u_1}, \frac{\partial f_2}{\partial u_2}, \frac{\partial f_2}{\partial u_3}, \dots \\ \vdots \end{bmatrix} \quad (2.51)$$

becomes singular (*i.e.* local minima) making it possible to carry out iterations until the sum of squares is below a specified tolerance of (typically) $1e-14$. This generally results in volume fractions that are correct to 5 or 6 significant figures.

Because of the large number of equations generated when even a small lattice is used, it is a challenge to devise a rapid solution scheme (*i.e.* 25 layers by 10 radials with 3 components gives 750 variables). It is common to solve a set of non-linear equations using Newton's method, or some form of modified Newton's method [Scales, 1985]. Whatever method is used, it is necessary to have some gradient information about the functions being solved. This is a very costly step if the gradient is evaluated numerically each iteration, since finite differences must be carried out for each function with respect to each iteration variable. In the class of

methods known as Quasi-Newton methods, the information obtained from a previous iteration is used to update the Jacobian (or Hessian) matrix so that the solution is more rapid.

In a typical Newton iteration, it is necessary to solve a large set of linear equations in order to calculate the search direction. This can sometimes be avoided when the Jacobian is tri-diagonal or has some specific symmetry. Decompositions might also be used to speed up the solution of the linear equations. With a large set of equations, the solution by Gaussian reduction can be the single most time consuming step. It is therefore often desirable to approximate the Jacobian for the first iteration, invert the matrix and obtain the search direction by direct multiplication. If an updated inverse is then calculated, the method will proceed rapidly toward the solution, even for the case of several hundred variables.

An algorithm having these time saving features is known as Broyden's rank-one method, and uses an update formula developed to improve the inverse Jacobian [Broyden, 1965]. An outline of the algorithm is as follows [Scales, 1985; p.128]:

1. Input \mathbf{u} , TOL
2. Approximate \mathbf{J} , and calculate \mathbf{J}^{-1}
3. Calculate $\Delta\mathbf{u} = -\mathbf{J}^{-1} * \mathbf{f}$
4. Compute α {so that $F(\mathbf{u} + \alpha * \Delta\mathbf{u}) < F(\mathbf{u})$ }
5. Set $\mathbf{u} = \mathbf{u} + \alpha * \Delta\mathbf{u}$
6. Compute \mathbf{Q}^J
7. Set $\mathbf{J}^{-1} = \mathbf{J}^{-1} + \mathbf{Q}^J$
8. Repeat steps 3 to 7 until $F < \text{TOL}$

In this algorithm, \mathbf{J} and \mathbf{J}^{-1} are approximations to the Jacobian and its inverse respectively. The calculation of α is done using a line search algorithm, in order to minimize the sum of squares

(approximately) in the search direction, and the matrix Q^J is calculated using Broyden's update formula:

$$Q^J = -\frac{(J^{-1}\Delta f - \Delta u)\Delta u^T J^{-1}}{\Delta u^T J^{-1}\Delta f} \quad (2.52)$$

Broyden's update formula comes from an extension of the secant method to multiple dimensions. In a one dimensional secant method, the finite difference approximation of the first derivative is replaced by the difference in the last two function evaluations over the difference in the last two values of the independent variable:

$$f'_{k+1} = \frac{f(u_{k-1}) - f(u_k)}{u_{k-1} - u_k} \quad (2.53)$$

This saves time if the extra function evaluations needed for finite differences are costly. The method can be extended to multiple dimensions, where the analogous model becomes:

$$f(u_k) = f(u_{k-1}) + J_{k+1}(u_k - u_{k-1}) \quad (2.54)$$

In multiple dimensions Equation (2.54) does not provide enough information to specify J precisely, because as long as Δu is not equal to zero, a large number of matrices J can satisfy Equation (2.54) [Dennis, 1983]. Broyden's method, however, generates J (the Jacobian approximation) by minimizing the change in the model while still satisfying Equation (2.54). Broyden's [1965] Jacobian update formula is given by

$$J_{k+1} = J_k + \frac{(\Delta f - J_k \Delta u)\Delta u^T}{\Delta u^T \Delta u} \quad (2.55)$$

which, when rearranged using Householder's formula [Dennis, 1983], gives the inverse update formula shown as Equation (2.52).

The search direction that is generated using Newton's method may not always reduce the sum of squares if the full step is taken. When attempting to solve a set of nonlinear equations by minimizing their sum of squares, it can be shown that the Newton direction should always produce a descent direction [Dennis, 1983], as long as a local minimum is not encountered. For this reason it is often desirable to take a fractional step in the search direction. The subroutine LINSRCH carries out a univariate minimization, in which the sum of squares is minimized with respect to the fraction, α , using the current search direction. Brent [1973] first published the algorithm.

The minimization interval of the function is specified to be between XI and XF assuming a unimodal function. Brent's [1973] subroutine uses a hybrid method, which combines a quadratic interpolation with "Golden Section" search. If the predicted position of the next point found by quadratic interpolation does not meet several criteria, such as falling between the last two lowest points, being non-zero, and not being too small or large a step, then a "Golden Section" step is taken. This is a fractional step toward the lower of the points. By combining the two methods, the algorithm is guaranteed to find the minimum of a function as long as one exists on the search interval.

In practice, the fraction α is chosen to lie between 0.001 and 0.7 and the search is allowed to proceed for a maximum number of interpolations, usually 5 to 7 before accepting the change in u of $\alpha \cdot \Delta u$. There is also a termination criterion based on the width of the search interval (which narrows as it proceeds) and the distance of the next interpolation from the interval edges.

Our algorithm is somewhat simplistic, which warrants some discussion given the complex problem to which it has been applied. The use of a line search helps to make the

solution method more global. However, convergence is not assured when a poor initial guess of the starting values is made. An increase in the sum of squares can be observed in cases where a poor search direction is generated by the Jacobian update, since the line search terminates after a fixed number of iterations. In general though, the solution will wander uphill slightly under such conditions and then make large steps downhill from the new position.

2.3 Evaluation of Model Parameters

2.3.1 Scaling the Lattice Model

It can be difficult to describe the results of lattice-model calculations in terms of real dimensions. This is due to the fact that a real molecule, with many degrees of conformational freedom and non-uniform shape, is being described by a set of contiguous lattice sites, which have a fixed volume and simplistic spatial arrangement. When a solution of different types of molecules is being described by a single lattice geometry, the lattice scaling is made even more difficult by the desire to find a lattice size that simultaneously describes well the different types of molecules. In this study, the physical properties of the system that require scaling include the polymer chain length, the surface density of polymer and the size of the particle (protein) interacting with the polymer. The lattice analogs of these properties are summarized in Table 2.1.

There are different methods of scaling, depending on the lattice model chosen. In the original work by Flory dealing with a bulk solution of polymer, the dimensions of a lattice unit were never required. Polymer chain length in the lattice was scaled against the size of the solvent molecules. The number of segments in a polymer chain was then calculated as the ratio of the polymer to solvent molar volume [Flory, 1953]. In more complex lattice models, such as

ours, where concentration gradients exist or chains are tethered to a specific location, more complicated scaling techniques are necessary.

Table 2.1: Experimental properties that require direct comparison with lattice values.

Property	Lattice Value	Experimental Value
Chain Length	N (segments)	r (monomers)
Surface Density	θ (monolayers)	Γ (mg/m ²)
Particle Size	R (lattice units)	R_g (Å)

2.3.1.1 Lattice Unit and Chain Length

Meaningful comparison of a lattice chain to a real chain is possible by making use of two chain properties, the radius of gyration and the contour length. Equating these two properties between lattice chains and real chains allows one to calculate the appropriate dimension for one lattice unit and the number of lattice segments N corresponding to a chain of a given molecular weight. In experimental systems, the radius of gyration is given by

$$R_g = \alpha M^{1/2} = \alpha (r M_m)^{1/2} \quad (2.56)$$

where α is an experimentally determined parameter and M is the polymer molecular weight, also given by the number of monomers r multiplied by the monomer molecular weight M_m [Fleer et al., 1993].

For chains described using a random-walk model, the radius of gyration is given by

$$R_g = p N_B l^2 \quad (2.57)$$

where N_B is the number of bonds per chain ($N_B = r - 1$), l is the bond length and p is the persistence (a measure of the chain stiffness). If we treat the smallest step in the random-walk as a monomer, then equating Equations (2.56) and (2.57) give a simple expression for p based on experiment

$$p = \frac{a^2 r M_m}{N_B l^2} \approx \frac{a^2 M_m}{l^2} \quad (2.58)$$

since at large N_B , $r / N_B \approx 1$. The persistence p_L can also be calculated directly by the for lattice model

$$p_L = \frac{1}{6} \left(\frac{1 + z^{-1}}{1 - z^{-1}} \right) \quad (2.59)$$

where z is the lattice coordination number [Fleer et al., 1993]. Here p_L is a consequence of the lattice geometry only.

Equating the random-walk radius of gyration (Equation (2.57)) for a real chain with that for a lattice chain gives

$$p N_B l^2 = p_L N_{LB} l_L^2 \quad (2.60)$$

where N_{LB} is the number of lattice bonds ($N_{LB} = N - 1$) and l_L is the segment length, or length of one lattice unit. Similarly, equating the fully extended chain length (contour length) of both chains gives:

$$N_B l = N_{LB} l_L \quad (2.61)$$

Combining Equations (2.60) and (2.61) and substituting for the persistence values (Equations (2.58) and (2.59)) of each chain then allows us to calculate the dimensions of the lattice unit based on experimental parameters

$$l_L = \frac{\alpha^2 M_m}{lp_L} \quad (2.62)$$

Finally, substituting this result back into Equation (2.61) allows us to calculate the lattice chain length N .

For example, polyethylene has an $M_m = 28$, $\alpha = 0.434$ nm [Fleer et al., 1993], and $l = 0.25$ nm; in a cubic lattice, $p_L = 0.233$. This gives $l_L = 0.9$ nm and a chain consisting of 100 monomers should have a number of lattice segments N equal to about 28. In cases where the monomers are large, or the chains are very stiff, this method may break down. The resulting lattice unit sizes can become too large to allow simultaneous scaling of the solvent size and polymer size.

A second method of scaling the chain length is based on rotational isomeric state theory [Flory, 1969]. Cosgrove and Ryan [1990b] have scaled their results based on work by Cohen Stuart [1980], which relates N_B to N_{LB} by:

$$N_B / N_{LB} = \log \left(\frac{z}{z_p} \right) \quad (2.63)$$

Here z is the lattice coordination number and z_p is a characteristic constant related to the chain persistence.

It is also possible to arbitrarily specify the dimension of a lattice unit. Baskir et al. [1989a; 1989b; 1987] chose a lattice unit of 4Å to model polyethylene oxide and Dextran, and

scaled the number of chain segments equal to the degree of polymerization. Using this simple approach, they obtained good quantitative comparison with aqueous two-phase partitioning data for various globular proteins.

2.3.1.2 Polymer Surface Concentration

Once a lattice unit is chosen and a lattice chain length defined, the polymer surface density can be calculated. However, due to the limitations imposed by treating real chains as segments in an ideal lattice, comparing lattice graft densities to experiment is not trivial. In the simplest case, a lattice chain can be considered to occupy a real volume equivalent to that of the lattice sites it occupies. In this case, the surface density Γ (mg/m^2) is related to the lattice analog θ by

$$\Gamma = \frac{m\theta}{N_{LB}l_L^2} \quad (2.64)$$

where m (mg/chain) is the mass of one polymer chain. In comparison to experiment, however, Equation (2.64) is not always satisfied. For example, if a lattice unit of 1.0 nm is used (100 \AA^2 per surface site) and it is experimentally determined that the chains are grafted with 100 \AA^2 per chain, the lattice model requires that the grafting density σ be unity, indicating no solvent is present in the lattice model. Clearly this is unrealistic, so at high surface densities it may be necessary to arbitrarily reduce the value of l_L in order to reduce σ . If l_L is made too small, however, the lattice chains can have an unrealistic density. This occurs because, although the contour length is matched, the cross-sectional area of the lattice chains is not scaled properly.

The problem of matching lattice chains exactly to the volume of real chains can be avoided by scaling the total number of grafted segments based on constant polymer density.

Cosgrove and Ryan [1990b] scaled their lattice model in order to compare calculated polymer density distributions of end-grafted polyethylene oxide (PEO) with those measured using small-angle neutron scattering (SANS). They used the true polymer density $\rho_{polymer}$ and the lattice unit to calculate a monolayer coverage

$$A_{mon} = l_L \rho_{polymer} \quad (2.65)$$

in units of (mg/m²). It then follows that the experimental coverage is equal to the monolayer capacity multiplied by the number of equivalent monolayers θ of segments in the lattice

$$\Gamma = A_{mon} \theta \quad (2.66)$$

Cosgrove and Ryan's method gave very good quantitative agreement between experiment and model calculations. They state, however, that the method may break down at high surface overage, or for very high molecular weight chains.

2.3.1.3 Particle Size

In order to model a particle interacting with the end-grafted polymer, a third component has been added to the lattice with a specific geometry. In the cylindrical lattice the most convenient particle geometry is that of a small cylinder (usually with length set equal to radius) in which the volume fraction of particle is specified to be very high ($\Phi_p > 0.99$). The radius of the cylinder then allows scaling to the relative size of real molecules, such as a protein with a specific molecular weight. Thus, we assume that a particle with a given radius has about the same interaction with the polymer as a protein of the same radius would. This seems reasonable because, in terms of particle dimensions, our calculations show that the radius has the dominant effect on brush-particle interaction energies.

Tyn and Gusek [1990] cite several different empirical correlations for estimating protein diffusion coefficients using protein molecular weight or radius. By coupling two of these methods it is possible to derive an equation, which directly relates molecular weight to radius. For example, based on the Stokes-Einstein equation, Polson developed a correlation relating the diffusion coefficient of a protein to its molecular weight

$$D = A / M^{1/3} \quad (2.67)$$

where A is a constant and M is the protein molecular weight. Tyn and Gusek proposed the following correlation between D and the radius of gyration R_g of the protein

$$D = B / R_g \quad (2.68)$$

where B is a constant. Equating these two expressions gives

$$M = (CR_g)^3 \quad (2.69)$$

where C is a constant that can be fit over a molecular weight range of interest.

For proteins up to about $M = 150$ kDa, a non-linear curve fit was carried out using Equation (2.69). Figure 2.4 shows that a very good fit was obtained, giving a value of $C = 1.50 \pm 0.02$ (kDa^{1/3}/Å), allowing direct scaling of model particles to real molecular weights.

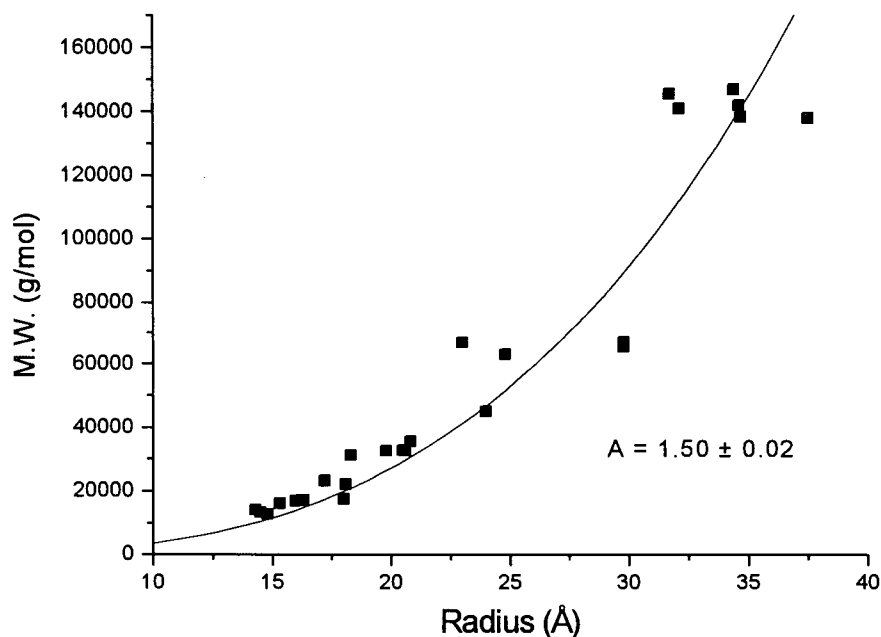


Figure 2.4: Non-linear curve fit of data taken from Tyn and Gusek [1990] for use scaling particle size to protein molecular weight.

2.3.2 Measuring Interaction Parameters

The Flory interaction parameter χ_{ij} is based on the statistical mechanical quantity known as the interchange energy $\Delta\omega_{ij}$. The interchange energy is a physico-chemical property, which can and has been measured experimentally. Several techniques can be used to measure chemical potentials of solvent and/or polymer including differential-vapour-pressure, osmometry and low-angle laser-light-scattering (LALLS) [Rathbone et al., 1990; Haynes *et al.*, 1989]. Based on predictions of the chemical potential using our model, interaction parameters may then be calculated from the experimental results.

2.3.2.1 Differential-Vapour-Pressure and Osmometry

To fix ideas, consider a binary mixture of solvent (1) and polymer (2). For such a mixture, the derivative of the Gibbs' energy of mixing from Flory-Huggins theory taken with respect to the number of solvent molecules $[\partial G_m / \partial n_1]_{T,P,n_2}$ gives the solvent chemical potential:

$$\mu_1 - \mu_1^o = RT \left[\ln(1 - \Phi_2) + \Phi_2 \left(1 - \frac{1}{N_2} \right) + \chi_{12} \Phi_2^2 \right] \quad (2.70)$$

The chemical potential of a component is related to its activity by

$$\mu_1 - \mu_1^o = RT \ln a_1 \quad (2.71)$$

where a_1 is the activity of the solvent. In the differential-vapour-pressure experiment, a_1 is related to the difference in the vapour pressure between pure solvent and the polymer-containing solvent ΔP by

$$a_1 = \frac{(P_1^o - \Delta P)}{P_1^o} \quad (2.72)$$

where P_1^o is the vapour pressure of pure solvent. If P_1^o is low, the vapour phase can be treated as ideal. Haynes et al. [1989] give a detailed description of the experimental technique and apparatus used for differential-vapour-pressure measurement. Substitution of Equations (2.70) and (2.72) into Equation (2.71) with subsequent rearrangement allows direct calculation of χ_{12} for a given concentration of polymer. It is useful to note that the polymer volume fraction Φ_2 is equal to the weight concentration c_2 (g/mL) multiplied by the partial specific volume of the polymer in solution \bar{v}_2 (mL/g).

Osmotic pressure measurements can be used in the same manner as vapour pressure measurements to calculate interaction parameters. The osmotic pressure of the solvent

$$\Pi = \frac{(\mu_1 - \mu_1^o)}{V_1} \quad (2.73)$$

is related directly to the solvent chemical potential and the molar volume of the solvent V_1 .

2.3.2.2 Low-Angle Laser-Light-Scattering (LALLS)

A more direct measure of nonideal intermolecular interaction in solution can be gained from the light-scattering properties of its molecules. Consider once again a dilute binary polymer solution of solvent (1) and polymer (2). The osmotic virial expansion of McMillan and Mayer [1945] expresses the solvent chemical potential μ_1 in such a solution exactly in terms of an expansion in polymer concentration c_2 (g/mL)

$$\mu_1 - \mu_1^o = -RTV_1 \left[\frac{c_2}{M_{w2}} + A_{22}c_2^2 + A_{222}c_2^3 + \dots \right] \quad (2.74)$$

where V_1 is the molar volume of the solvent, M_{w2} is the weight-averaged molecular weight of the polymer, and A_{22} (mL-mol/g²) and A_{222} (mL²-mol/g³) are the osmotic second and third virial coefficients, respectively. Osmotic virial coefficients are dependent only on temperature and the nature of the solute and solvent at normal pressures. Statistical mechanics suggests that A_{22} accounts for two-body interactions in solution and A_{222} accounts for three-body interactions. At low enough concentrations it is possible to truncate the virial expansion after the second-order terms since higher-order interactions will be approximately negligible.

For dilute polymer solutions, Equation (2.74) can be truncated after the second virial coefficient term without loss in accuracy. The solvent chemical potential μ_1 can then be determined as a function of polymer concentration if M_{w2} and A_{22} are known. The values of both of these constants can be determined by low-angle laser-light scattering (LALLS), which measures the light-scattering properties of a solute (polymer) molecule whose size is small compared to the wavelength of the incident light (*i.e.*, Rayleigh scattering). A detailed description of the technique and associated theory, which is not of direct relevance to this thesis, is provided by Rathbone *et al.* [1990].

Equating the right-hand side of Equation (2.74), truncated after the second virial coefficient term, with that of Equation (2.70), allows regression of χ_{12} from LALLS data. One advantage of the LALLS technique over the two colligative methods (vapour-pressure and membrane osmometry) is that it is easily extended to multicomponent measurements, allowing determination of χ_{ij} parameters characterizing the interaction of solute i with solute j (*i.e.*, polymer i with protein j). The theory used to calculate χ_{ij} parameters from LALLS data for a ternary aqueous polymer solution is that derived in Haynes *et al.* [1993]. The principle equations relating the osmotic second virial coefficients to the Flory interaction parameters are

$$A_{ii} = \left(\frac{1}{2} - \chi_{1i} \right) \frac{\bar{v}_i^2}{V_1}; \quad i = 2, 3 \quad (2.75)$$

$$A_{23} = \left(1 + \chi_{23} - \chi_{12} - \chi_{13} \right) \frac{\bar{v}_2 \bar{v}_3}{V_1} \quad (2.76)$$

where \bar{v}_i is the partial specific volume of component i in solution.

Regrettably, χ_{ij} data are extremely rare for aqueous polymer systems. LALLS data (as well as vapour-pressure and membrane osmometry data to a lesser extent) are available for a few aqueous solutions containing polymer and protein [Haynes *et al.*, 1993; Rathbone *et al.*, 1990; King *et al.*, 1988]. Equations (2.70) to (2.76) are therefore valuable because they allow determination of the realistic range of χ_{ij} values we would expect to observe in our systems of interest; namely, the interaction of a protein with a grafted-polymer brush, both of which are solvated by water.

Flory interaction parameters are shown in Table 2.2 to Table 2.6 for a number of polymers and proteins regressed from osmotic second virial coefficients measured by LALLS [Haynes *et al.*, 1993]. All polymer-solvent and protein-solvent interaction parameters (Table 2.1 to Table 2.5) are significantly positive indicating an unfavourable enthalpic interaction between the solute and water. In a very good solvent, χ_{12} is negative or very close to zero (athermal). In cases where χ_{12} is positive, solvation can only result because of a large increase in entropy on mixing. Most water-soluble polymers have χ_{12} values close to the theoretical point at which phase separation will occur for polymer of infinite molecular weight ($\chi_{12} = 0.5$). Thus, decreased solvent quality (increased χ_{12}) in these cases can lead to phase separation of polymer or precipitation of proteins. Interaction parameters χ_{23} shown in Table 2.6 indicate that there is a very weak enthalpic interaction between the polymers (PEG or dextran) and proteins. Bovine serum albumin and lysozyme appear to have a very weak attraction to the polymers while α -Chymotrypsin has a very weak repulsion.

Table 2.2: Polymer-solvent interaction parameters for PEG and Dextran in water at 25 °C calculated from light-scattering data of Haynes et al. [1993].

Polymer	M_w (g/mol)	$A_{ii} \times 10^4$ (mL-mol/g ²)	χ_{12}
PEG 3350	3860	36.3	0.45
PEG 8000	11700	30.3	0.45
Dextran T-70	10100	4.0	0.49
Dextran T-500	43400	1.3	0.50

Table 2.3: Protein-solvent interaction parameters calculated from light-scattering data for bovine serum albumin (BSA) in water at 25 °C.

Buffer Salt (or Salt)	Salt Conc. (mol/kg)	Ionic Strength (mol/kg)	pH	$A_{ii} \times 10^4$ (mL-mol/g ²)	χ_{12}
Potassium Phosphate	----	0.075	7.0	8.3	0.47
	----	0.14	7.0	6.1	0.48
	----	0.28	7.0	3.7	0.49
	----	0.4	7.0	2.5	0.49
	----	0.5	7.0	2.4	0.49
KCl	0.05	----	7	8.7	0.47
NaCl	0.05	----	7	8.9	0.47

Table 2.4: Protein-solvent interaction parameters calculated from light-scattering data for lysozyme in water at 25 °C.

Buffer Salt (or Salt)	Salt Conc. (mol/kg)	Ionic Strength (mol/kg)	pH	$A_{ii} \times 10^4$ (mL-mol/g ²)	χ_{12}
Potassium Phosphate	----	0.075	7.0	4.1	0.49
	----	0.14	7.0	-2.5	0.51
	----	0.28	7.0	-7.2	0.53
	----	0.4	7.0	-10.0	0.54
	----	0.5	7.0	-10.0	0.54
KCl	0.05	----	7	5.8	0.48
NaCl	0.05	----	7	6.1	0.48

Table 2.5: Protein-solvent interaction parameters calculated from light-scattering data for α -chymotrypsin in water at 25 °C.

Buffer Salt (or Salt)	Salt Conc. (mol/kg)	Ionic Strength (mol/kg)	pH	$A_{ii} \times 10^4$ (mL-mol/g ²)	χ_{12}
Potassium Phosphate	----	0.075	7.0	-26.0	0.59
	----	0.14	7.0	-13.0	0.55
	----	0.28	7.0	-4.9	0.52
	----	0.4	7.0	-3.5	0.51
	----	0.5	7.0	-2.8	0.51
KCl	0.05	----	7	-13.0	0.55
NaCl	0.05	----	7	-13.0	0.55

Table 2.6: Protein-polymer interaction parameters χ_{23} calculated from light-scattering data in potassium phosphate buffer at 25 °C.

Protein	Polymer		Dextran	Dextran
	PEG 3350	PEG 8000	T-70	T-500
BSA				
pH 7: 50mM buffer	-0.07	-0.08	-0.04	-0.04
pH 7: 100mM buffer	-0.06	-0.06	-0.03	-0.02
Lysozyme				
pH 7: 50mM buffer	-0.06	-0.06	-0.02	-0.02
pH 7: 100mM buffer	-0.04	-0.04	0.00	0.00
α -Chymotrypsin				
pH 7: 50mM buffer	0.06	0.06	0.10	0.10
pH 7: 100mM buffer	0.03	0.03	0.07	0.07

3 Isolated Terminally-Attached Chains

3.1 Motivation

Before proceeding to our analysis of the interaction of a particle (protein) with a brush, it is useful to gain a better understanding of how grafted-chain conformation is altered by the movement of an impenetrable particle or surface into its volume space. The only meaningful study is that of Subramanian *et al.* [1995], who modeled the compression of a single grafted polymer chain using scaling theory (see Section 3.2).

In this chapter, we apply our SCF model to the calculation of grafted-chain configurations and energetics during compression by a cylinder of radius R . A schematic of the system under investigation showing all characteristic dimensions is shown in Figure 3.1. Polymer segment density distributions and compression energies have been calculated in the cylindrical lattice for mushrooms of various chain lengths compressed by discs of varying radius.

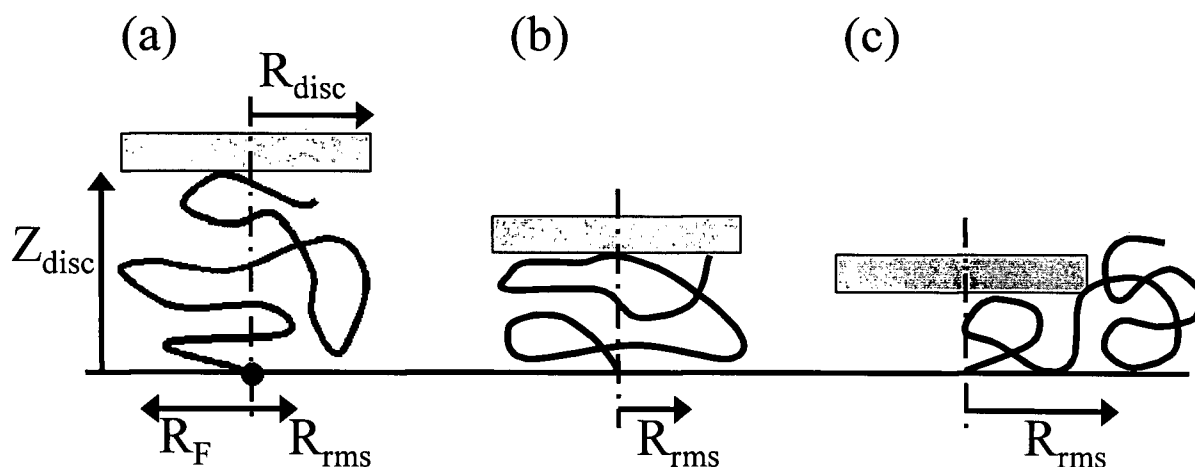


Figure 3.1 Schematic diagram of a single end-grafted chain in (a) uncompressed (b) compressed, and (c) escaped states. The chain grafting point indicated by \bullet is at lattice position $(z=0, r=0)$. Characteristic dimensions include: (i) disc position, Z_{disc} , (ii) disc radius, R_{disc} (iii) r.m.s. radius of segments from cylinder axis, R_{rms} and, (iv) Flory radius, R_F .

3.2 Scaling Theory of Mushroom Compression

Subramanian *et al.* [1995] model the compression of a single polymer chain by a finite disc of radius R_{disc} using scaling theory. They have studied the case where the disc is centered over the grafting point of the chain, and as a result the chain cannot fully escape under compression. Under such conditions, they predict that the chain will undergo pure compression until a point is reached at which a first-order transition occurs, where the free end of the chain suddenly escapes from under the disc. The scaling development is briefly described here.

Subramanian *et al.* [1995] consider the grafted chain to be a mushroom-type coil of radius $R_g = lN^{3/5}$ which can be modeled as a string of blobs each of diameter D under compression, where D is also the distance of the disc from the grafting surface. The number of blobs B (each with N_B segments) in the chain are calculated from the scaling result that the blob radius is given by $D = lN_B^{3/5}$ and thus $B = N / N_B = N(l/D)^{5/3}$. The formation of each blob is associated with energy kT and the total energy associated with chain compression is thus $A_{blob} = kTN(l/D)^{5/3}$.

Partial chain escape is predicted by the model at conditions where the chain can lower its energy by stretching a tether to the edge of the disc and forming a larger escaped blob outside the disc radius. If the tether contains B_t blobs, the tether energy based on unperturbed blob formation is kTB_t . However, the tether may stretch to allow partial chain escape from the disc radius R_{disc} , particularly when R_{disc} is larger than the two dimensional radius of the string of blobs in the tether, given by $R_{2D,tether} = DB_t^{3/4}$. The stretching energy required for this process is given by scaling arguments to be $kT(R_{disc}/R_t)^4$. The total free energy of the mushroom may then be written as $A_{Total} = kT(B_t + (R_{disc}/D)^4 B_t^{-3})$.

The minimum total free energy with respect to the number of blobs in the tether is found when $B_t = 3^{1/4}(R_{disc}/D)$. Subramanian *et al.* [1995] equate this minimum total energy to the energy of the fully confined chain (*i.e.* no escape or stretching) to determine the critical point for chain escape, given by $D_c = (3^{1/2}/4^{2/3})N^{3/2}l^{5/2}/R_{disc}^{3/2}$. The two dimensional radius of the chain just before escape is therefore predicted to be $R_{2D} = D_c B^{3/4} = R_{disc}(R_g/R_{disc})^{5/8}$. From this expression, Subramanian *et al.* predicted that if the disc radius is greater than the free coil radius of gyration, there will be a jump in the chain radius upon escape that is analogous to a first-order transition. They also predict that there is an energy barrier to be overcome for chain escape to occur, which is equal to the energy required for the chain to stretch to the edge of the disc. This stretching energy is given by $kT(R_{disc}/R_{2D}(D_c))^4$ and can be significantly larger than kT .

Using similar scaling arguments Guffond *et al.* [1997] studied the compression of end-grafted mushrooms in a poor solvent by various flat discs and step-discs finding similar results for an escape transition. Williams and MacKintosh [1995] also studied the compression of mushrooms under curved surfaces and reported regimes of surface curvature resulting in an escape transition and an unconfined chain. They also investigated compression under irregular surfaces finding multiple-escape transitions.

3.3 Analysis of Mushroom Compression using Numerical SCF Theory

At low grafting density, the conformation of an end-grafted chain is based only on the impenetrable nature of the grafting surface and interactions of the chain with itself and solvent, assuming no other species are present. As mentioned previously (Chapter 1), de Gennes [1980] has shown that a single end-grafted chain in a good solvent forms a random coil, roughly in the

form of a half sphere, with a Flory radius of approximately $R_F \approx IN^{3/5}$. Thus, a chain of 100 segments will have a Flory radius of about 16 lattice units. The root-mean-squared distance of segments from the cylinder axis

$$R_{rms} = \left[\sum_r r^2 \frac{n(r)}{N} \right]^{1/2} \quad (3.1)$$

has also been calculated in this work in order to characterize the amount of spreading and escape a chain undergoes when compressed.

The fractional segment distribution in both the radial (r) and normal (z) directions is shown in Figure 3.2 for an end-grafted chain of 100 segments in a good solvent ($\chi_{12}=0$) under no compression. The Flory radius and R_{rms} of the coil as calculated in Equation (3.1) are also shown in Figure 3.2 for comparison. The number of segments in each radial $n(r)$ is calculated as

$$n(r) = \sum_z L(r) \Phi(z, r) \quad (3.2)$$

which is simply the volume fraction $\Phi_i(z, r)$ multiplied by the number of lattice sites L in the radial r summed over all layers. The fractional distribution was then computed by normalizing Equation (3.2) by the number of segments in the chain. In agreement with de Gennes' predictions, we find a maximum in the segment fraction a few layers from the surface in the normal direction. There is also a maximum in the segment fraction a few radials from the center. This is due to the fact that the inner radials have fewer lattice sites and can thus accommodate fewer segments despite having higher segment densities. The two curves approach zero at roughly the same distance, suggesting the chain forms roughly a half-sphere (or mushroom), spreading more in the radial than normal direction.

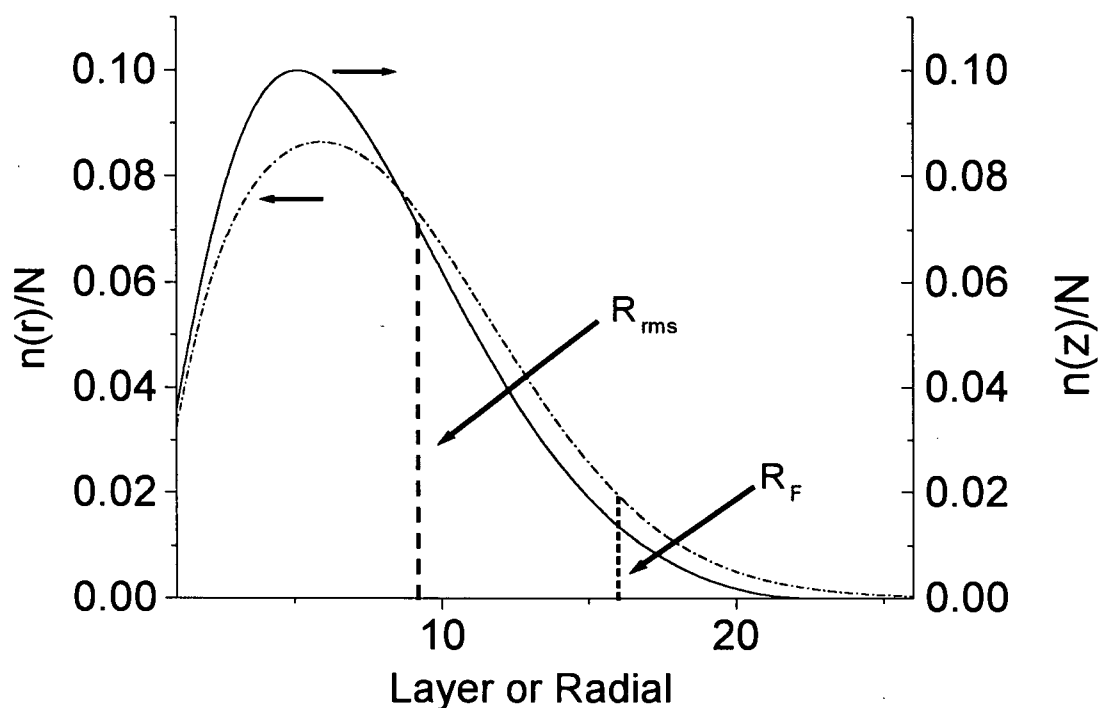


Figure 3.2 Fractional segment distribution of a single end-grafted chain in the radial (r) (dash-dot line) and normal (z) (solid line) directions with $N=100$ segments. Dashed line shows the root mean squared (rms) distance of segments from the center axis, R_{rms} , and dotted line shows the Flory radius, R_F .

The segment density profile of a single end-grafted chain is shown in Figure 3.3 (a). The density is highest at the point of grafting and drops off rapidly with distance from the surface. The graft density at (1,1) is about 0.4, which corresponds to slightly more than 1 segment in the π lattice sites of the first radial in layer 1. In Figure 3.3 (b), a disc of radius 20 with a thickness of 4 layers has been placed in layer 2 and the chain distribution around the disc is shown. It can be seen that the chain density becomes much higher in the outer radials ($r = 15-20$) of layer 1. A significant portion of the chain is escaped from under the disc and forms a smaller coil outside the edges of the disc.

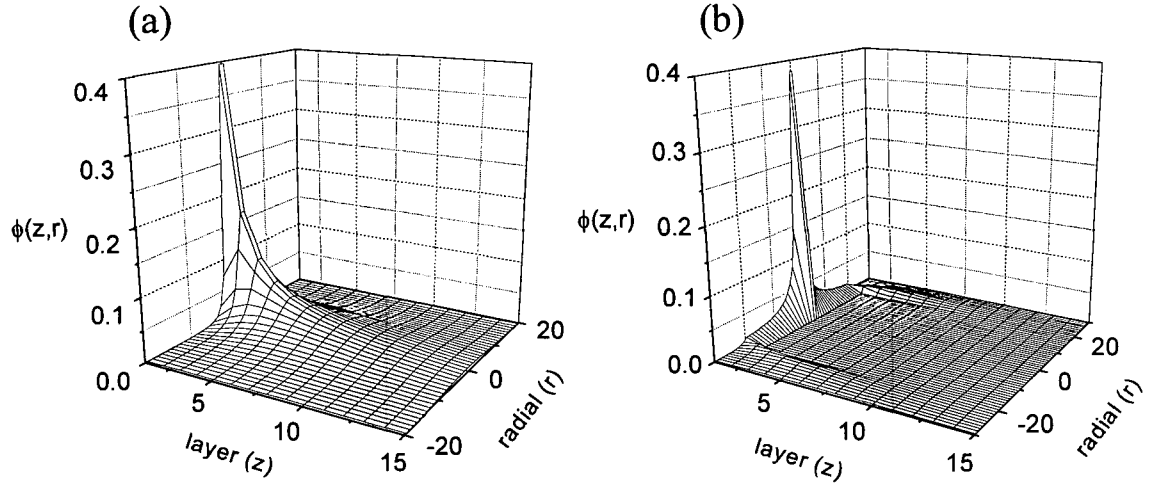


Figure 3.3 Segment density distribution of a single end-grafted chain with $N=100$. The chain is shown in (a) with no disc and in (b) with a disc of radius, $R_{\text{disc}}=20$, sitting in layer 2 compressing the mushroom.

The extent to which segments spread out in the radial direction under a compressing disc is proportional to R_{rms} (Equation (3.1)). The r.m.s. distance of segments from the center of the cylinder is shown in Figure 3.4 for a chain of 100 segments compressed by two discs of different diameters. In both curves, R_{rms} is the same under compression and decompression. We see no hysteresis in chain density profiles. The chain distribution is generated in our model using a step-weighted walk starting from position (1,1). If the disc is placed in layer 2 for example, we find only one self-consistent solution for the chain density distribution around that disc. An important feature of Figure 3.4 is that as the disc is made larger, more compression is required in order for chain escape. Consequently, the escape region is sharper due to the fact that more work is required to squeeze the chain to the edge of a larger disc. The escape of the chain under the disc of radius 20 is gradual, as seen by the solid line in Figure 3.4.

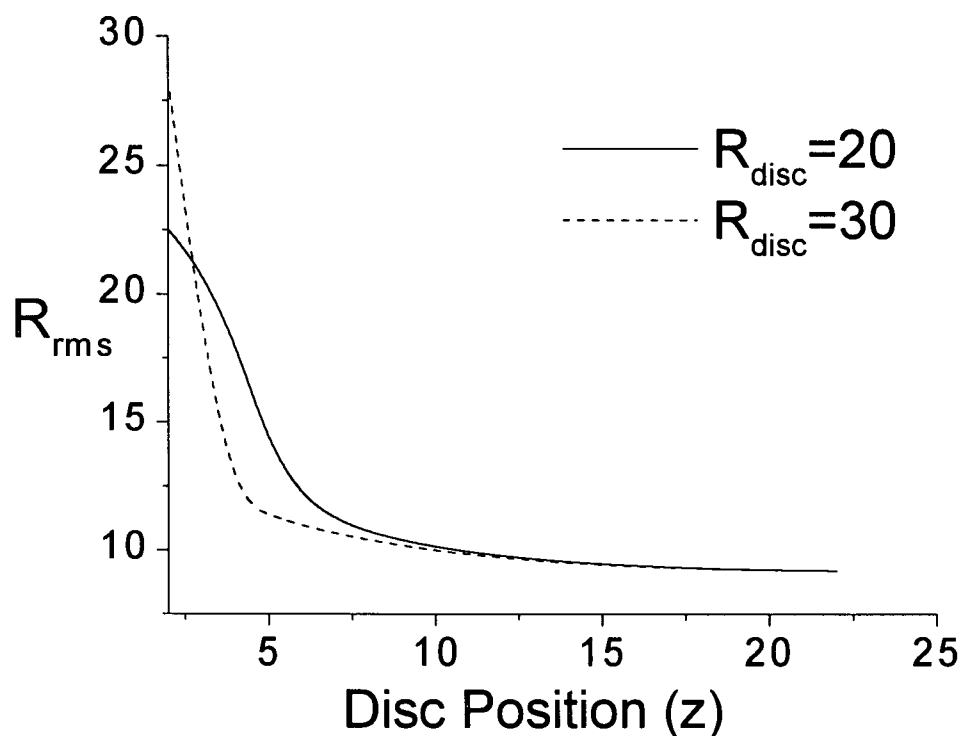


Figure 3.4 Root mean squared distance of segments from the center of the cylinder, R_{rms} , is shown as the disc compresses a mushroom with $N=100$. $R_{disc}=20$ (solid), $R_{disc}=30$ (dashed)

As discussed in section 3.2, Subramanian *et al.* [1995; 1996] report that for a disc larger than R_F , a first-order escape transition is found. They argue that this transition is associated with an energy required to stretch the compressed polymer chain to the edge of the disc. However, for such a system (a disc of radius 20 compressing a polymer of Flory radius *ca.* 16), we observe a gradual, reversible transition, which does not conform to a first-order escape transition. The scaling model of Subramanian *et al.* equates the calculated energy of two limiting cases in order to predict the compression at which a partially-escaped chain is in equilibrium with a compressed chain whose 2D Flory radius is close but not equal to the disc radius. The strongly compressed chain is modeled crudely as a string of blobs, each with energy kT , and the escaped chain is

modeled as a strongly stretched string of blobs (tether) with a fraction of the chain escaped. The fact that no such first-order transition is observed in our calculations suggests that information about the transition between these two states is lost in the scaling model, which is not altogether surprising given the assumptions that are made.

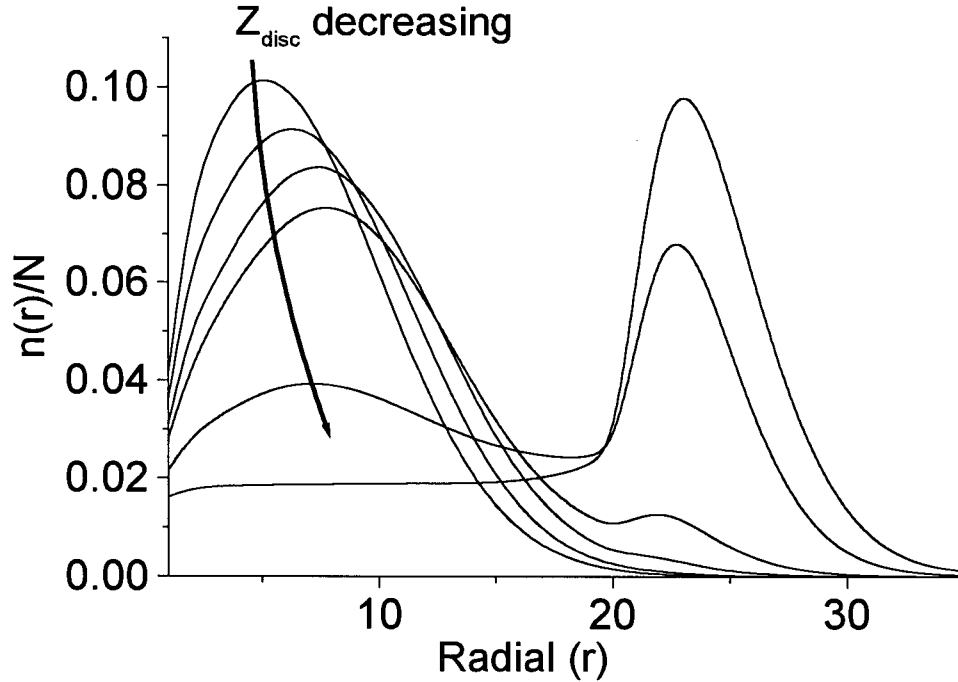


Figure 3.5 Fractional segment distribution in the radial direction as a mushroom with $N=75$ is compressed by a disc with $R_{disc}=20$. The curves represent the disc in positions of $z=16, 8, 5, 4, 3$, and 2 .

The segment fraction in each radial is shown in Figure 3.5 for a chain of $N=75$ segments compressed by a disc of radius $R_{disc}=20$. This set of curves shows the results when the disc is placed in layer 16, 8, 5, 4, 3, and 2. Initial chain escape can be seen when the disc is placed in layer 5, and the fraction of segments escaped increases significantly as the disc is moved in further. The R_{rms} curve for compression shown in Figure 3.6 looks very similar to the dashed line in Figure 3.4, but with a slightly less abrupt escape. It is interesting to note that with the disc

in layer 2, the number of covered segments in each radial is about 1.5. Within the mean field approximation, we could interpret this result as formation of a strongly stretched tether under the disc with a large escaped portion. As the chain becomes longer, the tether becomes more strongly stretched and at infinite chain length, would become fully stretched to its limit of one segment per radial under a finite sized disc.

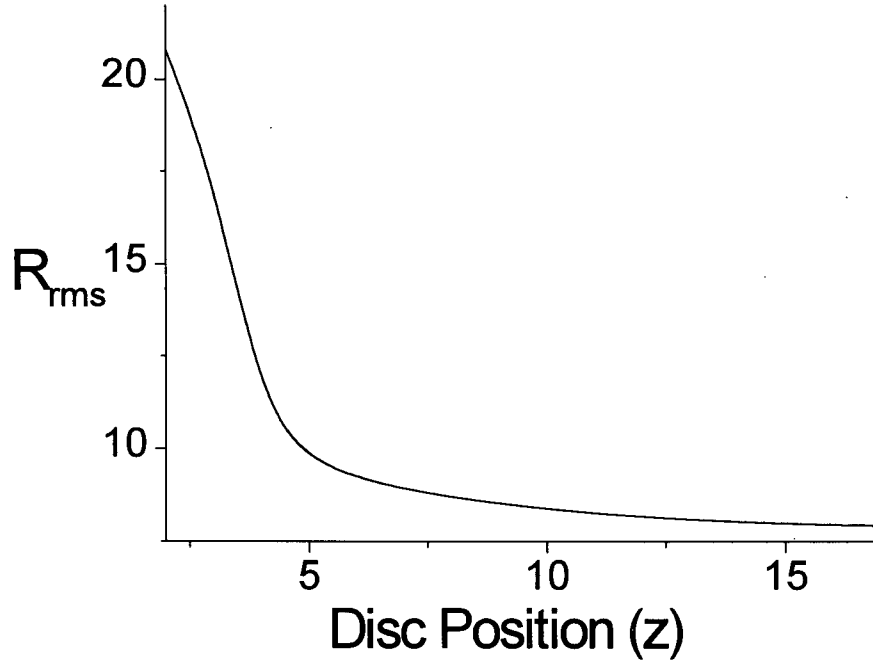


Figure 3.6 Root mean squared distance of segments from the center of the cylinder, R_{rms} , is shown as the disc of $R_{disc}=20$ compresses a mushroom with $N=75$.

The energetic cost of compressing a mushroom has been calculated based on the loss of conformational entropy. Figure 3.7 shows the compression energy for four different chain lengths. The curves represent compression under a disc of radius $R_{disc}=20$, and the chain lengths are $N=20$, 50, 100, and 200 segments. The curves are all monotonically increasing with compression and show no behavior indicating a first-order transition. Comparing the calculated energy curves for long chains with that for the $N=20$ chain, which cannot escape, shows that

chain escape is not accompanied by anomalies in A^{int} . The only clear difference between the systems is a shift of the curve to the right (higher disc positions) with increasing chain length, due to the increased excluded volume repulsion of the compressed chain. For the longer chains, $N=50$, $N=100$ and $N=200$, it can be seen that portions of the energy curves coincide at high compression. The energy curves for $N=50$ and $N=100$ overlap on the $N=200$ curve at a point where the shorter chains have just started to escape. Further compression therefore involves only the work of compressing the polymer tether, which is independent of chain length.

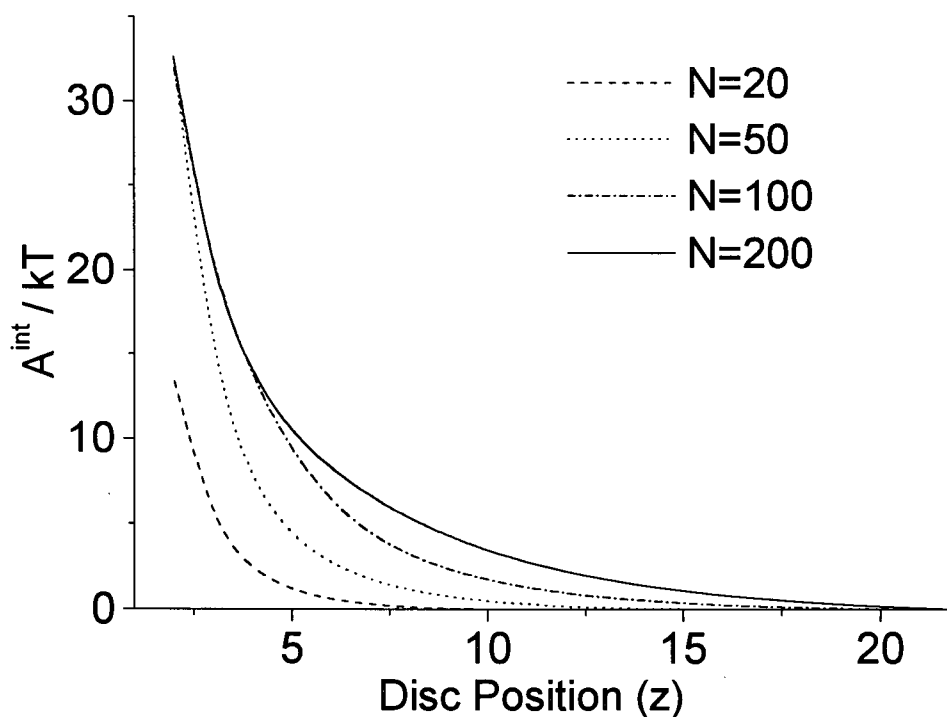


Figure 3.7 Energy required to compress a mushroom with a disc of radius, $R_{disc}=20$, for several chain lengths: $N=20$ (dashed), $N=50$ (dotted), $N=100$ (dot-dash), $N=200$ (solid)

In order to investigate the chain escape further, chain length was varied under a fixed disc of radius $R_{disc}=20$. The disc extended from layer 3 to $z=Z_{max}$. Figure 3.8 shows the fraction of segments covered by the disc (dotted) and the fraction of segments escaped (solid) from under it.

Again, a smooth curve is seen with no discontinuities that would indicate a first-order transition. The onset of escape occurs at just over 50 segments. As a final test for stability of the compressed chain, the chemical potential of the grafted chain was calculated for various chain lengths under a fixed disc and is shown in Figure 3.9 for a chain of $N = 80$. Conditions were the same as in Figure 3.8. In the binary mixture under consideration (1=solvent, 2=grafted-chain), phase instability will occur if $(\delta\mu_2/\delta n_2)_{T,\mu_1,\underline{y}} < 0$ [Prausnitz *et al.*, 1986]. However, $(\delta\mu_2/\delta n_2)_{T,\mu_1,\underline{y}}$ remains positive as shown in Figure 3.10 for all conditions (*i.e.* chain length and escaped fractions) investigated in Figure 3.8, providing more thermodynamically rigorous proof that although chain escape occurs, it does not involve a first-order phase transition.

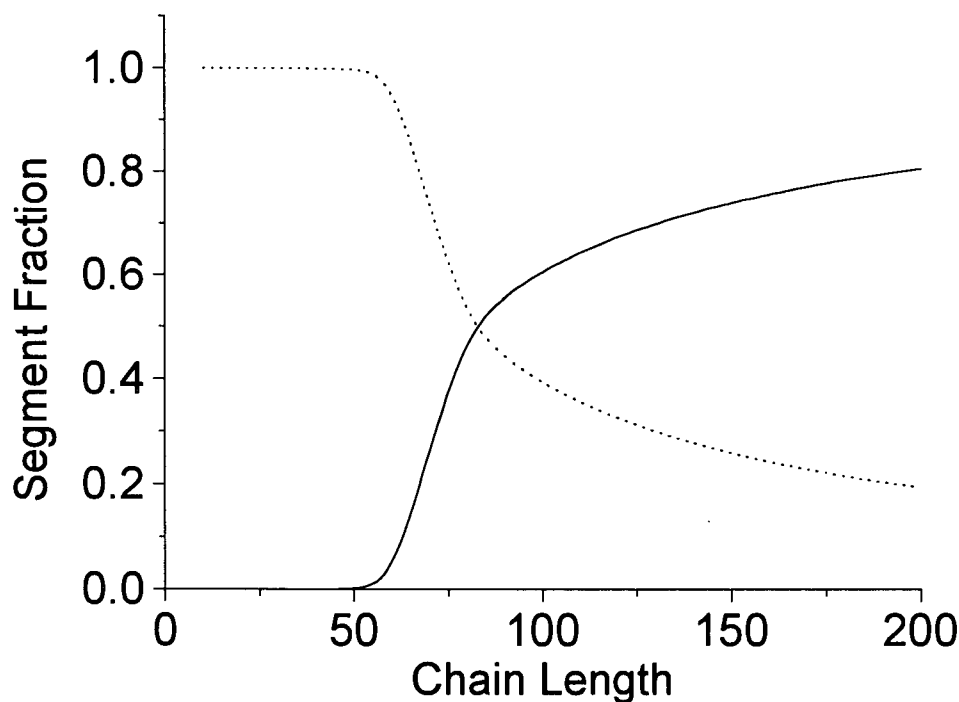


Figure 3.8 Fraction of segments covered (dotted) and escaped (solid) from under a stationary disc of radius 20, extending from $z=3$ to the end of the cylinder (Z_{\max}), as chain length is varied.

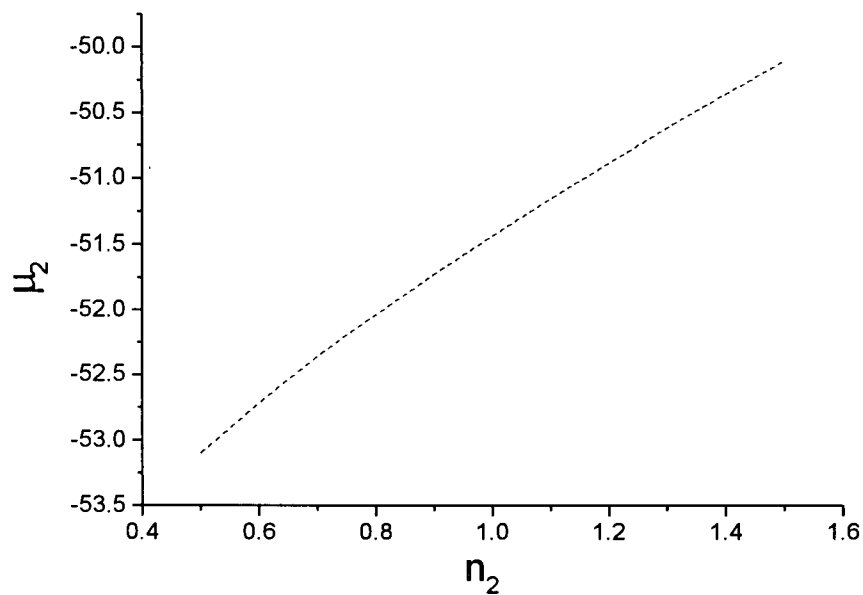


Figure 3.9 Chemical potential of a single end-grafted chain under a stationary disc of radius 20, that extends from $z=3$ to the end of the cylinder (Z_{\max}), as a function of the number of grafted chains.

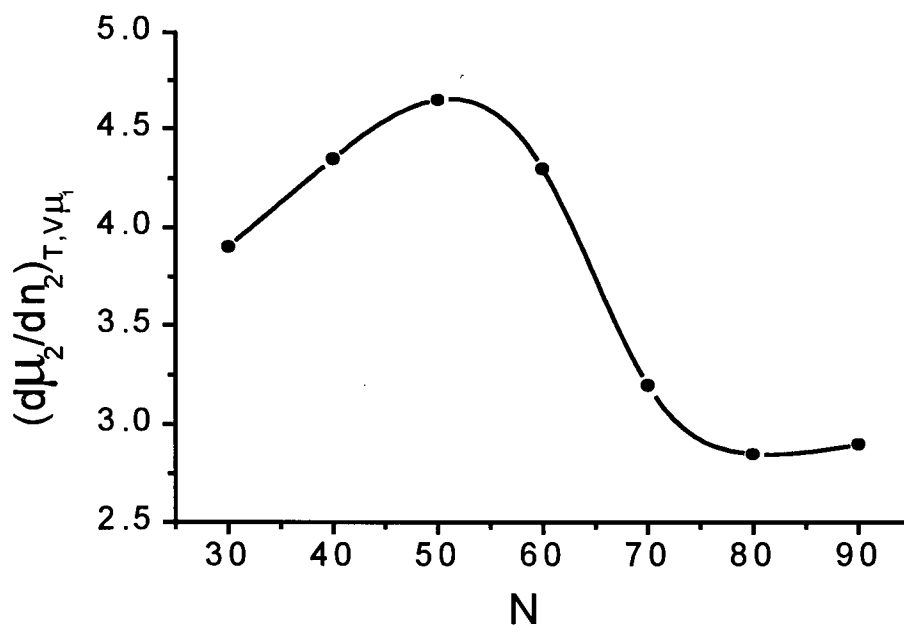


Figure 3.10 The change in chemical potential with respect to the number of grafted chains (at $n_{\text{chain}} = 1$) as a function of chain length. This value always remains positive indicating stability against phase separation.

3.4 Summary

The compression of a single end-grafted chain by a disc of finite radius was investigated using numerical SCF theory. Chain segment distributions for uncompressed chains (mushrooms) are consistent with results predicted by de Gennes [1980]. However, in contrast to more recent work using a model based on scaling theory [Subramanian *et al.* 1995; 1996] we find no first-order escape transition with hysteresis when a chain is compressed. Based on our model, the chain appears to be squeezed out from under the disc gradually as the disc approaches the surface. The energy required to compress the mushroom increases monotonically with compression and becomes independent of chain length following chain escape.

4 Brushes and Brush-Particle Interactions

4.1 Outline of Calculations

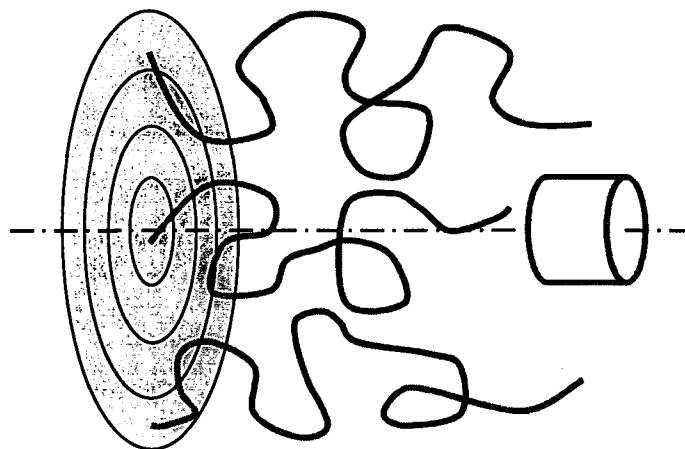


Figure 4.1 Schematic diagram showing a solute molecule interacting with polymer chains end-grafted to a surface. The centerline represents the axis of a cylindrical coordinate system, and the rings on the surface represent spatial increments in the radial direction.

Because of applications for end-grafted polymer surfaces in the field of biomaterials and bioseparations, the interactions between solute molecules and the end-grafted polymer chains becomes important to understand. Several molecular-based models have been developed for analyzing brush distributions as a function of conditions. Few studies however, have focused on a small impenetrable particle (a protein molecule perhaps) interacting with, or moving into, polymer chains that are end-grafted to a surface. In this work we have studied the interaction between a cylindrical particle and a brush using our cylindrical SCF model (Figure 4.1). The density distribution of an undisturbed brush has been calculated using different interaction parameters, and as a function of surface density and chain length. The brush density distribution around a particle has also been calculated for varying system conditions and displacement of polymer segments by the particle has been monitored. Finally, the excess energy to move the particle into the brush has been evaluated.

4.2 Brush Density Distributions

A thorough discussion of brush density distributions has been presented in Chapter 1. Here, we provide a few examples of results from our model, which are in excellent agreement with experiment [Cosgrove, 1990a; 1990b] and provide a significantly more detailed and accurate picture than previous analytical theories. Figure 4.2 shows density profiles for a 50 segment brush (b) at 5% grafting density under various solvent (o) conditions. The polymer-solvent interaction parameter χ_{bo} has been varied from -0.5 to 1.0. The polymer-surface (s) and solvent-surface interaction is athermal (*i.e.* $\chi_{bs} = \chi_{ps} = 0$).

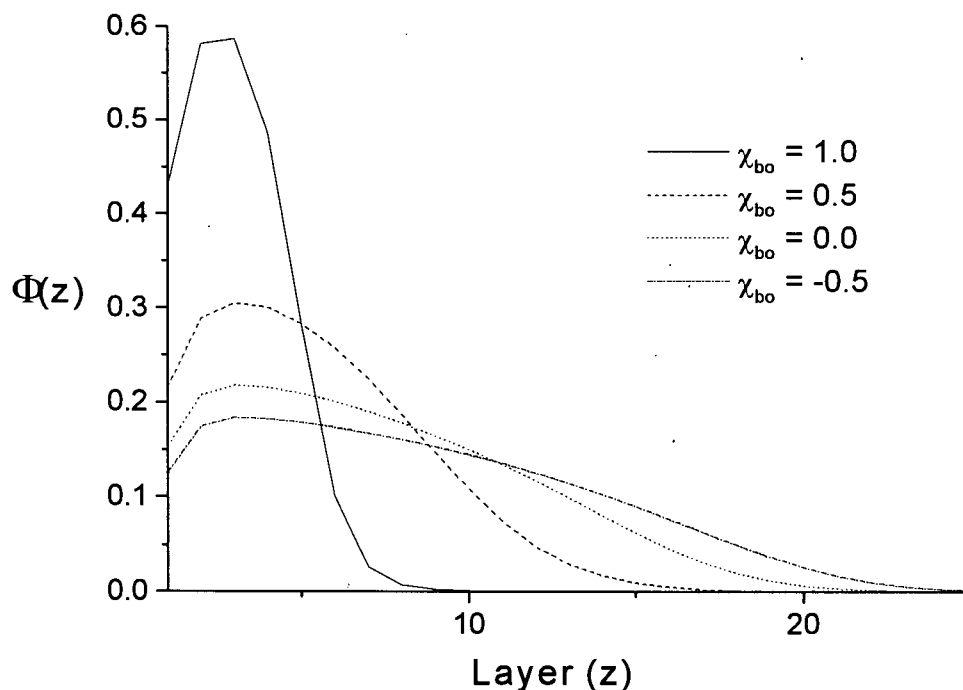


Figure 4.2 Brush density distributions for various polymer-solvent interaction parameters. $N = 50$ segments, $\sigma = 5\%$, $\chi_{os} = \chi_{bs} = 0$.

A more favourable brush-solvent interaction (*i.e.* more negative) leads to a more extended polymer layer. The brush profile for the case of $\chi_{bo} = 1.0$ is almost completely

collapsed, forming a very dense surface layer. In a worse than theta solvent ($\chi_{bo} > 0.5$ as $N \rightarrow \infty$) the polymer layer collapses since free polymer in solution would prefer to phase separate under these conditions. The brush rapidly expands away from the grafting surface as χ_{bo} decreases from poor ($\chi_{bo} = 1$) to athermal ($\chi_{bo} = 0$) solvent conditions. However, further improvement of the solvent ($\chi_{bo} < 0$) does not promote as significant an enhancement in chain stretching. In a miscible solvent, the degree of chain stretching is determined by a balance between the loss in chain entropy when extended to a linear conformation, and the gain in polymer-segment stepping paths when adjacent lattice sites become occupied by solvent. The energy required to stretch a chain into a more linear state scales with brush height squared, while the energy gain accompanying an increase in polymer-segment free volume scales approximately linearly with brush height. Thus, the stretching penalty becomes prohibitive at large brush heights and results in a very weak dependence of brush height on χ_{bo} when $\chi_{bo} < 0$.

The effect of polymer-surface interactions on the brush density profile is shown in Figure 4.3. For chains of 50 segments at 5% surface density, the polymer-surface interaction determines whether or not a depletion zone is seen next to the grafting surface. For a strong polymer-surface attraction, the depletion zone disappears. Although the overall brush profile is not changed much at high enough surface densities, a strongly adsorbing surface can lead to a profile that decreases exponentially away from the surface at low surface densities (pancake).

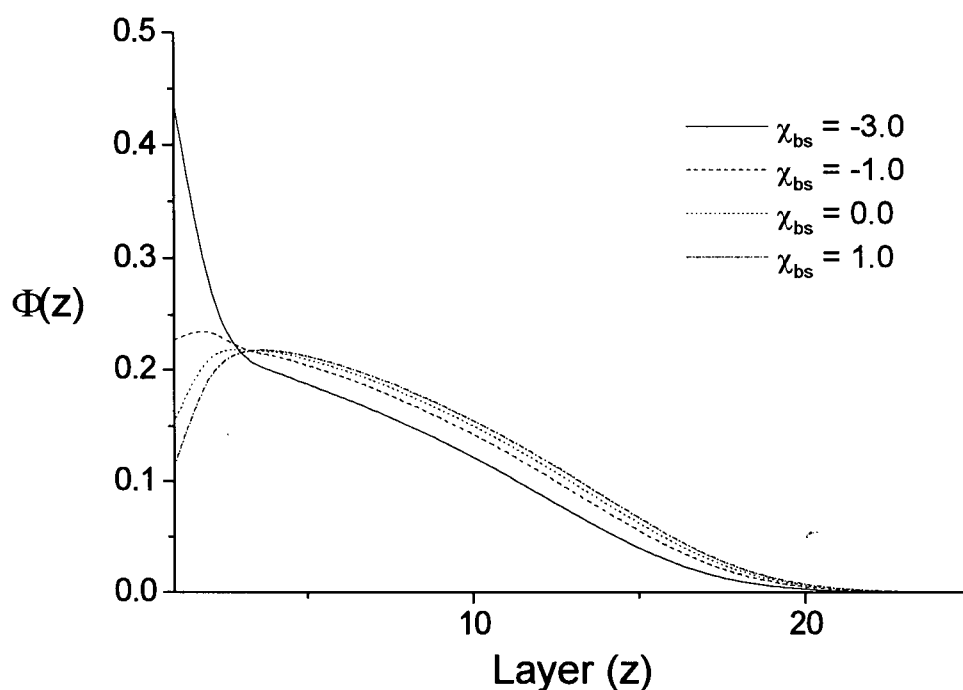


Figure 4.3 Brush density profiles for various polymer-surface interactions are shown. $N = 50$ segments, $\sigma = 5\%$, $\chi_{os} = \chi_{bo} = 0$.

Brush density distributions are shown in Figure 4.4 for four different chain lengths at 10% surface density with $\chi_{bo} = 0.5$. As the chain length is increased, the brush extends further away from the surface. Relatively little increase is observed in the maximum density, especially at the longer chain lengths. Both results are in agreement with analytical predictions [Milner *et al.* 1988a; de Gennes, 1976]. The brush height increases approximately linearly with chain length. In contrast to analytical model results [Milner *et al.*, 1988a] the segment density in the outer edge of the brush is predicted to decrease more slowly, forming an extended tail region. Due to this effect, it is common to discuss the brush height in terms of the root mean squared layer thickness, given by $h_{rms} = \int z^2 \Phi(z) dz / \int \Phi(z) dz$. It is also worth noting that the depletion and tail regions occupy a smaller fraction of the overall distribution as chain length increases.

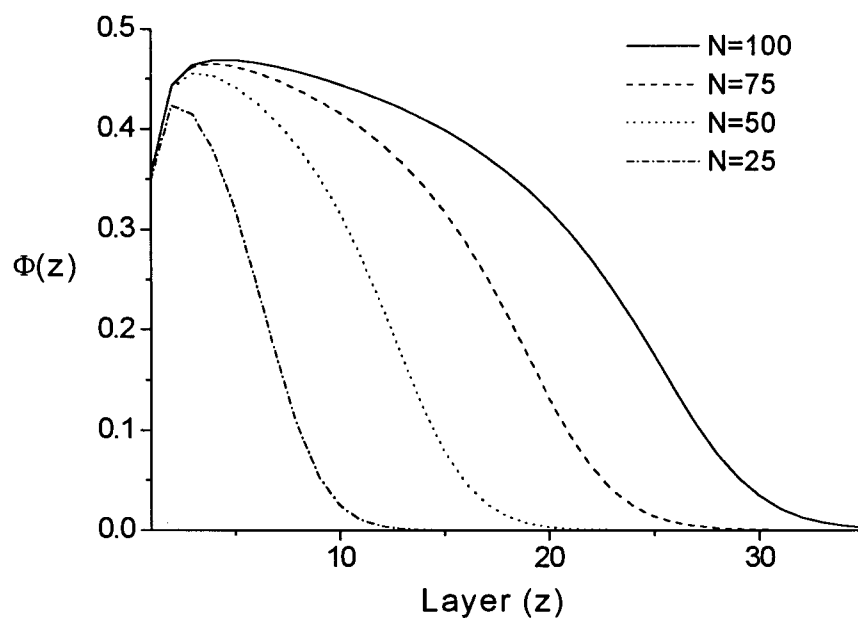


Figure 4.4 Segment density profiles for brushes of different lengths. Surface density is 10% and the polymer-solvent interaction parameter χ_{bo} is 0.5. All other interactions are athermal.

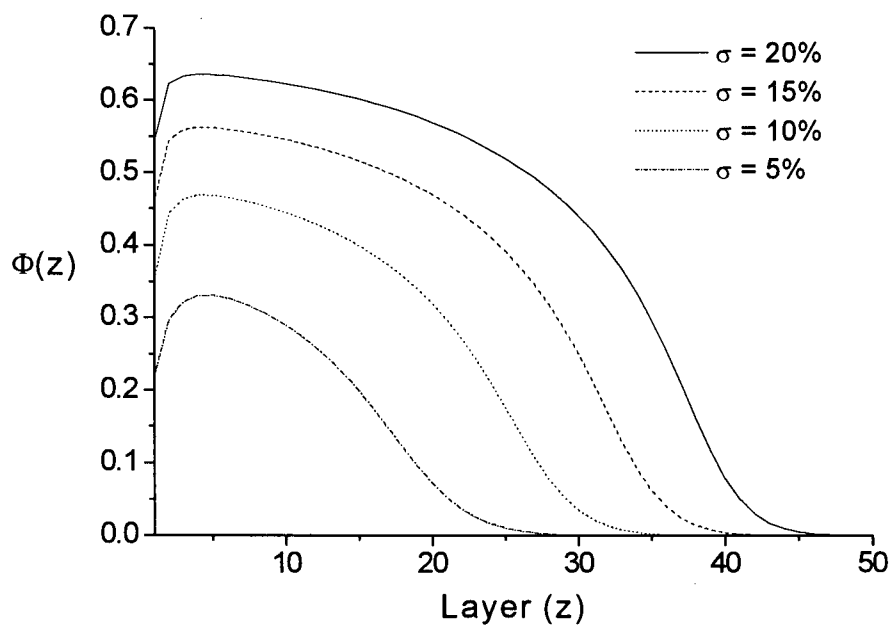


Figure 4.5 Brush density profiles for various surface densities. Chain length is 100 segments and $\chi_{bo} = 0.5$.

Figure 4.5 shows brush density distributions for 100 segment chains at four different surface grafting densities. Increasing surface density causes the maximum density of the brush to increase, as scaling models predict [Milner, 1991]. Also the increased excluded volume interactions lead to a more stretched brush and hence the height scales (less than linearly) with surface density.

4.3 Brush-Particle Interactions

4.3.1 2D Brush Density Distributions

Introduction of a particle changes the conformations of chains in the brush (Figure 4.6). The distribution of chains of $N = 50$ segments at a grafting density of $\sigma = 0.1$ is shown in Figure 4.6 for an interacting particle of radius $R_p = 3$ and length $L_p = 3$ (referred to as a 3 by 3 particle) at various distances from the surface. In order to try and simulate physiological conditions, we have set χ_{bo} , χ_{po} , and χ_{bp} to 0.4, 0.4 and 0, respectively, for most of our calculations. In addition, the calculations involve non-surface-mobile chains, unless otherwise specified. All other χ_{ij} are set to zero. These values were chosen based on the interaction parameters calculated from the LALLS data of Haynes *et al.* [1993] discussed in Chapter 2. In this way, the results should provide at least a semi-quantitative picture of globular protein interactions with grafted PEG brushes, which are finding increased application as biomaterials and anti-fouling surfaces. It is worth noting, however, that the energy curves due to brush interaction with the particle are not very sensitive to the brush-solvent or particle-solvent interaction parameters, although they are sensitive to a favorable interaction between the brush and particle.

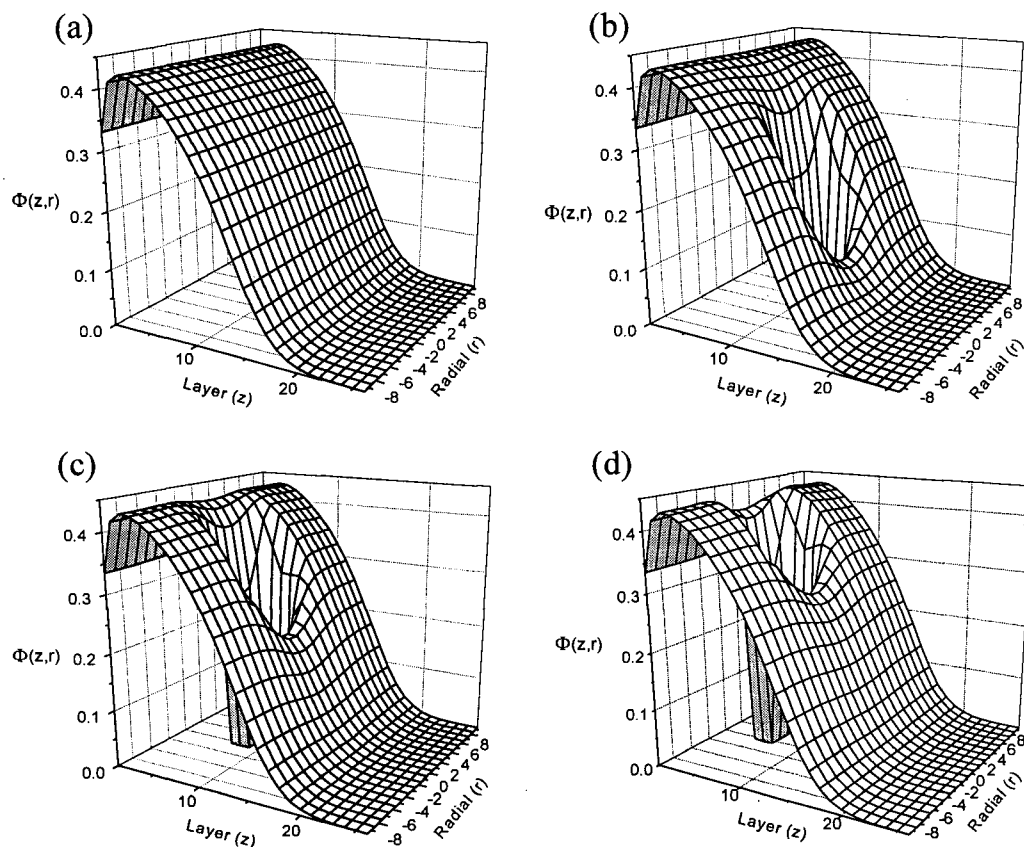


Figure 4.6 Polymer segment density distributions in the cylindrical lattice are indexed in both the z and r directions. The chains of length $N=50$ with a grafting density of $\sigma=0.1$ are interacting with a particle of dimensions $R_p=3$ and $L_p=3$ (3 by 3). Interaction parameters are set as $\chi_{bo}=0.4$ and $\chi_{po}=0.4$ (unspecified interaction parameters are always zero). The density distribution is shown for a particle position (a) outside the brush, (b) at layer $z_p = 10$, (c) $z_p = 7$, and (d) $z_p = 5$.

A brush density profile is shown in Figure 4.6 (a) at conditions where the particle is positioned outside the brush. The distribution is completely uniform in the radial direction, and shows a typical brush profile in the z -direction at near theta solvent conditions. The z and r coordinates on the plot index the mean-field radial of the cylinder, whose average brush segment volume fraction is shown on the vertical axis. In Figure 4.6 (b), (c) and (d), brush distributions are shown when the particle is sitting at layers $z_p = 10$, $z_p = 7$, and $z_p = 5$, respectively. For lattice sites occupied by the particle, the volume fraction of solvent and brush is essentially zero.

There is a slight decrease in the brush density near the edges of the particle due to the entropic penalty of chains stepping next to an impenetrable object. As the particle begins to penetrate the brush, the segment density fills in quickly behind the particle, indicating chain splaying. To reach this extended chain state there is a concomitant depletion of the segment density between the particle and the surface (in front of the particle). When the particle is positioned in layer 5 (Figure 4.6 (d)), the segment density profile also increases slightly at the sides of the particle. This leads to a physical picture of grafted chains spread around the particle such that they radially partition away from the centerline, thereby lowering the brush density in the center of the particle's path.

Segment depletion between the particle and grafting surface does not occur at all conditions, however. Figure 4.7 shows the brush density distribution for four different chain lengths (at constant surface density), with a 3 by 3 particle sitting at layer 5. For a chain length of 15 segments, Figure 4.7 (a) shows that the segment density is slightly higher between the particle and the surface, indicating brush compression without significant chain splaying. Segment depletion is first observed at a chain length of $N=25$ and becomes increasingly more pronounced with increasing chain length. Thus, the configuration of the grafted chains in the presence of a penetrating particle is a strong function of the chain length relative to the particle radius. This relationship has not been reported previously since the modeling methods based on the Alexander-de Gennes brush [Alexander, 1977; de Gennes, 1976] and analytical SCF theory [Milner *et al.*, 1988a] do not allow splaying to occur.

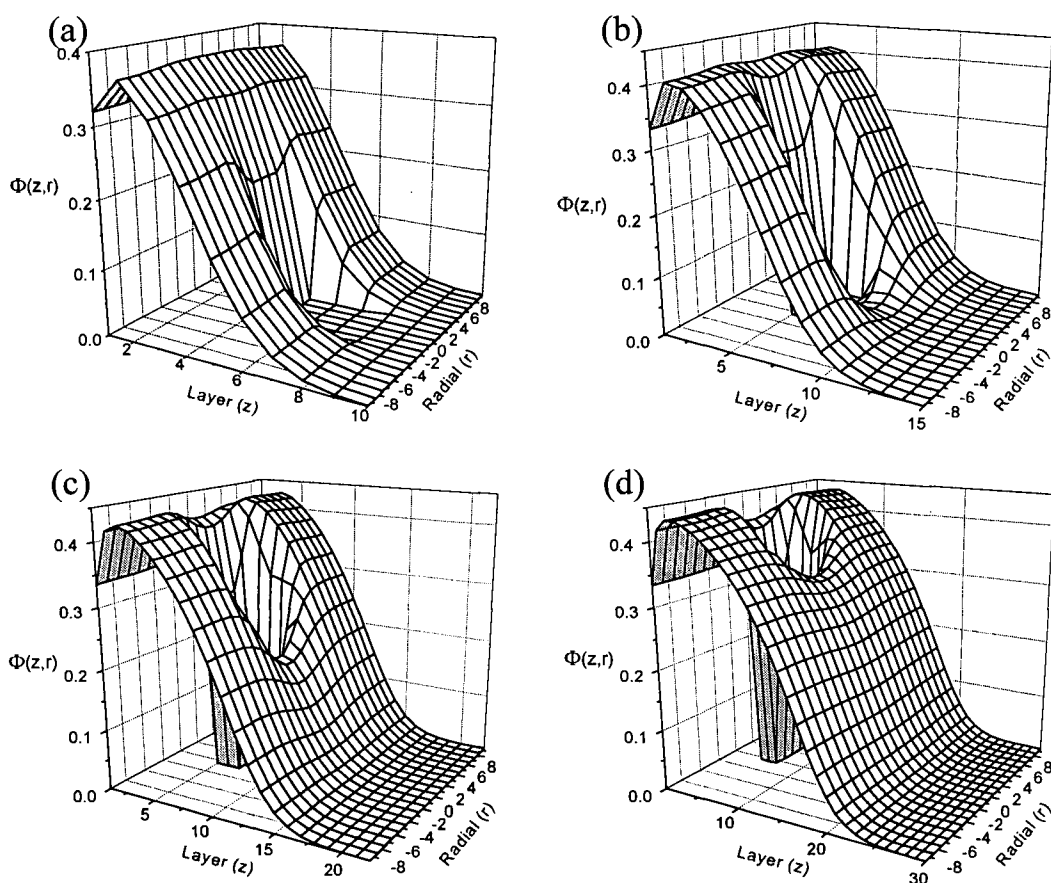


Figure 4.7 The 2-dimensional segment density distributions for four different chain lengths are shown around a 3 by 3 particle placed with the leading edge at $z_p = 5$. Interaction parameters are specified as $\chi_{bo}=0.4$ and $\chi_{po}=0.4$. Chain lengths are (a) $N = 15$, (b) $N = 25$, (c) $N = 40$ and (d) $N = 60$ segments.

Changing the surface density of the grafted chains also affects the density distribution of the brush. Figure 4.8 shows a graft of $N = 50$ segment chains interacting with a 5 by 5 particle placed at layer 7. The chains are grafted at densities of $\sigma = 0.05$, $\sigma = 0.1$, $\sigma = 0.2$, and $\sigma = 0.3$ in Figure 4.8 (a), (b), (c), and (d), respectively. Increasing the surface density results in an extension of the brush along with an increase in the maximum in its density distribution. At high surface densities, the brush profile begins to approach a step-profile in accordance with the Alexander-de Gennes brush model. Unlike variations in chain length (see Figure 4.7), increasing

the grafting density does not in general lead to a transition from complete compression of the brush to a regime where chain splaying makes a dominant contribution to the perturbed density distribution. Instead, it changes the relative amount of segment compression or splaying as seen in the segment density distribution. As the surface density increases, changes in segment density between the particle and the surface due to particle approach become less significant with respect to the rest of the density profile.

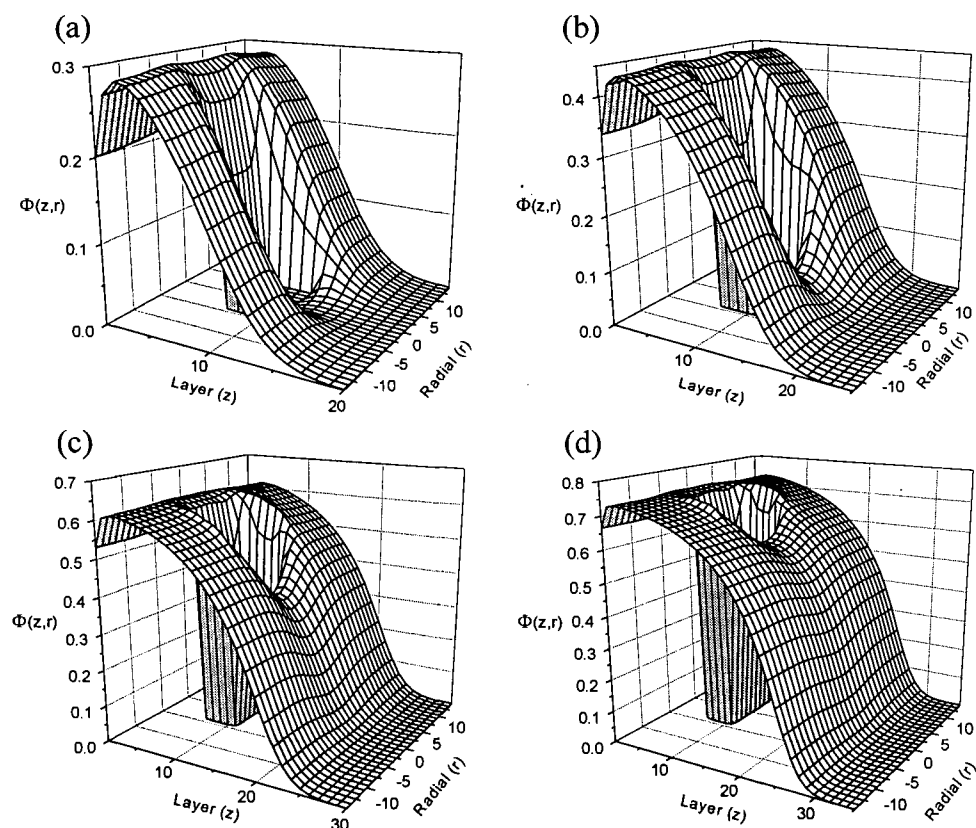


Figure 4.8 The brush distribution of $N=50$ segment chains is shown around a 5 by 5 particle at four different grafting densities. Interaction parameters are $\chi_{bo}=0.4$ and $\chi_{po}=0.4$. Grafting densities are (a) $\sigma=0.05$, (b) $\sigma=0.1$, (c) $\sigma=0.2$ and (d) $\sigma=0.3$.

4.3.2 Brush-Particle Interaction Energy

The excess energy A^{int} required to move different sized particles into a brush is shown in Figure 4.9. For a brush made up of 50-segment chains at a graft density of $\sigma = 0.1$, A^{int} increases with increasing particle size, particularly at deeper penetration depths. Under the chosen conditions, formation of contacts between brush and particle segments is enthalpically favorable since both segments have a net unfavorable interaction with the solvent ($\chi_{io} > 0$). Nevertheless, the calculated A^{int} values are always positive and increase sharply as the particle penetrates deeper into the brush. Thus, A^{int} is dominated by entropic effects, which are strongly repulsive due to the chain conformations that are eliminated by the presence of the particle.

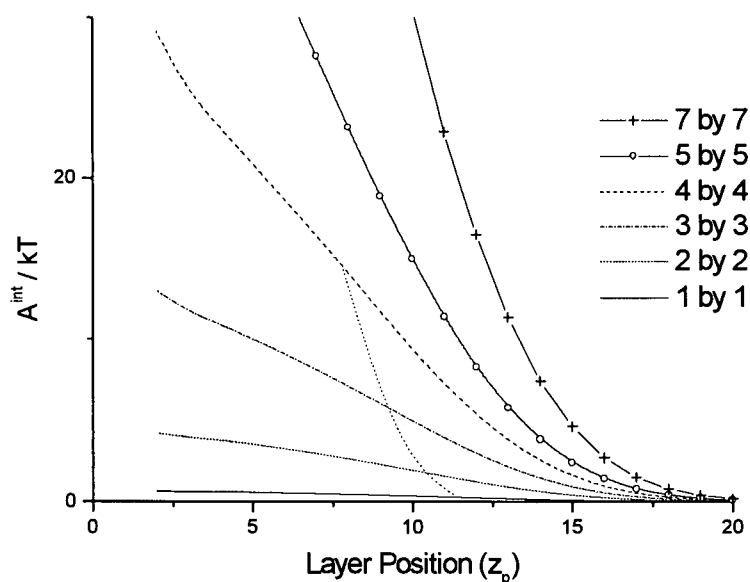


Figure 4.9 Brush-particle interaction energy curves are shown for chains of $N=50$ with a graft density of $\sigma=0.1$ interacting with various sized particles. Interaction parameters are specified as $\chi_{bo}=0.4$ and $\chi_{po}=0.4$. Particle size has been varied from $R_p=1$, $L_p=1$ up to $R_p=7$, $L_p=7$. The dashed line shows the inflection point of each curve that shows one.

The effect of chain length on brush-particle interaction energies is shown in Figure 4.10 for a 3 by 3 particle. As the chains are made longer the onset of an energetic repulsion occurs farther from the surface. This distance appears to scale linearly with N , as we might expect since $h \sim N$ [Milner, 1991]. For longer chains, A^{int} becomes nearly independent of chain length at particle positions close to the surface. This might be explained by the fact that increased chain length extends the brush, and allows chains to fill in the space behind the particle more easily. Once a particle has significantly penetrated a relatively long brush, the conformational entropy lost by the chains due to particle approach is at least partly offset by the gain of configurations of the chain segments, which step behind the particle.

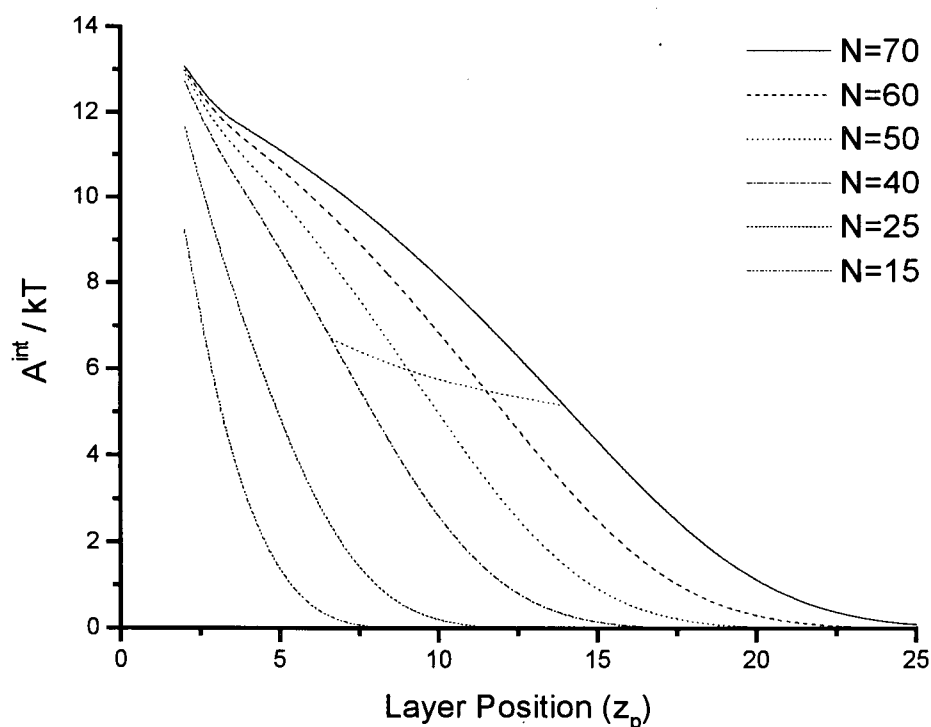


Figure 4.10 Interaction energy curves are shown for a particle of $R_p=3$, $L_p=3$ interacting with different length polymer chains of constant grafting density $\sigma = 0.1$. Interaction parameters are $\chi_{bo}=0.4$ and $\chi_{po}=0.4$. The dashed line shows the inflection point of each curve.

The dotted lines in Figure 4.9 and Figure 4.10 intersect the energy curves at a point of inflection. Each inflection point represents a maximum in the force F required to move the particles into the brush, since $F = -\partial A^{\text{int}} / \partial z_p$. An inflection point is not observed for all combinations of N and R_p . Instead, there is a critical chain length N_{critical} above which an inflection point is seen for a given particle size. Figure 4.11 shows N_{critical} as a function of R_p for a constant grafting density of 10%. The critical chain length for this system increases linearly with R_p . A linear dependence of the critical chain length on R_p corresponds to a linear increase in the distance that chain segments must reach in order to occupy space behind the particle. The minimum chain length for an inflection point in the limit of an infinitesimal particle is *ca.* 5 segments.

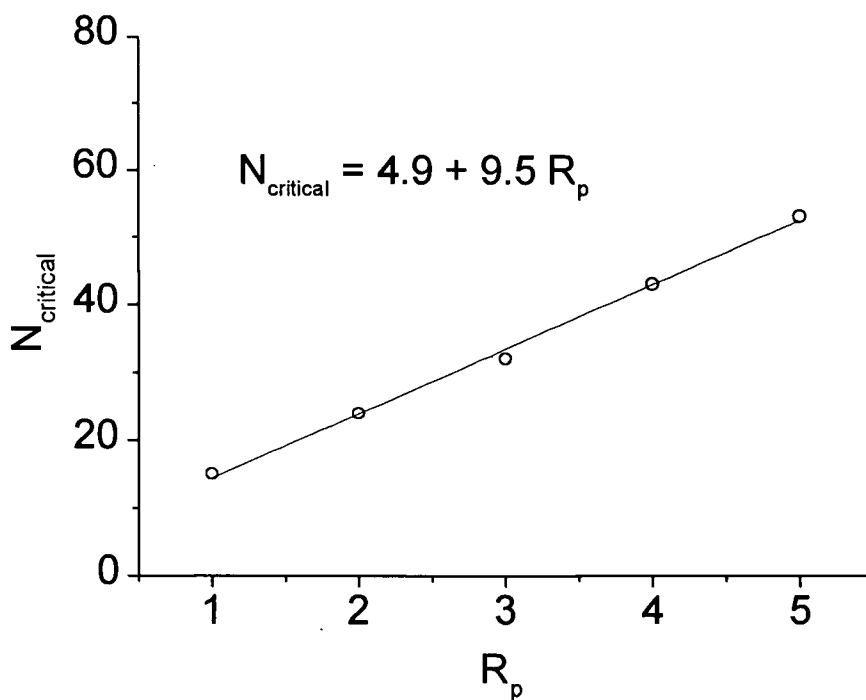


Figure 4.11 The critical chain length N_{critical} for which an inflection point is observed is shown as a function of R_p for the system with $\sigma = 0.1$, the previous interaction parameters, and particles with a cylindrical geometry where $L_p = R_p$.

The change in brush-segment density profile which leads to the observed inflection point was analyzed by calculating A^{int} curves for penetration of a 3 by 3 particle under two limiting cases: (i) pure compression of the brush by the particle (which is equivalent to the model of Subramanian *et al.* [1996]), and (ii) penetration into a brush in which all chains grafted directly beneath the particle have been removed (so that no chain splaying can occur).

Placing the reflecting boundary of the lattice in radial $R_p + 1$, where R_p is the particle radius, allows the energy of pure chain compression to be calculated. Under this limiting condition, A^{int} increases monotonically with particle approach and no inflection point is observed. Thus, the inflection point is related to chain segment escape from beneath the approaching particle. In principle, the inflection point could result from the lower energy of splayed chains relative to compressed chains and/or the increase in configurational entropy of chains which extend beyond the particle volume and can thereby step into the solvent-rich space behind the particle.

Results from limiting case (ii), where no chain splaying can occur, show an inflection point, suggesting that the inflection is due to the invasion of extended chain segments into the space behind the particle. Indeed, in this case A^{int} begins to decrease (indicating a slight attraction) as the particle is moved very close ($z_p < 3$) to the grafting surface. Segment density profiles under this condition indicate that the chains adjacent to the side walls of the particle reach a lower energy state by stretching slightly in the z-direction to allow a larger number of segments to sample the volume directly behind the particle. A similar result, in which there is an inflection point and a decrease in A^{int} when the particle is close to the surface, is obtained when model calculations are carried out for a brush of surface-mobile chains (section 4.3.3). It is also worth noting that the model of Subramanian *et al.*, which is limited by the severe assumption that

chain splaying can not occur, does not predict the presence of an inflection point. As a result, Subramanian *et al.* predict the existence of a maximum in compression force only for a surface covered by multiple mobile mushrooms.

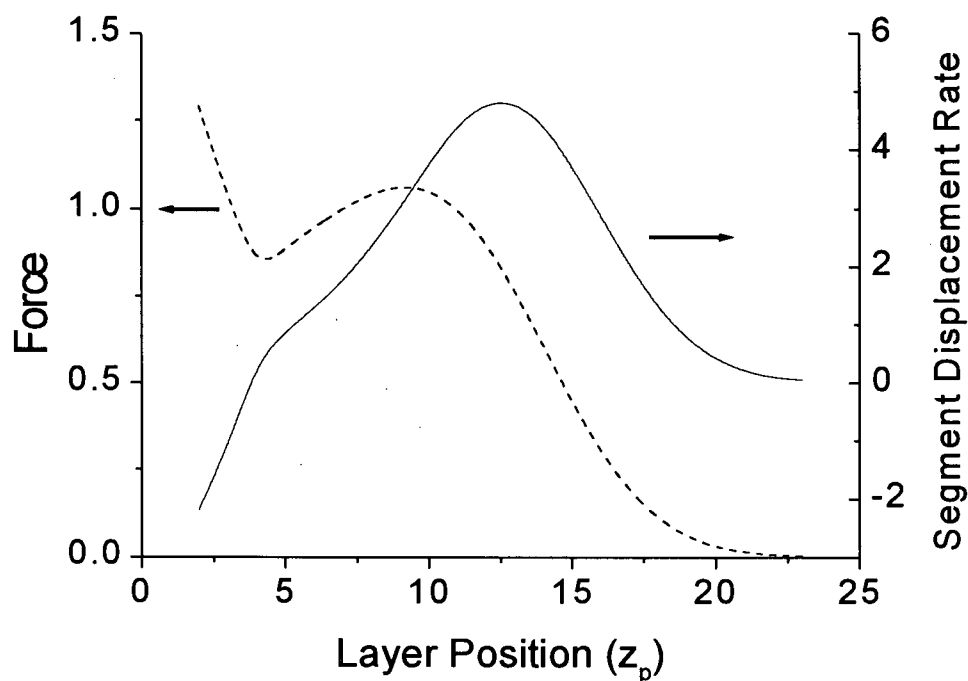


Figure 4.12 F and the rate of segment displacement from the total volume the particle moves through are shown as a function of z_p for a 3 by 3 particle moving into a brush with $N = 50$ and $\sigma = 0.1$.

Our results indicate that an inflection point can appear when chain segments are able to fill in the space behind the particle. As it penetrates the brush, the particle reduces the conformational entropy of the brush, increasing A^{int} . When the chains are able to gain a significant amount of conformational entropy by filling in behind the particle, the rate of increase in A^{int} with respect to particle position gets smaller, giving rise to the inflection point. It is therefore useful to consider the segment density in the volume defined by the particle and the volume directly above and below it. As the particle is moved toward the surface, the number of

chain segments in the particle's path volume is always decreasing. As segments begin to fill in behind the particle, however, the rate of segment displacement changes. Figure 4.12 shows the rate of decrease in the total number of segments (in front of and behind the particle) as a function of particle position; $-\partial A^{int}/\partial z_p$ is also shown for the same system. In systems where N is above $N_{critical}$, the inflection point in A^{int} always coincides with the point where the rate of displacement of segments by the particle is decreasing the fastest with respect to z_p . That is, where the rate of accumulation of segments behind the particle is a maximum.

In the MD simulations by Murat and Grest [1996], the segment density between an AFM tip and the surface was found to remain approximately constant due to rearrangement of the polymer chains around the tip. The radius of their AFM cylinder was large compared to the segment length (7 to 16 times) for simulations with 100 segment chains. Under such conditions, we also see little or no depletion of segments if particle size is made large. They also found a constantly increasing repulsive force under compression. Our results are consistent with the fact that they used a long cylinder, which extends outside the brush to model the AFM tip. As a result, there was no empty space behind the tip that would allow chains segments to fill in behind it.

The dependence of the inflection point position $Z_{inflection}$ and the magnitude of the force maximum F_{max} on particle size, chain length and surface density were also investigated for specific cases. For a brush with $N = 50$ and $\sigma = 0.1$ The inflection point was found to move toward the surface in roughly linear proportion with increasing R_p (Figure 4.9). For the same system, F_{max} was found to increase in proportion to $R_p^{2.8}$, as shown in Figure 4.13, which suggests that it scales closely with particle volume. For a 3 by 3 particle and 10% grafting density (Figure 4.10), $Z_{inflection}$ moves away from the surface almost linearly with increasing N

($Z_{\text{inflection}} \sim N^{0.8}$), which corresponds closely to the scaling of brush height. Furthermore, F_{max} was found to decrease with increasing chain lengths such that $F_{\text{max}} \sim N^{-1.2}$. Longer brush chains can more quickly adopt configurations that step behind a particle. This combined with the fact that a particle of fixed size will take away a smaller fraction of the conformations sampled by larger chains, results in an earlier inflection point in A^{int} and lower F_{max} .

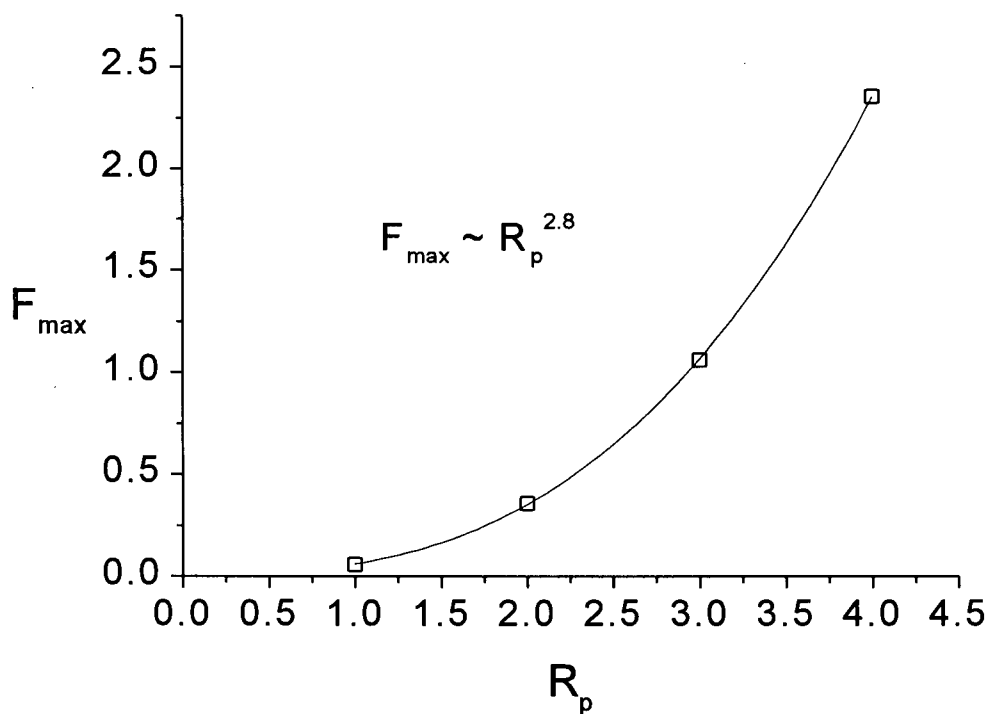


Figure 4.13 F_{max} is shown as a function of particle size for a brush with $N = 50$ and a 10% graft density. The maximum force appears to scale closely with particle volume.

The dependence of A^{int} , $Z_{\text{inflection}}$ and F_{max} on surface density was also investigated for a brush with $N = 50$ and 3 by 3 particle and is shown in Figure 4.14. The energetic repulsion was found to increase significantly with grafting density, due primarily to the increased overall density in the brush distribution. The onset of repulsion also appears to start at a distance from the surface that increases linearly with grafting density. This agrees with the observation that

brush height scales linearly with σ in a very poor solvent ($\chi = 0.4$) [Fleer *et al.*, 1993]. The values of Z_p and F_{max} were both found to increase approximately linearly with the grafting density ($Z_{inflection} \sim \sigma^{0.8}$, $F_{max.} \sim \sigma$).

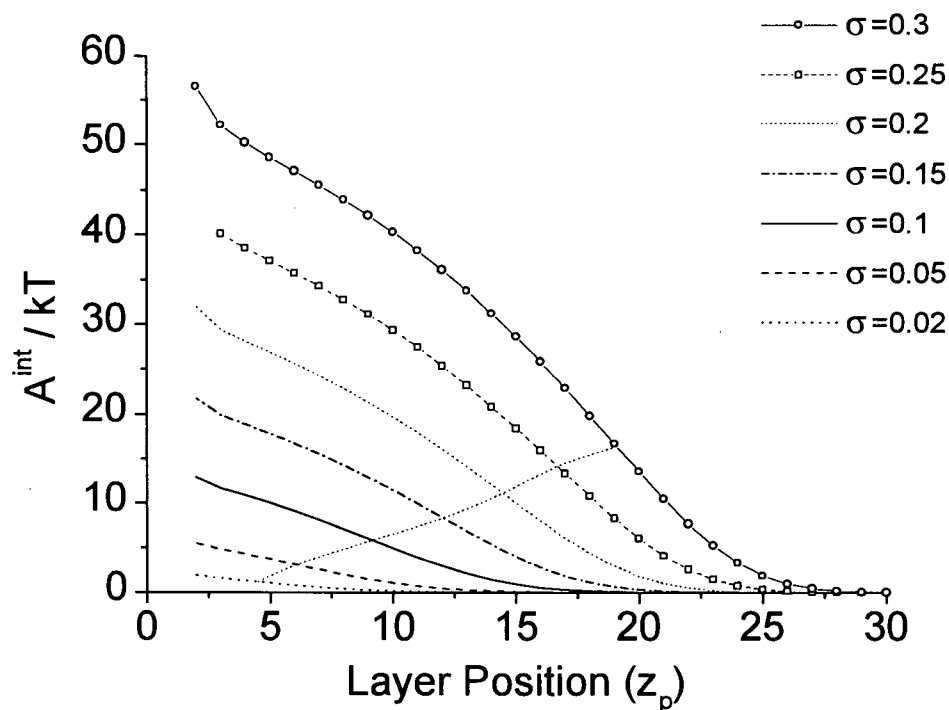


Figure 4.14 Interaction energy curves are shown for a particle of $R_p=3$, $L_p=3$ interacting with 50 segment polymer chains of varied grafting density. Interaction parameters are $\chi_{bo}=0.4$ and $\chi_{po}=0.4$. The dashed line shows the inflection point of each curve.

4.3.3 Surface Mobile Brushes

Grafting can be simulated such that the chain segments attached at layer 1 redistribute themselves radially when a particle is placed very close to the surface, simulating what might occur if the graft were surface mobile. The chain ends can also be fixed such that each grafted segment is confined to a specific radial at $z=1$. In the latter case, the brush is fixed to the grafting surface by individually grafting chains to each radial. The number of chains used to calculate the

normalization constant for each separate radial must then be calculated using the number of lattice sites in the radial and assuming a constant grafting density. The fixed brush therefore consists of R_{max} components, for each of which Equation (2.39) has a different starting point. Finally the total brush density distribution is calculated by summing the volume fractions of the separate components.

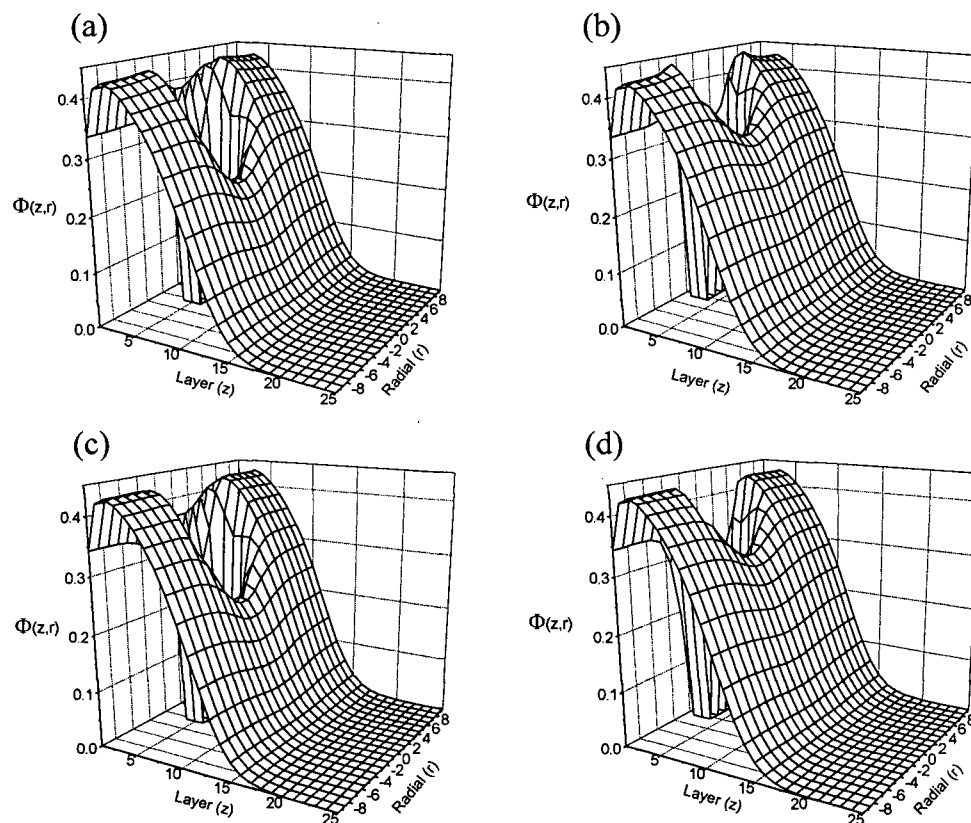


Figure 4.15 Brush distribution around a 3 by 3 particle is shown for surface non-mobile and mobile brushes. Brushes consist of $N=40$ segment chains at 10% surface density and interaction parameters used were $\chi_{bo}=0.4$ and $\chi_{po}=0.4$. The distributions for non-mobile chains around a particle in (a) layer $z_p = 4$ and (b) $z_p = 2$ are shown; distributions of mobile chains around a particle in (c) $z_p = 4$ and (d) $z_p = 2$ are also shown.

A comparison of the segment density distribution for mobile and non-mobile chains around a particle is shown in Figure 4.15. The brush distributions were calculated for $N = 40$ segment chains at 10% surface density around a 3 by 3 particle. Figure 4.15 (a) and (b) show

non-mobile chains with the particle positioned in layer $z_p = 4$ and $z_p = 2$, respectively. The non-mobile chains can not decrease their density in layer $z = 1$ below the grafting density of 10% ($\Phi = 0.1$). As a result, the chain segment density at the maximum can be seen to increase around the edges of the particle. Figure 4.15 (c) and (d) show the density distribution of the surface mobile brush around a particle in layer $z_p = 4$ and 2, respectively. The brush density for the mobile chains at the maximum is uniform in the radial distribution indicating that the chains are able to redistribute themselves within the lattice. When the particle is positioned at $z_p = 2$, the density between the particle and the surface in Figure 4.15 (d) is significantly below $\Phi = 0.1$, indicating that chains have been displaced from the volume directly beneath the particle.

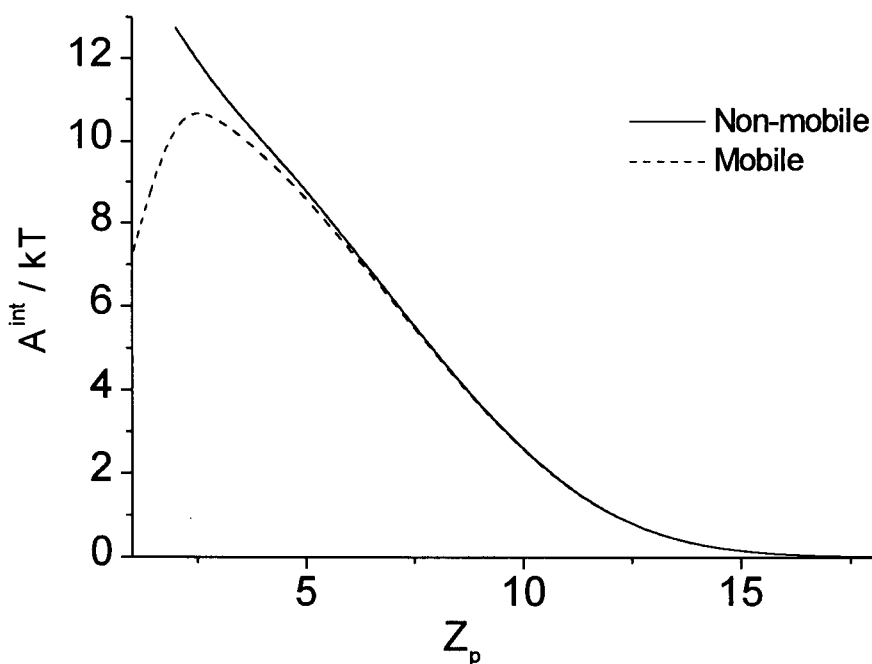


Figure 4.16 Interaction energy curves are shown for a 3 by 3 particle interacting with 40 segment polymer chains that are surface mobile (dashed) and non-mobile (solid). Interaction parameters are $\chi_{bo}=0.4$ and $\chi_{po}=0.4$.

The brush-particle interaction energies A^{int} for the mobile and non-mobile brushes are compared in Figure 4.16 (for the same conditions as Figure 4.15). At close approach to the surface ($z_p < 6$) the mobile brush density directly beneath the particle becomes lower than that of the non-mobile brush, thus providing a weaker entropic repulsion. At a particle position directly next to the surface ($z_p = 1$) the interaction energy actually decreases for the mobile brush due to an increase in the configurational entropy of the chains. This suggests that if the particle were able to penetrate all the way into the brush it would prefer to remain there.

4.3.4 Brush-Particle Attraction

Joel et al. [1991a; 1991b] have predicted a minimum in the interaction energy (negative A^{int}) between a protein and a polyethylene oxide graft when a strong hydrophobic interaction free energy term is included in their model. On closer approach of the particle to the grafting surface, they predict a strong steric repulsion that leads to a monotonically increasing interaction free energy. In order to compare our model predictions with those of Joel *et al.* we have set the brush-solvent χ_{bo} , particle-solvent χ_{po} , and the brush-particle χ_{bp} interaction parameters to 0.5, 0.5 and -0.5 respectively (all other $\chi_{ij} = 0$). These interaction parameters will be assumed for the remainder of this discussion.

A strongly negative brush-particle interaction parameter is needed in order to see a minimum in A^{int} with our model. The magnitude of χ_{bp} is almost unrealistic for an interaction that is not electrostatic in nature, suggesting that perhaps Joel *et al.* might have over-estimated the hydrophobic interaction energy. Experiments have shown that short PEG chains can increase protein adsorption slightly [Merril, 1992; Kishida *et al.*, 1992] suggesting a net weak attraction between polymer and protein. Interaction parameters calculated from data of Haynes *et al.*

[1993] show that the polymer-protein interaction is weak, however, with a maximum attractive value of $\chi_{bp} = -0.1$.

The interaction energy for various sized particles with a 50-segment brush at 10% grafting density is shown in Figure 4.17. As the particles begin to move into the brush, favorable brush-particle energetic contacts dominate the interaction energy, leading to negative values of A^{int} . With further penetration, a net energetic repulsion occurs once the loss of chain entropy is greater than the favorable contact energy. As the particle size increases, the position of the onset of energetic repulsion Z_{onset} occurs sooner (higher z_p). As shown in Figure 4.17, the increase in Z_{onset} with particle size gets progressively smaller as the particle size becomes larger. This suggests that Z_{onset} will reach a constant value, equal to that for compression by an infinite flat plate.

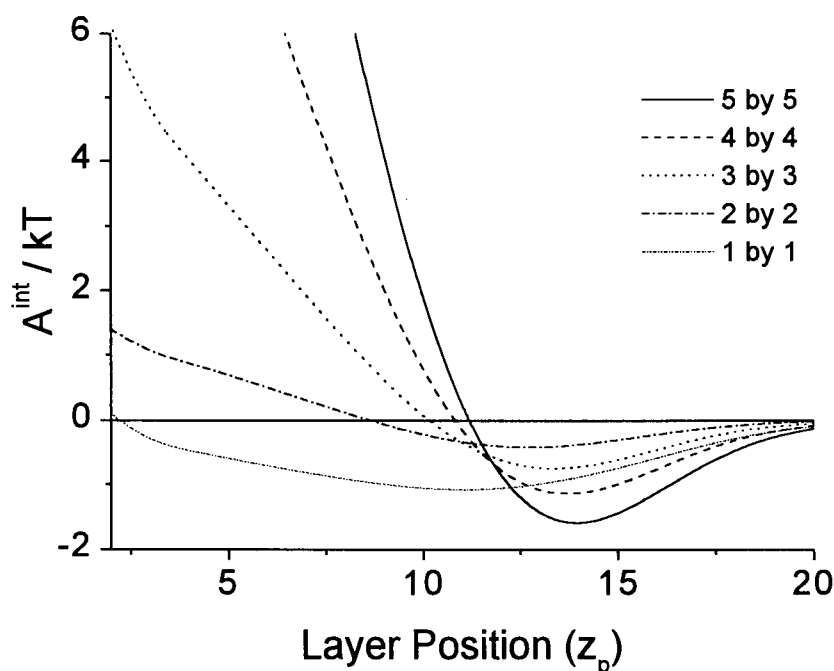


Figure 4.17 Brush-particle interaction energy curves are shown for five different sized particles interacting with chains of length $N=50$ and grafting density $\sigma=0.1$. Interaction parameters are $\chi_{bo}=0.5$, $\chi_{po}=0.5$ and $\chi_{bp}=-0.5$.

The smallest particle (1 by 1) occupies *ca.* 3 lattice sites and because of its small size does not experience a significant entropic repulsion by the chains. As a result A^{int} is negative for the 1 by 1 particle beyond layer 2 due to the energetic attraction. For the particles with $R_p > 1$, as R_p increases, the magnitude of the attractive minimum $|A_{min}^{int}|$ increases significantly such that $|A_{min}^{int}| \sim R_p^{1.8}$ (ignoring the 1 by 1 particle). This favorable interaction energy scales closely with particle surface area, since it is based on the number of contacts that brush and solvent segments make with the surface of the particle. The minimum in A^{int} indicates that the solute particles can preferentially adsorb to the surface of a brush under appropriate conditions.

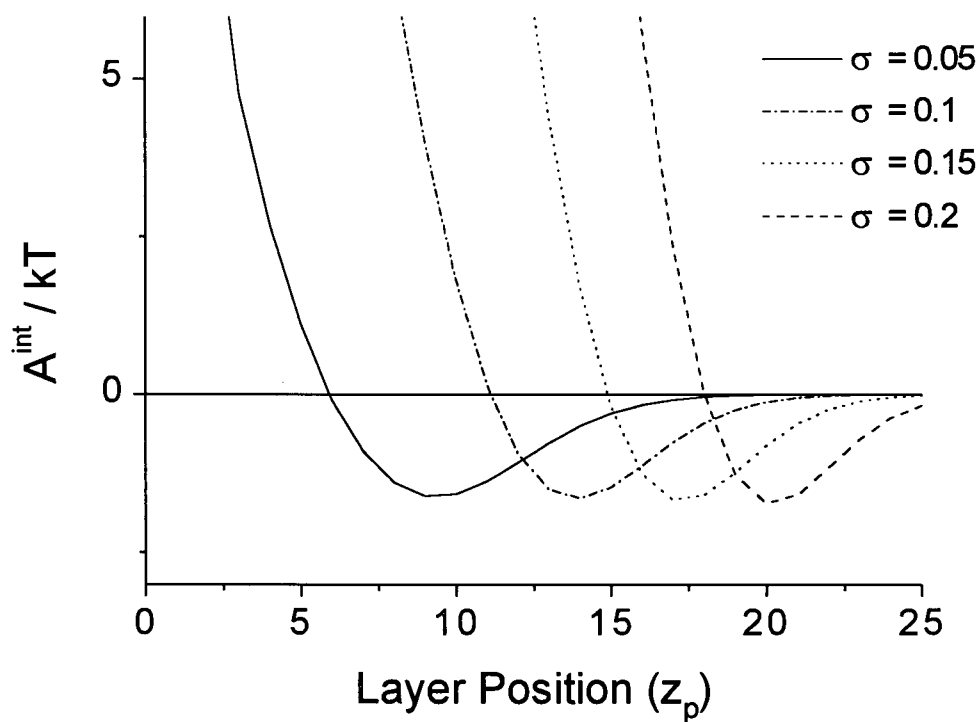


Figure 4.18 Brush-particle interaction energy curves are shown for a 5 by 5 particle penetrating chains of length $N=50$ at four different grafting densities. Interaction parameters are $\chi_{bo}=0.5$, $\chi_{po}=0.5$ and $\chi_{bp}=-0.5$.

The dependence of A^{int} on σ is shown in Figure 4.18. The brush consists of 50 segment chains that are interacting with a 5 by 5 particle. As the grafting density is increased, Z_{onset} increases with increasing σ ($Z_{onset} \sim \sigma^{0.4}$) due to the extension of the brush with increased graft density. The model predicts that A_{min}^{int} decreases slightly with increasing σ and is shifted away from the grafting surface. The gradual increase in the attractive minimum may result from more brush-particle contacts at higher surface density. The entropic repulsion appears to scale more strongly with increasing σ than the energetic attraction, and as a result the attractive regions of the A^{int} curves become narrower with increasing σ . These two effects agree with the observation that a brush profile becomes more step-like as surface density is increased. However, the dependence of A_{min}^{int} on σ is quite weak and the scaling therefore difficult to determine.

We have also investigated the effect of N on the interaction energy for this set of interaction parameters as shown in Figure 4.19. Z_{onset} shifts away from the surface approximately linearly with increasing N , again corresponding to the extension of the brush from the surface. The minimum in A^{int} becomes slightly shallower with increasing N , although the dependence appears very weak. However, longer chains have a broader attractive minimum than short chains. This may be because long chains are able to form multiple contacts with the particle over a wider range of particle positions.

If the criterion for protection of a surface is the distance at which a repulsion energy begins, Z_{onset} , then for a given brush length and surface density, we predict that larger particles should be repelled better. Also, because h and Z_{onset} increase with increasing N and σ , maximum repulsion will be obtained with long chains at the highest surface density possible.

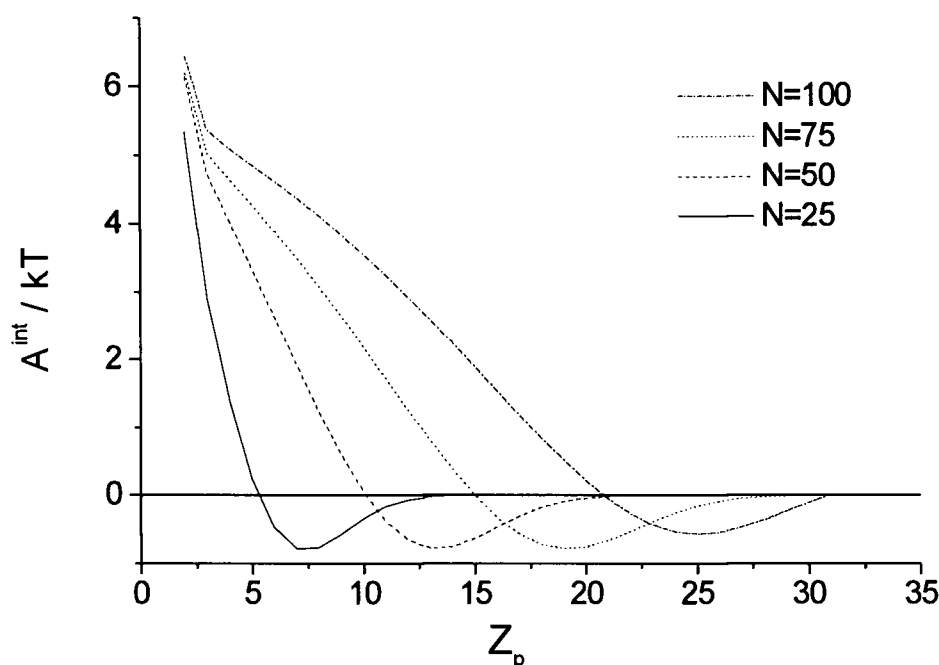


Figure 4.19 Brush-particle interaction energy curves are shown for a 3 by 3 particle penetrating brushes of varied chain length, each at 10% grafting density. Interaction parameters are $\chi_{bo}=0.5$, $\chi_{po}=0.5$ and $\chi_{bp}=-0.5$.

The magnitude and width of the attractive minimum may also be important considerations if it is important to minimize any possible interaction between a protein and the brush. For example, studies have shown that although grafted polymer will strongly inhibit platelet adhesion, transient contacts can still lead to platelet activation and decreased platelet counts [Llanos and Sefton, 1993]. If the criteria for choosing the optimum surface coverage are maximizing Z_{onset} while at the same time minimizing the concentration of particles in the region of attractive interaction with the brush, predicting the optimum conditions becomes more difficult.

In the ideal solution limit, the Boltzmann factor $K_p(z_p) = \exp(-A^{int}(z_p)/kT)$, gives the concentration of solute particles $C_p(z_p)$ at position z_p with respect to the bulk solution as $C_p(z_p) =$

$C_p^{bulk} * K_p(z_p)$. The region of negative interaction energy will therefore have a higher concentration of particles than in the bulk solution, while the repulsive region has a much lower concentration. In order to determine optimum brush conditions when considering both the magnitude and width of the minimum, it is useful to calculate the average concentration of solute particles in the brush. For simplicity, we assume that the brush is an infinite plane in the x and y -directions (perpendicular to the grafting surface). The average particle concentration in the brush is then given by

$$C_p^{avg} = C_p^{bulk} \frac{\int_{z_p=0}^{z=h} K_p(z_p) dz_p}{\int_{z_p=0}^{z=h} dz_p} \quad (4.1)$$

where h is the brush height arbitrarily chosen by us as the point at which the volume fraction of an undisturbed brush falls below 0.1%. Multiplying the average concentration by the height of the brush gives a value that is proportional to the number of particles that are interacting with the brush.

Figure 4.20 shows K_p as a function of particle position z_p for different sized particles interacting with a brush of 50 segments. At positions z_p where K_p is greater than unity (negative A^{int}), the concentration of solute particles will be greater than that in bulk solution. Based on Equation (4.1), the average particle concentration in the brush C_p^{avg} is equal to the area under each curve (up to the brush height h) divided by h . The smallest particle (1 by 1) will partition strongly into the brush due to the attractive energetic interaction and a lack of entropic repulsion. For the larger particles, however, the entropic repulsion is much more significant and K_p is seen

to fall below unity upon any appreciable penetration into the brush. The attractive region at the outer edge of the brush increases with particle size as seen by the increase in K_p .

We predict that the total number of particles interacting with the brush decreases with increasing σ due to the narrower attractive region at higher σ (Figure 4.18). Therefore, increasing surface density for a given chain length should always improve resistance to solute interaction with a surface, even in cases where brush-particle attraction occurs.

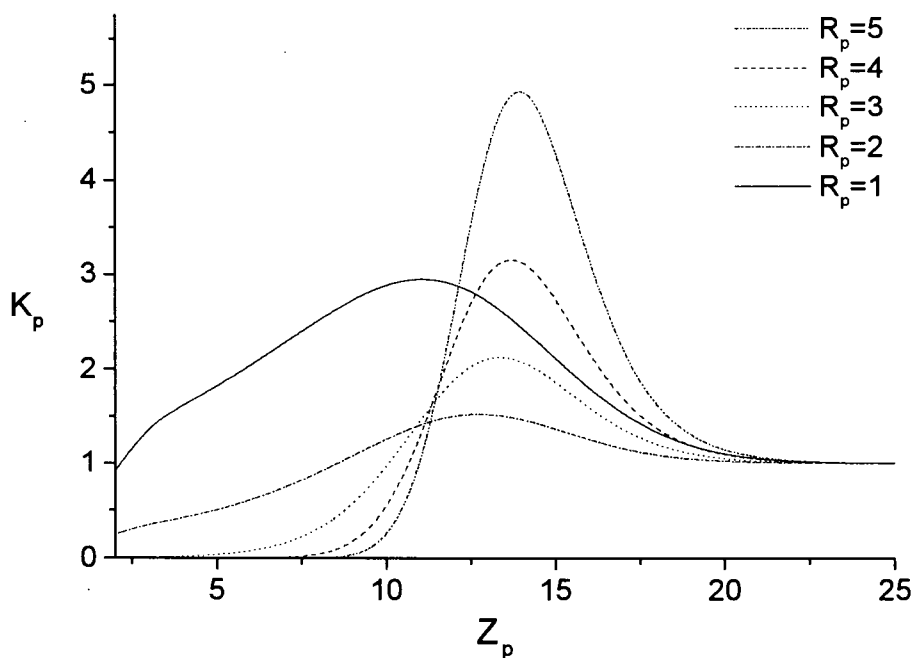


Figure 4.20 Layer partition coefficient $K_p(z_p)$ for various particle sizes interacting with 50 segment chains at 10% surface density. Interaction parameters are $\chi_{bo}=0.5$, $\chi_{po}=0.5$ and $\chi_{bp}=-0.5$.

When chain length is increased, the width of the attractive minimum is increased causing an increase in partitioning of particles to the brush surface region (Figure 4.19). This suggests that very long flexible chains may actually be less effective at reducing adsorption, especially since experimentally, lower surface densities are normally obtained with higher degrees of

polymerization. Under conditions of weak attraction, the optimum properties of end-grafted polymer for protection against adsorption are therefore a combination of low N and high σ that gives an acceptable value of Z_{onset} .

It is important to note that we find a different result for optimum protein repulsion than Joen et al. [1991a; 1991b]. Their steric repulsion term, based on an energy balance between a chain stretching term and an osmotic energy term, does not allow the brush to splay around the protein. We have shown that splaying is an important phenomenon in the case where a small particle penetrates a brush. Their model assumes a constant density for the brush, which increases as the protein moves toward the surface. As a result, they overestimate the density of polymer between the particle and the surface and thereby predict very large repulsive energies. By adding a steric repulsion term to a hydrophobic interaction energy term, they have assumed that the terms are thermodynamically additive. This is almost certainly a poor assumption, since entropy plays a significant role in the "steric" repulsion by the polymer chains as well as in the hydrophobic interaction energy.

Other work which considers the mechanism of protein repulsion by polymers such as PEG predicts that it may be due to the hydrophilic nature of the polymer, or the strong hydration shell required to solvate the polymer [Gölander *et al.*, 1992]. Our calculations suggest that while those may contribute, the dominant effect in protein repulsion is the high degree of flexibility in the polymer chains, which in thermodynamic terms is seen as high conformational entropy. Penetration of a particle into the chains decreases the chain entropy, giving rise to a sharp increase in the brush-particle interaction energy. This is supported by the results of Schroën *et al.* [1995] who found that an extended brush configuration of adsorbed Pluronic copolymer was

significantly better at reducing protein adsorption than a collapsed layer, even though the surface was made more hydrophilic in both cases.

NOMENCLATURE

Symbols

a	= activity (mol/L, g/L)
	= experimental constant used to calculate radius of gyration (nm)
A	= Helmholtz energy
A_{ii}, A_{iii}	= osmotic second (mL-mol/g ²) and third virial coefficient (mL ² -mol/g ³)
A_{mon}	= maximum monolayer capacity of grafted polymer (g/m ²)
B	= proportionality constant for calculation of analytical brush density profile
c	= weight concentration of solute (g/mL)
	= conformation of a polymer chain in the lattice model
C_i	= normalization constant for volume fraction calculation in numerical SCF model
$C_p(z_p)$	= concentration of the particle at position z_p within the brush
C_p^{avg}	= average concentration of solute within the brush
D	= distance between two grafting surfaces upon brush compression
f_i	= probability that any site adjacent to a previously occupied site is already filled during placement of chain $i+1$ in a lattice
f	= vector set of nonlinear functions used to solve numerical SCF model
F	= sum of squares of nonlinear functions used to measure the extent of solution convergence
$G(z, r)$	= free segment weighting factor; weight for a free segment to be in lattice position (z, r) with respect to the bulk solution.
$G(z, r, s)$	= chain end distribution function; weight for segment s of the chain to be in lattice position (z, r)
h	= brush height
J	= Jacobian matrix used for solution of nonlinear set of equations
k	= Boltzmann constant (1.38×10^{-23} J/K)

K_p	=	Boltzmann factor giving the ratio of solute concentration inside the brush to that in bulk solution (partition coefficient)
l, l_L	=	polymer repeat unit length; lattice unit length for one chain segment (nm)
L_i^c	=	number of lattice sites available for placement of the first chain segment of the first chain in the cylindrical lattice
$L(r)$	=	number of lattice sites in one layer of radial r of the cylindrical lattice
m	=	mass of one polymer molecule
M_m	=	mass of one monomer unit (kDa)
M, M_n, M_w	=	polymer molecular weight; number and weight averaged molecular weight
n_i	=	number of molecules of component i present in the solution or lattice
n_i^c	=	number of chains of type i adopting a conformation defined by c
$n(r)$	=	total number of polymer segments in radial r summed over all lattice layers z
N	=	number of segments in a lattice chain = degree of polymerization of a polymer molecule
N_B, N_{LB}	=	number of bonds in a polymer molecule; number of segment bonds in a lattice chain
p, p_L	=	polymer chain persistence (a measure of stiffness); lattice chain persistence based on lattice geometry
P^0	=	pure component vapour pressure (kPa)
Q	=	canonical partition function (fixed N , V , and T)
r	=	radial position index in cylindrical lattice geometry
$r_i^c(z, r)$	=	number of segments of a chain of type i adopting conformation c that are in lattice radial (z, r)
R	=	root mean squared end-to-end distance of a polymer molecule in solution
R_g	=	radius of gyration; root mean squared distance of segments from the center of mass of a polymer molecule in solution
R_{max}	=	maximum radial dimension in cylindrical lattice

R_{rms}	=	root mean squared distance of chain segments from the cylindrical axis
s	=	segment ranking number
$S(r)$	=	surface area of the outer edge of radial r (lattice units squared)
S, S_m, S_m^{id}	=	entropy; entropy of mixing; ideal entropy of mixing (J/K)
T	=	absolute temperature (K)
u	=	potential of mean force
u'	=	hard core potential (space filling potential)
u^{int}	=	interaction potential
\mathbf{u}	=	vector of iteration variables consisting of potential of mean force values
U	=	internal energy
V_1	=	molar volume of solvent (L/mol)
x_i	=	mole fraction of component i
z	=	layer position index in lattice model
Z_{max}	=	maximum layer position in cylindrical lattice

Greek Letters

Φ	=	volume fraction
Γ	=	experimental surface concentration (g/m ²)
Π	=	osmotic pressure
Ω	=	multiplicity term; total possible number of ways of arranging the system
Ξ	=	grand canonical partition function (fixed μ , V , and T)
$\alpha(z, r)$	=	Lagrange multiplier that ensures lattice sites in position (z, r) are filled completely, but without segment overlap
χ	=	Flory interaction parameter

λ, λ^c	=	lattice step probability; product of step probabilities for a chain adopting conformation c
μ	=	chemical potential
ν	=	proportionality constant in analytical SCF theory
ν_{i+1}	=	number of sites available for placing chain $i+1$ into a lattice already containing i chains
\bar{v}	=	partial specific volume of a dissolved solute (mL/g)
θ	=	surface coverage in equivalent monolayers (or total number of grafted chain segments per surface lattice site)
ρ	=	density (g/mL)
σ	=	lattice model surface grafting density or surface fraction (chains/surface site)
ω_i^c	=	number of ways of placing a single volumeless chain of type i with conformation c into the lattice
ω_{ij}	=	energy associated with contact between one segment of i and one segment of j
$\Delta\omega_{ij}$	=	interchange energy; difference in contact energy between one unlike contact [12] and half the sum of two different like contacts [11], [22]

REFERENCES

1. Alexander, S. (1977) Adsorption of Chain Molecules with a Polar Head: A Scaling Description, *J. Phys. (Paris)*, **38**, 977-987.
2. Andrade, J.D. and V. Hlady (1986) Protein Adsorption and Materials Biocompatibility: A Tutorial Review and Suggested Hypotheses, *Advances in Polymer Science* (K. Dušek, ed.) Springer-Verlag: Berlin, 1-63.
3. Ansarifar, M.A. and P.F. Luckham (1988) Measurement of the Interaction Force Profiles Between Block Copolymers of Poly(2-vinylpyridine)/Poly(t-butylstyrene) in a Good Solvent, *Polymer*, **29**, 329-335.
4. Auroy, P., L. Auvray and L. Leger (1991a) Structures of End-Grafted Polymer Layers: A Small-Angle Neutron Scattering Study, *Macromolecules*, **24**, 2523-2528.
5. Auroy, P., L. Auvray and L. Leger (1991b) Characterization of the Brush Regime for Grafted Polymer Layers at the Solid-Liquid Interface, *Physical Review Letters*, **66**(6), 719-722.
6. Bamford, C.H. and K.G. Al-Lamee (1992) Chemical Methods for Improving the Haemocompatibility of Synthetic Polymers, *Clinical Materials*, **10**, 243-261.
7. Baranowski, R. and M.D. Whitmore (1997) Theory of the Structure of Adsorbed Block Copolymers: Detailed Comparison with Experiment, *J. Chem. Phys.*, **103**(6), 2343-2353.
8. Baskir, J.N., T.A. Hatton and U.W. Suter (1989a) Affinity Partitioning in Two-Phase Aqueous Polymer Systems: A Simple Model for the Distribution of the Polymer-Ligand Tail Segments near the Surface of a Particle, *J. Phys. Chem.*, **93**(2), 969-976.
9. Baskir, J.N., T.A. Hatton and U.W. Suter (1989b) Thermodynamics of the Partitioning of Biomaterials in Two-Phase Aqueous Polymer Systems: Comparison of Lattice Model to Experimental Data, *J. Phys. Chem.*, **93**, 2111-2122.
10. Baskir, J.N., T.A. Hatton and U.W. Suter (1987) Thermodynamics of the Separation of Biomaterials in Two-Phase Aqueous Polymer Systems: Effect of the Phase-Forming Polymers, *Macromolecules*, **20**, 1300-1311.
11. Bayer, E. and W. Rapp (1992) Polystyrene-Immobilized PEG Chains: Dynamics and Application in Peptide Synthesis, Immunology, and Chromatography, *Poly(Ethylene Glycol) Chemistry: Biotechnical and Biomedical Applications* (J.M. Harris, ed.) Plenum Press: New York, 325-345.

12. Bergström, K., K. Holmberg, A. Safran, A.S. Hoffman, M.J. Edgell, A. Kozłowski, B.A. Hovanes and J.M. Harris (1992) Reduction of Fibrinogen Adsorption on PEG-coated Polystyrene Surfaces, *J. Biomedical Materials Research*, **26**, 779-790.
13. Brandrup, J. and E.H. Immergut (1989) *Polymer Handbook*, Wiley: New York.
14. Brent, R.P. (1973) *Algorithms for Minimization Without Derivatives*, Prentice-Hall Inc.: New York.
15. Brooks, D.E. and V.J. Müller (1996) Size Exclusion Phases and Repulsive Protein-Polymer Interaction/Recognition, *J. Molecular Recognition*, **9**, 697-700.
16. Broyden, C.G. (1965) A Class of Methods for Solving Nonlinear Simultaneous Equations, *Mathematical Computing*, **19**, 577-593.
17. Chakrabarti, A., P. Nelson and R.J. Toral (1994) Interpenetrations in Polymer Brushes, *J. Chem. Phys.*, **100**, 748-749.
18. Chakrabarti, A. and R. Toral (1990) Density Profile of Terminally Anchored Polymer Chains: A Monte Carlo Study, *Macromolecules*, **23**, 2016-2021.
19. Claesson, P.M. *et al.* (1996) Techniques for Measuring Surface Forces, *Advances in Colloid and Interface Sci.*, **67**, 119-183.
20. Clayfield, E.J. and E.C. Lumb (1966) A Theoretical Approach for Polymeric Dispersant Action I. Calculation of Entropic Repulsion Exerted by Random Polymer Chains Terminally Adsorbed on Plane Surfaces and Spherical Particles, *J. Colloid Interface Sci.*, **22**, 269-284.
21. Cohen Stuart, M.A. (1980) Ph.D. Thesis, Wageningen Agricultural University.
22. Cosgrove, T., T.G. Heath, J.S. Phipps and R.M. Richardson (1991) Neutron Reflectivity Studies of Polymers Adsorbed on Mica from Solution, *Macromolecules*, **24**, 94-98.
23. Cosgrove, T. (1990a) Volume-Fraction Profiles of Adsorbed Polymers, *J. Chem. Soc. Faraday Trans.*, **86**(9), 1323-1332.
24. Cosgrove, T. and K. Ryan (1990b) NMR and Neutron-Scattering Studies on Poly(ethylene oxide) Terminally Attached at the Polystyrene/Water Interface, *Langmuir*, **6**, 136-142.
25. Cosgrove, T., T. Heath, B. van Lent, F. Leermakers and J. Scheutjens (1987a) Configuration of Terminally Attached Chains at the Solid/Solvent Interface: Self-Consistent Field Theory and a Monte Carlo Model, *Macromolecules*, **20**, 1692-1696.

26. Cosgrove, T., T. Heath, G. Ryan and B. van Lent (1987b) The Conformation of Adsorbed Poly(ethylene oxide) at the Polystyrene/Water Interface, *Polymer Communications*, **28**, 64-65.
27. Davis, S.S. (1997) Biomedical Applications of Nanotechnology - Implications for Drug Targeting and Gene Therapy, *Trends in Biotechnology*, **15**, 217-224.
28. de Gennes, P.-G. (1985) *C.R. Acad. Sci. Paris, Ser. II*, **300**, 839.
29. de Gennes, P.-G. (1980) Conformations of Polymers Attached to an Interface, *Macromolecules*, **13**, 1069-1075.
30. de Gennes, P.-G. (1976) Scaling Theory of Polymer Adsorption, *J. Phys. (Paris)*, **37**, 1443-1452.
31. Dennis, J.E. and R.B. Schnabel (1983) Numerical Methods for Unconstrained Optimization and Nonlinear Equations, Prentice-Hall, Inc.: Englewood Cliffs, N.J.
32. Desai, N.P. and J.A. Hubbell (1991) Biological Responses to Polyethylene Oxide Modified Polyethylene Terephthalate Surfaces, *J. Biomedical Materials Research*, **25**, 829-843.
33. DiMarzio, E.A. and R.J. Rubin (1971) Adsorption of a Chain Polymer between Two Plates, *J. Chem. Phys.*, **55**(9), 4318-4336.
34. Doroszkowski, A. and R. Lambourne (1971) Measurement of the Strength of Steric Barriers in Non-Aqueous Polymer Dispersions, *J. Polymer Sci.: Part C*, **34**, 253-264.
35. Du, H., P. Chandaroy and S.W. Hui (1997) Grafted Poly(ethylene glycol) on Lipid Surfaces Inhibits Protein Adsorption and Cell Adhesion, *Biochimica et Biophysica Acta*, **1326**, 236-248.
36. Dunn, S.E., A. Brindley, S.S. Davis, M.C. Davies and L. Illum (1994) Polystyrene-Poly(Ethylene Glycol) (PS-PEG2000) Particles as Model Systems for Site Specific Drug Delivery. 2. The Effect of PEG Surface Density on the *in Vitro* Cell Interaction and *in Vivo* Biodistribution, *Pharmaceutical Research*, **11**(7), 1016-1022.
37. Elbert, D.L. and J.A. Hubbell (1996) Surface Treatments of Polymers for Biocompatibility, *Annu. Rev. Mater. Sci.*, **26**, 365-394.
38. Evers, O.A., J.M.H.M. Scheutjens and G.J. Fleer (1991) Statistical Thermodynamics of Block Copolymer Adsorption. 3. Interaction between Adsorbed Layers of Block Copolymers, *Macromolecules*, **24**, 5558-5566.

39. Evers, O.A., J.M.H.M. Scheutjens and G.J. Fleer (1990) Statistical Thermodynamics of Block Copolymer Adsorption. 1. Formulation of the Model and Results for the Adsorbed Layer Structure, *Macromolecules*, **23**, 5221-5233.
40. Field, J.B., C. Toprakcioglu, R.C. Ball, H.B. Stanley, L. Dai, W. Barford, J. Penfold, G. Smith and W. Hamilton (1992) Determination of End-Adsorbed Polymer Density Profiles by Neutron Reflectometry, *Macromolecules*, **25**, 434-439.
41. Fleer, G.J., M.A. Cohen Stuart, J.M.H.M. Scheutjens, T. Cosgrove, B. Vincent (1993) *Polymers at Interfaces*, Chapman & Hall: London.
42. Flory, P. (1969) *Statistical Mechanics of Chain Molecules*, John Wiley & Sons, Inc.: New York.
43. Flory, P. (1953) *Principles of Polymer Chemistry*, Cornell University Press: Ithaca, N.Y.
44. Flory, P. (1942) Thermodynamics of High Polymer Solutions, *J. Chem. Phys.*, **10**, 51-61.
45. Gölander, C.G., J.N. Herron, K. Lim, P. Claesson, P. Stenius and J.D. Andrade (1992) Properties of Immobilized PEG Films and the Interaction with Proteins: Experiments and Modeling, *Poly(Ethylene Glycol) Chemistry: Biotechnical and Biomedical Applications* (J.M. Harris, ed.) Plenum Press: New York, 221-245.
46. Gombotz, W.R., W. Guanghai, T.A. Horbett and A.S. Hoffman (1992) Protein Adsorption to and Elution from Polyether Surfaces, *Poly(Ethylene Glycol) Chemistry: Biotechnical and Biomedical Applications* (J.M. Harris, ed.) Plenum Press: New York, 247-261.
47. Gombotz, W.R., W. Guanghai, T.A. Horbett and A.S. Hoffman (1991) Protein Adsorption to Poly(ethylene oxide) Surfaces, *J. Biomedical Materials Research*, **25**, 1547-1562.
48. Grest, G.S. and M. Murat (1993) Structure of Grafted Polymeric Brushes in Solvents of Varying Quality: A Molecular Dynamics Study, *Macromolecules*, **26**, 3108-3117.
49. Guffond, M.C., D.R.M. Williams and E.M. Sevick (1997) End-Tethered Polymer Chains under AFM Tips: Compression and Escape in Theta Solvents, *Langmuir*, **13**(21), 5691-5696.
50. Hadziioannou, G., S. Patel, S. Granick and M. Tirrell (1986) Forces Between Surfaces of Block Copolymers Adsorbed on Mica, *J. American Chemical Society*, **108**, 2869-2876.
51. Haynes, C.A. and W. Norde (1994) Globular Proteins at Solid/Liquid Interfaces, *Colloids and Surfaces B: Biointerfaces*, **2**, 517-566.

52. Haynes, C.A., F.J. Benitez, H.W. Blanch, J.M. Prausnitz (1993) Application of Integral-Equation Theory to Aqueous Two-Phase Partitioning Systems, *AIChE Journal*, **39**, 1539-1557.
53. Haynes, C.A., R.A. Beynon, R.S. King, H.W. Blanch and J.M. Prausnitz (1989) Thermodynamic properties of Aqueous Polymer Solutions: Poly(ethylene glycol)/Dextran, *J. Phys. Chem.*, **93**, 5612-5617.
54. Hesselink, F.T. (1971) On the Theory of the Stabilization of Dispersions by Adsorbed Macromolecules. I. Statistics of the Change of Some Configurational Properties of Adsorbed Macromolecules on the Approach of an Impenetrable Interface, *J. Phys. Chem.*, **75**(1), 65-71.
55. Huang, K. and A.C. Balazs (1993) A Two-Dimensional Self-Consistent-Field Model for Grafted Chains: Determining the Properties of Grafted Homopolymers in Poor Solvents, *Macromolecules*, **26**, 4736-4738.
56. Huggins, M.L. (1942) Some Properties of Solutions of Long Chain Compounds, *J. Phys. Chem.*, **46**, 151-158.
57. Jeon, S.I., J.H. Lee, J.D. Andrade and P.-G. de Gennes (1991a) Protein-Surface Interactions in the Presence of Polyethylene Oxide I. Simplified Theory, *J. Colloid Interface Sci.*, **142**(1), 149-158.
58. Jeon, S.I. and J.D. Andrade (1991b) Protein-Surface Interactions in the Presence of Polyethylene Oxide I. Effect of Protein Size, *J. Colloid Interface Sci.*, **142**(1), 159-166.
59. Johansson, H.O., G. Karlström, F. Tjerneld and C.A. Haynes (1997) Driving Forces for Phase Separation and Partitioning in Aqueous Two-Phase Systems, accepted January, 1997 to *J. Chromatography B*, in press.
60. Kent, M.S., L.T. Lee, B.J. Factor, F. Rondelez and G.S. Smith (1995) Tethered Chains in Good Solvent Conditions: An Experimental Study Involving Langmuir Diblock Copolymer Monolayers, *J. Chem. Phys.*, **103**(6), 2320-2342.
61. Kent, M.S., L.T. Lee, B. Farnoux and R. Rondelez (1992) Characterization of Diblock Copolymer Monolayers at the Liquid-Air Interface by Neutron Reflectivity and Surface Tension Measurements, *Macromolecules*, **25**, 6240-6247.
62. Kenworthy, A.K., K. Hristova, D. Needham and T.J. McIntosh (1995) Range and Magnitude of the Steric Pressure Between Bilayers Containing Phospholipids with Covalently Attached Poly(ethylene glycol), *Biophysical Journal*, **68**, 1921-1936.

63. King, R.S., H.W. Blanch and J.M. Prausnitz (1988) Molecular Thermodynamics of Aqueous Two-Phase Systems for Bioseparations, *AIChE Journal*, **34**(10), 1585-1594.
64. Kishida, A., K. Mishima, E. Corretge, H. Konishi and Y. Ikada (1992) Interactions of Poly(ethylene glycol)-grafted Cellulose Membranes with Proteins and Platelets, *Biomaterials*, **13**(2), 113-118.
65. Kuhn, W. (1934) *Kolloid Z*, **68**, 2.
66. Lai, P.Y. and K. Binder (1992) Structure and Dynamics of Polymer Brushes Near the θ Point: A Monte Carlo Simulation, *J. Chem. Phys.*, **97**(1), 586-595.
67. Lai, P.Y. and K. Binder (1991) Structure and Dynamics of Grafted Polymer Layers: A Monte Carlo Simulation, *J. Chem. Phys.*, **95**(12), 9288-9299.
68. Lee, L.T. and M.S. Kent (1997) Direct Measurement of the Penetration of Free Chains into a Tethered Chain Layer, *Physical Review Letters*, **79**(15), 2899-2902.
69. Lee, L.T., B.J. Factor, M.S. Kent and F. Rondelez (1994) *J. Chem. Soc. Faraday Discuss.*, **98**, 130.
70. Leermakers, F.A.M., J.M.H.M. Scheutjens and J. Lyklema (1990) Statistical Thermodynamics of Association Colloids. IV. Inhomogeneous Membrane Systems, *Biochimica et Biophysica Acta*, **1024**, 139-151.
71. Leermakers, F.A.M. and J.M.H.M. Scheutjens (1988) Statistical Thermodynamics of Association Colloids. I. Lipid Bilayer Membranes, *J. Chem. Phys.*, **89**(5), 3264-3274.
72. Lim, K. and J.N. Herron (1992) Molecular Simulation of Protein-PEG Interaction, *Poly(Ethylene Glycol) Chemistry: Biotechnical and Biomedical Applications* (J.M. Harris, ed.) Plenum Press: New York, 29-56.
73. Llanos, G.R. and M.V. Sefton (1993) Immobilization of Poly(ethylene glycol) onto a Poly(vinyl alcohol) Hydrogel: 2. Evaluation of Thrombogenicity, *J. Biomedical Materials Research*, **27**, 1383-1391.
74. Luckham, P.F. (1996) Recent Advances in Polymers at Surfaces: The Steric Effect, *Current Opinion in Colloid and Interface Science*, **1**, 39-47.
75. Malmsten, M. and J.M. Van Alstine (1996) Adsorption of Poly(Ethylene Glycol) Amphiphiles to Form Coatings Which Inhibit Protein Adsorption, *J. Colloid Interface Sci.*, **177**, 502-512.

76. Martin, J.I. and Z.G. Wang (1995) Polymer Brushes: Scaling, Compression Forces, Interbrush Penetration, and Solvent Size Effects, *J. Phys. Chem.*, **99**, 2833-2844.
77. McMillan, Jr., W.G. and J.E. Mayer (1945) The Statistical Thermodynamics of Multicomponent Systems, *J. Chem. Phys.*, **13**, 276.
78. Meier, D.J. (1967) Theory of Polymeric Dispersants. Statistics of Constrained Polymer Chains, *J. Phys. Chem.*, **71**(6), 1861-1868.
79. Merrill, E.W. (1992) Poly(Ethylene Oxide) and Blood Contact, A Chronicle of One Laboratory, *Poly(Ethylene Glycol) Chemistry: Biotechnical and Biomedical Applications* (J.M. Harris, ed.) Plenum Press: New York, 199-220.
80. Milner, S.T. (1991) Polymer Brushes, *Science*, **251**, 905-914.
81. Milner, S.T., T.A. Witten and M.E. Cates (1988a) Theory of the Grafted Polymer Brush, *Macromolecules*, **21**, 2610-2619.
82. Milner, S.T., T.A. Witten and M.E. Cates (1988b) A Parabolic Density Profile for Grafted Polymers, *Europhysics Letters*, **5**(5), 413-418.
83. Murat, M. and G.S. Grest (1996) Molecular Dynamics Simulations of the Force Between a Polymer Brush and an AFM Tip, *Macromolecules*, **29**, 8282-8284.
84. Murat, M. and G.S. Grest (1991) Interaction Between Grafted Polymeric Brushes, *Computer Simulation of Polymers* (R.J. Roe, ed.) Prentice-Hall Inc.: Englewood Cliffs, N. J., 141-153.
85. Murat, M. and G.S. Grest (1989) Structure of a Grafted Polymer Brush: A Molecular Dynamics Simulation, *Macromolecules*, **22**, 4054-4059.
86. Napper, D.H. (1983) *Polymeric Stabilization of Colloidal Dispersions*, Academic Press: New York.
87. Patel, S., M. Tirrell and G. Hadziioannou (1988) A Simple Model for Forces Between Surfaces Bearing Grafted Polymers Applied to Data on Adsorbed Block Copolymers, *Colloids and Surfaces*, **31**, 157-179.
88. Prausnitz, J.M., R.N. Lichtenthaler and E.G. de Azevedo (1986) *Molecular Thermodynamics of Fluid-Phase Equilibria*, 2nd ed., Prentice-Hall Inc.: Englewood Cliffs, N.J.

89. Privalov, P.L. (1979) Stability of Proteins: Small Globular Proteins, *Adv. Prot. Chem.*, **33**, 167.
90. Rathbone, S.J., C.A. Haynes, H.W. Blanch and J.M. Prausnitz (1990) Thermodynamic Properties of Dilute Aqueous Polymer Solutions from Low-Angle Laser-Light-Scattering Measurements, *Macromolecules*, **23**, 3944-3947.
91. Ruckenstein, E. and B.Q. Li (1997) Steric Interactions between Two Grafted Polymer Brushes, *J. Chem. Phys.*, **107**(3), 932-942.
92. Scales, L.E. (1985) *Introduction fo Non-Linear Optimization*, Springer-Verlag: New York.
93. Scheutjens, J.M.H.M. and G.J. Fleer (1985) Interaction between Two Adsorbed Polymer Layers, *Macromolecules*, **18**, 1882-1900.
94. Scheutjens, J.M.H.M. and G.J. Fleer (1980) Statistical Theory of the Adsorption of Interacting Chain Molecules. 2. Train, Loop and Tail Size Distribution, *J. Phys. Chem.*, **84**, 178-190.
95. Scheutjens, J.M.H.M. and G.J. Fleer (1979) Statistical Theory of the Adsorption of Interacting Chain Molecules. 1. Partition Function, Segment Density Distribution, and Adsorption Isotherms, *J. Phys. Chem.*, **83**, 1619-1635.
96. Schroën, C.G.P.H., M.A. Cohen Stuart, K. van der Voort Maarschalk, A. van der Padt and K. van't Reit (1995) Influence of Preadsorbed Block Copolymers on Protein Adsorption: Surface Properties, Layer Thickness, and Surface Coverage, *Langmuir*, **11**, 3068-3074.
97. Semenov, A.N. (1985) Contribution to the Theory of Microphase Layering in Block Copolymer Melts, *JETP*, **61**, 733.
98. Silberberg, A. (1968) Adsorption of Flexible Macromolecules IV. Effect of Solvent-Solute Interactions, Solute Concentration and Molecular Weight, *J. Chem. Phys.*, **46**, 2835-2851.
99. Subramanian, G., D.R.M. Williams and P.A. Pincus (1996) Interaction between Finite-Sized Particles and End Grafted Polymers, *Macromolecules*, **29**, 4045-4050.
100. Subramanian, G., D.R.M. Williams and P.A. Pincus (1995) Escape Transitions and Force Laws for Compressed Polymer Mushrooms, *Europhysics Letters*, **29**(4), 285-290.
101. Taunton, H.J., C. Toprakcioglu, L.J. Fetters and J. Klein (1990) Interactions between Surfaces Bearing End-Adsorbed Chains in a Good Solvent, *Macromolecules*, **23**, 571-580.

102. Taunton, H.J., C. Toprakcioglu, L.J. Fetters and J. Klein (1988) Forces between Surfaces Bearing Terminally Anchored Polymer Chains in Good Solvents, *Nature*, **332**, 712-714.
103. Tyn, M.T. and T.W. Gusek (1990) Prediction of Diffusion Coefficients of Proteins, *Biotechnology and Bioengineering*, **35**, 327-338.
104. Uchida, E. and Y. Ikada (1997) Topography of Polymer Chains Grafted on a Polymer Surface Underwater, *Macromolecules*, **30**, 5464-5469.
105. Van Alstine, J.M. and M. Malmsten (1997) Poly(ethylene glycol) Amphiphiles: Surface Behavior of Biotechnical Significance, *Langmuir*, **13**, 4044-4053.
106. van Lent, B., R. Israels, J.M.H.M. Scheutjens and G.J. Fleer (1990) Interaction between Hairy Surfaces and the Effect of Free Polymer, *J. Colloid Interface Sci.*, **137**, 380-394.
107. Wijmans, C.M. and B.J. Factor (1996) Self-Consistent Field Calculations of Tethered Chains in the Presence of Mobile Homopolymer: Comparison with Experiment, *Macromolecules*, **29**, 4406-4411.
108. Wijmans, C.M., E.B. Zhulina and G.J. Fleer (1994a) Effect of Free Polymer on the Structure of a Polymer Brush and Interaction between Two Polymer Brushes, *Macromolecules*, **27**, 3238-3248.
109. Wijmans, C.M., F.A.M. Leermakers and G.J. Fleer (1994b) Pair Potentials Between Polymer-Coated Mesoscopic Particles, *Langmuir*, **10**, 4514-4516.
110. Wijmans, C.M., F.A.M. Leermakers and G.J. Fleer (1994c) Chain Stiffness and Bond Correlations in Polymer Brushes, *J. Chem. Phys.*, **101**(9), 8214-8223.
111. Wijmans, C.M., J.M.H.M. Scheutjens and E.B. Zhulina (1992) Self-Consistent Field Theories for Polymer Brushes. Lattice Calculations and an Asymptotic Analytical Description, *Macromolecules*, **25**, 2657-2665.
112. Williams, D.R.M. and F.C. MacKintosh (1995) Polymer Mushrooms Compressed Under Curved Surfaces, *J. Phys. II France*, **5**, 1407-1417.
113. Woodle, M.C. and D.D. Lasic (1992) Sterically Stabilized Liposomes, *Biochimica et Biophysica Acta*, **1113**, 171-199.
114. Yang, Z. and H. Yu (1997) Preserving a Globular Protein Shape on Glass Slides: A Self-Assembled Monolayer Approach, *Advanced Materials*, **9**(5), 426-429.

115. Yeung, C., A.C. Balazs and D. Jasnow (1993) Lateral Instabilities in a Grafted Layer in a Poor Solvent, *Macromolecules*, **26**, 1914-1921.
116. Zhulina, E.B., V.A. Pryamitsyn and O.V. Borisov (1989) Structure and Conformational Transitions in Grafted Polymer Chain Layers. A New Theory, *Polymer Science U.S.S.R.*, **31**(1), 205-216.
117. Zubay, G.L. (1993) *Biochemistry*, Wm. C. Brown Publishers: Dubuque, Iowa.

Appendix A

Fortran Code for Cylindrical SCF Model

```

*****
PROGRAM SCF_CYLINDER
*****
C
C   This program calculates the volume fraction distribution of a
C   grafted polymer, solvent and a grafted particle in a
C   cylindrical geometry according to the Scheutjens and Fler
C   model.
C
C   Reference:  Scheutjens, Fler, Cosgrove, Vincent, Cohen Stuart,
C               "Polymers at Interfaces", Cambridge:  Chapman and
C               Hall, 1993
C
C   By Brad Steels
C
*****
C   **** List of Variables: MAIN ****
C
C   ISEG_B      : LENGTH OF BRUSH MOLECULES
C   ISEG_P      : LENGTH OF PARTICLE MOLECULES
C   BRUSH       : NUMBER OF BRUSH MOLECULES
C   PARTICL     : NUMBER OF PARTICLE MOLECULES
C   ILAY        : NUMBER OF LAYERS IN LATTICE
C   IRAD        : NUMBER OF RADIALS IN LATTICE
C   NSEGS       : NUMBER OF DIFFERENT SEGMENT TYPES IN SYSTEM
C   M           : TOTAL NUMBER OF VARIABLES (ILAY*IRAD*NSEGS)
C   CHIBO       : BRUSH-SOLVENT INTERACTION PARAM.
C   CHIBS       : BRUSH-SURFACE INTERACTION PARAM.
C   CHIBP       : BRUSH-PARTICLE INTERACTION PARAM.
C   CHIPO       : PARTICLE-SOLVENT INTERACTION PARAM.
C   CHIPS       : PARTICLE-SURFACE INTERACTION PARAM.
C   U(i)        : MEAN POTENTIAL (ITERATION VARIABLE)
C   F(i)        : FUNCTION VALUE
C   ENTR(i)     : CONFORMATIONAL ENTROPY
C   ENGY(i)     : INTERACTION ENERGY
C   TOTENG(i)   : HELMHOLTZ ENERGY CHANGE W.R.T. UNMIXED COMPONENTS
C   IPOS1, IPOS2, IPOS
C               : START, FINISH AND CURRENT POSITION OF PARTICLE
C
C   **** Subroutine NEWTON ****
C
C   DFDU(i,j)   : JACOBIAN MATRIX
C   H(i,j)      : INVERSE JACOBIAN
C   FNEW(i)     : NEW FUNCTION VALUES
C   UNEW(i)     : NEW POTENTIAL VALUES
C   DF(i)       : CHANGE IN FUNCTION VALUES FROM LAST ITERATION
C   DU(i)       : CHANGE IN POTENTIAL VALUES FROM LAST ITERATION
C   ALPHA       : FRACTIONAL STEP TAKEN IN SEARCH DIRECTION
C
C   **** Subroutine CYLINDER ****
C
C   L           : NUMBER OF LATTICE SITES IN A GIVEN RADIAL
C               : EQUAL TO  $\pi \cdot (2R-1)$ , R BEING INTEGER POSITION
C   L0,L1       : LATTICE STEP PROBABILITIES IN Z DIRECTION

```

```

C      LR,LR0,LR1 : RADIAL STEP PROBABILITIES (DEPEND ON R)
C      PHIP(z,r) , PHIB(z,r) , PHIO(z,r)
C      : VOLUME FRACTION OF PARTICLE, BRUSH AND SOLVENT
C      GEND(z,r,s) : CHAIN END WEIGHTING FACTORS
C      GTERM(z,r,s): CHAIN END WEIGHTING FACTORS -- GRAFTED CHAIN
C      UOHARD(z,r) , UBHARD(z,r) , UPHARD(z,r)
C      : HARD CORE POTENTIAL FOR SOLVENT, BRUSH AND
C      PARTICLE
C
C *****
      IMPLICIT REAL*8 (A-H,O-Z)
      PARAMETER (MD=2000,MAXZ=50,MAXR=20)
      DIMENSION PHIB(MAXZ,MAXR) , PHIO(MAXZ,MAXR) , PHIP(MAXZ,MAXR) ,
1      U(MD) , ENTR(MAXZ) , ENGY(MAXZ) , TOTENG(MAXZ)
      COMMON/PARAMS/CHIBO,CHIBP,CHIBS,CHIPO,CHIPS,CHIOS,BRUSH,
1      PARTICL,NSEGS
      COMMON/POSITION/IPOS1,IPOS2,IPOS
C
      OPEN (UNIT=14,FILE='OUT.DAT')
      OPEN (UNIT=1,FILE='LOG')
C
      CALL INPUTS(ILAY,IRAD,ISEG_B,ISEG_P,M)
C
      MAXIT = 1000
C
      START_TIME = F_TIME( )
C
      Loop to move particle position.
C
      DO I = IPOS2, IPOS1, -1
        IPOS = I
C
        CALL INITIALIZE(M,ILAY,IRAD,U)
C
        CALL NEWTON(M,U,ILAY,IRAD,ISEG_B,ISEG_P,MAXIT,
1        PHIB,PHIP,PHIO)
C
        CALL ENERGY(U,ILAY,IRAD,ISEG_B,ISEG_P,PHIO,PHIB,PHIP,
1        ENTR(I),ENGY(I),TOTENG(I))
C
        FINAL = (F_TIME( ) - START_TIME)
        I_MIN = INT(FINAL/60)
        I_SEC = INT(FINAL - I_MIN*60)
C
        CALL OUTPUT(ILAY,IRAD,ISEG_B,ISEG_P,U,PHIB,PHIP,PHIO,
1        I_MIN,I_SEC,M,ENTR,ENGY,TOTENG)
C
      END DO
C
      CLOSE (UNIT=14)
      CLOSE (UNIT=1)
C
      END
C

```

```

*****
      SUBROUTINE INPUTS (ILAY,IRAD,ISEG_B,ISEG_P,M)
C      Parameters necessary for execution are read from the input
C      file and printed to the screen and output file.
*****
      IMPLICIT REAL*8 (A-H,O-Z)
      COMMON/PARAMS/CHIBO,CHIBP,CHIBS,CHIPO,CHIPS,CHIOS,BRUSH,
1      PARTICL,NSEGS
      COMMON/POSITION/IPOS1,IPOS2,IPOS

C      OPEN ( UNIT = 10, FILE = 'in1.dat')

C      READ(10,*) NSEGS
      READ(10,*) ISEG_B
      READ(10,*) ISEG_P
      READ(10,*) ILAY
      READ(10,*) IRAD
      READ(10,*) IPOS1      !START POSITION OF PARTICLE CENTER
      READ(10,*) IPOS2      !END POSITION OF PARTICLE CENTER
      READ(10,*) CHIBO
      READ(10,*) CHIBS
      READ(10,*) CHIBP
      READ(10,*) CHIPPO
      READ(10,*) CHIPS
      CHIOS = 0.D0
      READ(10,*) SURDEN      !PERCENT SURFACE DENSITY
      READ(10,*) PARTICL

C      CLOSE(UNIT=10)

C      M = ILAY * IRAD * NSEGS
      BRUSH = SURDEN / 1.D2 * 3.14159D0 * DBLE(IRAD)**2.D0

C      WRITE(6,'(2X, A39,I4 )')
1      'VALUE FOR GRAFTED CHAIN LENGTH          ', ISEG_B
      WRITE(6,'(2X,A39,I4)')
1      'VALUE FOR PARTICLE CHAIN LENGTH          ', ISEG_P
      WRITE(6,'(2X,A39,I4)')
1      'VALUE FOR CYLINDRICAL LATTICE LENGTH      ', ILAY
      WRITE(6,'(2X,A39,I4)')
1      'VALUE FOR CYLINDER RADIUS                  ', IRAD
      WRITE(6,'(2X,A39,I4)')
1      'START POSITION FOR PARTICLE                  ', IPOS1
      WRITE(6,'(2X,A39,I4)')
1      'END POSITION FOR PARTICLE                    ', IPOS2
      WRITE(6,'(2X,A39,G12.4)')
1      'BRUSH-SOLVENT INTERACTION PARAMETER        ', CHIBO
      WRITE(6,'(2X,A39,G12.4)')
1      'BRUSH-SURFACE INTERACTION PARAMETER        ', CHIBS
      WRITE(6,'(2X,A39,G12.4)')
1      'BRUSH-PARTICLE INTERACTION PARAMETER        ', CHIBP
      WRITE(6,'(2X,A39,G12.4)')
1      'PARTICLE-SOLVENT INTERACTION PARAMETER      ', CHIPPO
      WRITE(6,'(2X,A39,G12.4)')

```

```

1  'PARTICLE-SURFACE INTERACTION PARAMETER ', CHIPS
WRITE(6,'(2X,A39,G12.4)')
1  'SURF DENS. OF BRUSH MOLECULES          ', SURDEN
WRITE(6,'(2X,A39,G12.4)')
1  'NUMBER OF BRUSH MOLECULES              ', BRUSH
WRITE(6,'(2X,A39,G12.4)')
1  'NUMBER OF PARTICLE MOLECULES          ', PARTICL
WRITE(6,'(2X,A39,I4)')
1  'NUMBER OF ITERATION VARIABLES         ', M

```

C

```

WRITE(14,'(2X, A39,I4 )')
1  'VALUE FOR GRAFTED CHAIN LENGTH        ', ISEG_B
WRITE(14,'(2X,A39,I4)')
1  'VALUE FOR PARTICLE CHAIN LENGTH       ', ISEG_P
WRITE(14,'(2X,A39,I4)')
1  'VALUE FOR CYLINDRICAL LATTICE LENGTH  ', ILAY
WRITE(14,'(2X,A39,I4)')
1  'VALUE FOR CYLINDER RADIUS             ', IRAD
WRITE(14,'(2X,A39,I4)')
1  'START POSITION FOR PARTICLE            ', IPOS1
WRITE(14,'(2X,A39,I4)')
1  'END POSITION FOR PARTICLE              ', IPOS2
WRITE(14,'(2X,A39,G12.4)')
1  'BRUSH-SOLVENT INTERACTION PARAMETER   ', CHIBO
WRITE(14,'(2X,A39,G12.4)')
1  'BRUSH-SURFACE INTERACTION PARAMETER   ', CHIBS
WRITE(14,'(2X,A39,G12.4)')
1  'BRUSH-PARTICLE INTERACTION PARAMETER  ', CHIBP
WRITE(14,'(2X,A39,G12.4)')
1  'PARTICLE-SOLVENT INTERACTION PARAMETER ', CHIPO
WRITE(14,'(2X,A39,G12.4)')
1  'PARTICLE-SURFACE INTERACTION PARAMETER ', CHIPS
WRITE(14,'(2X,A39,G12.4)')
1  'SURF DENS. OF BRUSH MOLECULES        ', SURDEN
WRITE(14,'(2X,A39,G12.4)')
1  'NUMBER OF BRUSH MOLECULES IN LATTICE  ', BRUSH
WRITE(14,'(2X,A39,G12.4)')
1  'NUMBER OF PARTICLE MOLECULES         ', PARTICL
WRITE(14,'(2X,A39,I4)')
1  'NUMBER OF ITERATION VARIABLES         ', M

```

C

```

RETURN
END

```

C

```

*****
SUBROUTINE NEWTON(M,U,ILAY,IRAD,ISEG_B,ISEG_P,MAXIT,
1  PHIB,PHIP,PHIO)
*****
IMPLICIT REAL*8 (A-H,O-Z)
PARAMETER (MD=2000,MAXZ=50,MAXR=20)
EXTERNAL FUNLIN
DIMENSION U(MD), F(MD), DFDU(MD,MD), FNEW(MD), UNEW(MD), DU(MD),
1  DF(MD), H(MD,MD), PHIB(MAXZ,MAXR), PHIO(MAXZ,MAXR),
2  PHIP(MAXZ,MAXR)

```



```

C      TOL = 1.D-7
      ITERS = 0
C
C      Initialize parameters for the line search routine.
C
      XI = 1.D-3
      XF = 7.D-1
      XTOL = 1.D-5
      FTOL = 1.D-6
      IMAX = 5
C
C      Carry out an initial function evaluation.
C
      CALL CYLINDER(U,ILAY,IRAD,ISEG_B,ISEG_P,F,PHIB,PHIP,PHIO)
      SUMSQR = SSQ(F,M)
C
      WRITE(6,*)
      WRITE(6,*) ' CALCULATING JACOBIAN '
C
      CALL NUM_DRIV(F,U,ILAY,IRAD,ISEG_B,ISEG_P,M,PHIB,PHIP,
1          PHIO,DFDU)
C
      WRITE(6,*)
      WRITE(6,*) ' CALCULATING INVERSE OF JACOBIAN '
C
      CALL MATINV(DFDU,M,H,IERROR)
C
      WRITE(6,*)
      WRITE(6,*) ' SEARCHING FOR SOLUTION OF NONLINEAR SYSTEM '
      WRITE(6,*)
      WRITE(6,*) ' ITERS ', ' SSQ (old)      (new) ', ' ALPHA'
      WRITE(1,*) ' ITERS ', ' SSQ (old)      (new) ', ' ALPHA'
C
      DO WHILE ( SQRT(SUMSQR) .GT. TOL )
        ITERS = ITERS + 1
        IF (ITERS .GT. MAXIT) THEN
          RETURN
        END IF
C
C      Obtain the search direction DU from H and F.
C
        DO 20 I = 1, M
          SUM = 0.D0
          DO 10 J = 1, M
            SUM = SUM - H(I,J) * F(J)
10          CONTINUE
          DU(I) = SUM
20          CONTINUE
C
        DO 25 I = 1, M
          FNEW(I) = F(I)
          UNEW(I) = U(I)
25          CONTINUE

```

```

C
C      Carry out the linear search in the direction DU.
C
      CALL LINSRCH(FUNLIN,XI,XF,XTOL,FTOL,IMAX,FNEW,UNEW,PHIB,PHIP,
1          PHIO,ILAY,IRAD,ISEG_B,ISEG_P,M,DU,SSQNEW,X,IERR)
C
      WRITE(6,30) ITTERS, SUMSQ, SSQNEW, X
      WRITE(1,30) ITTERS, SUMSQ, SSQNEW, X
30      FORMAT(I5,3(G15.5))
C
C      Update the function and variable values using X (alpha).
C
      DO 40 I = 1, M
          DF(I) = FNEW(I) - F(I)
          F(I) = FNEW(I)
          U(I) = UNEW(I)
          DU(I) = X * DU(I)
40      CONTINUE
      SUMSQ = SSQNEW
C
C      Update the inverse Jacobian using the new function values
C
      CALL APROX_DRIV(DF,DU,M,H)
C
      END DO
      RETURN
      END
C
*****
      DOUBLE PRECISION FUNCTION FUNLIN(X,U,ILAY,IRAD,ISEG_B,ISEG_P,
1          M,DU,F,PHIB,PHIP,PHIO)
C      Function called by LINSRCH to minimize SSQ w.r.t. X.
*****
      IMPLICIT REAL*8 (A-H,O-Z)
      PARAMETER (MD=2000,MAXZ=50,MAXR=20)
      DIMENSION DU(MD), U(MD), F(MD), UU(MD), PHIB(MAXZ,MAXR),
1          PHIO(MAXZ,MAXR), PHIP(MAXZ,MAXR)
      COMMON/LINEAR/UU
C
C      Update the temporary variable UU and try a function evaluation.
C
      DO 10 I = 1, M
          UU(I) = U(I) + X * DU(I)
10      CONTINUE
      CALL CYLINDER(UU,ILAY,IRAD,ISEG_B,ISEG_P,F,PHIB,PHIP,PHIO)
      FUNLIN = SSQ(F,M)
C
      RETURN
      END
C
*****
      SUBROUTINE LINSRCH(FUNC,XI,XF,XTOL,FTOL,IMAX,F,UP,PHIB,PHIP,
1          PHIO,ILAY,IRAD,ISEG_B,ISEG_P,NVAR,DU,Y,X,IERR)
C      Carries out a univariate minimization on the sum of squares

```

```

C      with respect to the step fraction, X, in the search direction.
*****
      IMPLICIT REAL*8 (A-H,O-Z)
      REAL*8 M
      PARAMETER (MD=2000,MAXZ=50,MAXR=20)
      DIMENSION F(MD), UP(MD), DU(MD), UU(MD), PHIB(MAXZ,MAXR),
1          PHIP(MAXZ,MAXR), PHIO(MAXZ,MAXR)
      COMMON/LINEAR/UU
      EXTERNAL FUNC
C
C      Initialize the search interval on A and B.
C      X has the least value of F, W the next lowest and V the
C      previous value of W. U is the current evaluation point.
C
      A = XI
      B = XF
      C = (3.D0 - DSQRT(5.D0)) / 2.D0
      V = A + C * (B-A)
      W = V
      X = V
      E = 0.D0
      FV = FUNC(V,UP,ILAY,IRAD,ISEG_B,ISEG_P,NVAR,DU,F,PHIB,
1          PHIP,PHIO)
      FW = FV
      FX = FV
      IFEVAL = 0
      IERR = 0
      M = 0.D0
      T2 = 0.D0
C
C      Check the stopping criteria for a local minimum.
C
      DO WHILE ( DABS(X-M) .GT. (T2- (.5D0*(B-A))) )
C
          IFEVAL = IFEVAL + 1
C
C      Check for maximum number of interpolations.
C
          IF (IFEVAL .GT. IMAX) THEN
              IERR = 1
              Y = FX
              DO 10 I = 1, NVAR
                  UP(I) = UU(I)
10          CONTINUE
              RETURN
          END IF
C
          M = .5D0 * (A+B)
          TOL = XTOL * DABS(X) + FTOL      ! Relative and absolute criteria
          T2 = 2 * TOL
          P = 0.D0
          Q = P
          R = P
          IF ( DABS(E) .GT. TOL ) THEN      ! Parabolic Interpolation

```

```

R = (X-W) * (FX-FV)
Q = (X-V) * (FX-FW)
P = (X-V) * Q - (X-W) * R
Q = 2 * (Q-R)
IF ( Q .GT. 0.D0 ) THEN
  P = -P
ELSE
  Q = -Q
END IF
R = E
E = D
END IF
IF ( DABS(P) .LT. DABS(.5D0*Q*R) .AND. P .GT. (Q*(A-X))
1  .AND. P .LT. (Q*(B-X)) ) THEN
  D = P / Q
  U = X + D                                ! Take a quadratic step
C
C  Cannot evaluate F too close to A or B.
C
  IF ( (U-A) .LT. T2 .OR. (B-U) .LT. T2 ) THEN
    D = TOL
    IF ( X .GE. M ) D = D * (-1.D0)
  END IF
ELSE
  IF ( X .LT. M ) THEN                      ! Golden Section step taken
    E = B - X
  ELSE
    E = A - X
  END IF
  D = C * E
C
C  Cannot evaluate F too close to X.
C
  IF ( DABS(D) .GE. TOL ) THEN
    U = X + D
  ELSEIF ( D .GT. 0.D0 ) THEN
    U = X + TOL
  ELSE
    U = X - TOL
  END IF
END IF
FU = FUNC(U,UP,ILAY,IRAD,ISEG_B,ISEG_P,NVAR,DU,F,PHIB,PHIP,PHIO)
C
C  Update the values of a, b, v, w, and x.
C
  IF ( FU .LE. FX ) THEN
    IF ( U .LT. X ) THEN
      B = X
      FB = FX
    ELSE
      A = X
      FA = FX
    END IF
    V = W

```

```

      FV = FW
      W = X
      FW = FX
      X = U
      FX = FU
    ELSE
      IF ( U .LT. X ) THEN
        A = U
        FA = FU
      ELSE
        B = U
        FB = FU
      END IF
      IF ( FU .LE. FW .OR. W .EQ. X ) THEN
        V = W
        FV = FW
        W = U
        FW = FU
      ELSEIF ( FU .LE. FV .OR. V .EQ. X .OR. V .EQ. W ) THEN
        V = U
        FV = FU
      END IF
    END IF
  END DO
  Y = FX
  DO 100 I = 1, NVAR
    UP(I) = UU(I)
100  CONTINUE
C
  RETURN
END

C
*****
SUBROUTINE APROX_DRIV(DF,DU,M,H)
C  Update the inverse Jacobian using Broyden's update.
*****
  IMPLICIT REAL*8(A-H,O-Z)
  PARAMETER (MD=2000)
  DIMENSION H(MD,MD), DU(M), DF(M), HDF(MD), DUH(MD)
  DO 20 I = 1, M
    SUM = 0.D0
    DO 10 J = 1, M
      SUM = SUM + H(I,J) * DF(J)
10    CONTINUE
    HDF(I) = SUM
20  CONTINUE
  DENOM = 0.D0
  DO 40 I = 1, M
    SUM = 0.D0
    DO 30 J = 1, M
      SUM = SUM + DU(J) * H(J,I)
30    CONTINUE
    DUH(I) = SUM
    DENOM = DENOM + SUM * DF(I)

```

```

40    CONTINUE
      DO 80 I = 1, M
        DO 70 J = 1, M
          ADD = (HDF(I) - DU(I)) * DUH(J) / DENOM
          H(I,J) = H(I,J) - ADD
60    CONTINUE
70    CONTINUE
80    CONTINUE
      RETURN
      END

C
*****
      SUBROUTINE NUM_DRIV(F,U,ILAY,IRAD,ISEG_B,ISEG_P,M,PHIB,PHIP,
1      PHIO,DFDU)
C      Derivatives are approximated by finite differences. A relative
C      step size, DELU, of about SQRT(machine precision)*U is used and
C      if U is zero, then a step size of SQRT(machine precision) is
C      used. In double precision, machine precision = 2.2e-16
*****
      IMPLICIT REAL*8(A-H,O-Z)
      PARAMETER (MD=2000,MAXZ=50,MAXR=20)
      DIMENSION U(MD), DFDU(MD,MD), F(MD), F2(MD),
1      PHIB(MAXZ,MAXR), PHIP(MAXZ,MAXR), PHIO(MAXZ,MAXR)
C
      DO 20 I = 1, M
        DUM = U(I)
        DELU = 1.D-8 * U(I)
        IF ( DELU .EQ. 0. ) DELU = 1.D-8
        U(I) = U(I) + DELU
        CALL CYLINDER(U,ILAY,IRAD,ISEG_B,ISEG_P,F2,PHIB,PHIP,PHIO)
        DO 10 J = 1, M
          DFDU(J,I) = (F2(J)-F(J)) / DELU
10    CONTINUE
        U(I) = DUM
20    CONTINUE
C
      RETURN
      END

C
*****
      DOUBLE PRECISION FUNCTION SSQ(F,M)
C      Evaluates the sum of squares of the functions.
*****
      IMPLICIT REAL*8(A-H,O-Z)
      PARAMETER (MD=2000)
      DIMENSION F(MD)
      SUM = 0.D0
      DO 10 I = 1, M
        SUM = SUM + F(I)**2
10    CONTINUE
      SSQ = SUM
      RETURN
      END

C
*****

```

```

      SUBROUTINE INITIALIZE(M,ILAY,IRAD,U)
C      Initializes the potential values, sets step probabilities,
C      sets indexing values, and calculates lattice sites in each
C      radial.
*****
      IMPLICIT REAL*8 (A-H,O-Z)
      REAL*8 L,L1,L0,LR,LR0,LR1
      PARAMETER (MD=2000,MAXR=20)
      DIMENSION U(MD), L(MAXR), LR(MAXR), LR0(MAXR), LR1(MAXR)
      COMMON/INDEX/ISTAR1,ISTAR2,ISTAR3
      COMMON/SITES/PI,L
      COMMON/STEPPROB/L1,L0,LR,LR0,LR1
C
      DO 10 I = 1, M
        U(I) = 0.D0
10     CONTINUE
      DO 15 I = 1, IRAD
        U(IRAD*ILAY+I) = 1.D-1
15     CONTINUE
C
C      Assign the lattice step weighting factors.
C
      L1 = 2.5D-1
      L0 = 5.D-1
      DO 20 I = 1, IRAD
        LR(I) = (DBLE(I)-1.D0) / (4.D0*DBLE(I)-2.D0)
        LR1(I) = DBLE(I) / (4.D0*DBLE(I)-2.D0)
        LR0(I) = 1.D0 - LR(I) - LR1(I)
20     CONTINUE
      LR1(IRAD) = LR(IRAD)
      LR0(IRAD) = 1.D0 - 2.D0*LR(IRAD)
C
C      Calculate the indexing positions, and the number of
C      sites per radial in the cylinder.
C
      ISTAR1 = 0
      ISTAR2 = ILAY * IRAD
      ISTAR3 = 2 * ISTAR2
      PI = 4.D0 * DATAN(1.D0)
      DO 30 J = 1, IRAD
        L(J) = PI * ( 2.D0 * DBLE(J) - 1.D0 )
30     CONTINUE
C
      RETURN
      END
C
*****
      SUBROUTINE CYLINDER(U,ILAY,IRAD,ISEG_B,ISEG_P,F,PHIB,PHIP,PHIO)
C      Subroutine to calculate the volume fraction distribution of
C      a polymer brush, grafted particle and solvent in a cylindrical
C      geometry, based on the SF model. U and F are indexed vectors
C      representing a 2D distribution. They are organized by layer,
C      such that the first IRAD values represent the solvent potential
C      in each radial for the first layer, followed by the second layer

```

```

C      for IRAD values and so on. Once the lattice is completed for
C      the solvent, the sequence is repeated for the brush and then
C      the particle. The indexing is started in the correct position
C      by the ISTART value.
*****
      IMPLICIT REAL*8 (A-H,O-Z)
      PARAMETER (MD=2000,MAXZ=50,MAXR=20,MAXS=500)
      REAL*8 L1,L0,LR,LR0,LR1
      DIMENSION U(MD), F(MD), PHIB(MAXZ,MAXR), PHIO(MAXZ,MAXR),
1          PHIP(MAXZ,MAXR), LR(MAXR), LR0(MAXR), LR1(MAXR),
2          GEND(MAXZ,MAXR,MAXS), GTERM(MAXZ,MAXR,MAXS),
3          UOHARD(MAXZ,MAXR), UBHARD(MAXZ,MAXR), UPHARD(MAXZ,MAXR)
      COMMON/PARAMS/CHIBO,CHIBP,CHIBS,CHIPO,CHIPS,CHIOS,BRUSH,
1          PARTICL,NSEGS
      COMMON/POSITION/IPOS1,IPOS2,IPOS
      COMMON/INDEX/ISTAR1,ISTAR2,ISTAR3
      COMMON/STEPPROB/L1,L0,LR,LR0,LR1
      COMMON/BULK/BULKO,BULKB,BULKP
C
C      Calculate the solvent volume fraction distribution.
C      ( phi(z,r) = G(z,r) for monomeric solvent )
C
      BULKO = 1.D0
      DO 30 I = 1, ILAY
          IMO = I - 1
          DO 20 J = 1, IRAD
              PHIO(I,J) = EXP ( -U(IMO*IRAD+J) )
20          CONTINUE
30          CONTINUE
C
C      Assign the correct free segment weighting factors for the
C      brush.
C
      ISTART = ISTAR2          ! Index proper location in list.
      DO 50 I = 1, ILAY
          IMO = I - 1
          DO 40 J = 1, IRAD
              GEND(I,J,1) = EXP( -U(ISTART + IMO*IRAD + J) )
40          CONTINUE
50          CONTINUE
C
C      Calculate the chain end distribution functions for free chains.
C
      CALL ENDDIST(ILAY,IRAD,ISEG_B,GEND)
C
C      Assign the correct free segment weighting factors for
C      terminally attached chains. This "grafts" the chains to the
C      first layer of the lattice.
C
      DO 70 I = 2, ILAY
          DO 60 J = 1, IRAD
              GTERM(I,J,1) = 0.D0
60          CONTINUE
70          CONTINUE

```



```

DO 75 J = 1, IRAD
    GTERM(1,J,1) = GEND(1,J,1)
75 CONTINUE
C
C Calculate the chain end distribution functions for grafted
C chains. Combine the chain end weighting factors from free
C and grafted chains to return the segment density distribution.
C
CALL VOLFRAC(ILAY,IRAD,ISEG_B,GEND,GTERM,BRUSH,PHIB,BULKB)
C
C Assign the correct free segment weighting factors for the
C particle.
C
ISTART = ISTAR3           ! Index proper location in list.
DO 150 I = 1, ILAY
    IMO = I - 1
    DO 140 J = 1, IRAD
        GEND(I,J,1) = EXP( -U(ISTART + IMO*IRAD + J) )
140 CONTINUE
150 CONTINUE
C
C Calculate the chain end distribution function for the
C particle.
C
CALL ENDDIST(ILAY,IRAD,ISEG_P,GEND)
C
DO 170 I = 1, ILAY
    DO 160 J = 1, IRAD
        GTERM(I,J,1) = 0.D0
160 CONTINUE
170 CONTINUE
C
C Assign the correct segment weighting factors for the grafted
C particle. i.e. specify the position of the particle
C
GTERM(IPOS,1,1) = GEND(IPOS,1,1)
C
C Calculate the chain end distribution functions for a grafted
C particle. Combine the chain end weighting factors from free
C and grafted particle to return the segment density
C distribution.
C
CALL VOLFRAC(ILAY,IRAD,ISEG_P,GEND,GTERM,PARTICL,PHIP,BULKP)
C
C Calculate the interaction energies, and the average
C hard core potential for the solvent, brush and particle.
C
ISTART = ISTAR1
CALL HCPOT(U,ISTART,ILAY,IRAD,PHIB,PHIP,CHIBO,CHIPO,CHIOS,
1          UOHARD)
ISTART = ISTAR2
CALL HCPOT(U,ISTART,ILAY,IRAD,PHIO,PHIP,CHIBO,CHIBP,CHIBS,
1          UBHARD)
ISTART = ISTAR3

```

```

      CALL HCPOT(U, ISTART, ILAY, IRAD, PHIO, PHIB, CHIPO, CHIBP, CHIPS,
1          UPHARD)
C
C      Calculate the function values based on the segment density
C      distribution and average hard core potentials.
C
      DO 270 I = 1, ILAY
          IMO = I - 1
          DO 260 J = 1, IRAD
              AVG = ( UOHARD(I,J) + UBHARD(I,J) + UPHARD(I,J) ) /
1                  DBLE(NSEGS)
              F(IMO*IRAD+J) = 1.D0 - 1.D0/(PHIO(I,J)+PHIB(I,J)+PHIP(I,J))
1                  + AVG - UOHARD(I,J)
              F(ISTAR2+IMO*IRAD+J) = 1.D0 - 1.D0/(PHIO(I,J)+PHIB(I,J)+
1                  PHIP(I,J)) + AVG - UBHARD(I,J)
              F(ISTAR3+IMO*IRAD+J) = 1.D0 - 1.D0/(PHIO(I,J)+PHIB(I,J)+
1                  PHIP(I,J)) + AVG - UPHARD(I,J)
260      CONTINUE
270      CONTINUE
          RETURN
      END
C
*****
      SUBROUTINE ENDDIST(ILAY, IRAD, ISEG, GEND)
C      Subroutine to calculate the chain end distribution function.
C      KEY values handle the reflecting boundary conditions at IRAD
C      and ILAY, as well as solid boundary at z = 0.
*****
      IMPLICIT REAL*8 (A-H,O-Z)
      REAL*8 L1, L0, LR, LR0, LR1, KEY1, KEY2A, KEY2B, KEY3A, KEY3B
      PARAMETER (MAXZ=50, MAXR=20, MAXS=500)
      DIMENSION GEND(MAXZ, MAXR, MAXS), LR(MAXR), LR0(MAXR), LR1(MAXR)
      COMMON/STEPPROB/L1, L0, LR, LR0, LR1
C
      ISMO = ISEG - 1
      IF ( ISMO .EQ. 0 ) RETURN
      DO 90 N = 1, ISMO
          NPO = N + 1
          KEY1 = 0.D0
          KEY2A = 0.D0
          KEY2B = 1.D0
          KEY3A = 0.D0
          KEY3B = 1.D0
          DO 70 I = 1, ILAY
              IPO = I + 1
              IMO = I - 1
              IF (I .EQ. ILAY) THEN
                  KEY2A = 1.D0
                  KEY2B = 0.D0
              END IF
              DO 60 J = 1, IRAD
                  JPO = J + 1
                  JMO = J - 1
                  IF (J .EQ. IRAD) THEN

```

```

        KEY3A = 1.D0
        KEY3B = 0.D0
      END IF
      GEND(I,J,NPO) = GEND(I,J,1) * ((L1 * KEY1 * (LR(J) *
1      GEND(IMO,JMO,N) + (LR0(J) + KEY3A * LR1(J)) *
2      GEND(IMO,J,N) + LR1(J) * KEY3B * GEND(IMO,JPO,N))) +
3      ((L0 + KEY2A * L1) * (LR(J) * GEND(I,JMO,N) + (LR0(J)
4      + KEY3A * LR1(J)) * GEND(I,J,N) + LR1(J) * KEY3B *
5      GEND(I,JPO,N))) + (L1 * KEY2B * (LR(J) * GEND(IPO,JMO,N)
6      + (LR0(J) + KEY3A * LR1(J)) * GEND(IPO,J,N) + LR1(J) *
7      KEY3B * GEND(IPO,JPO,N))))
60      CONTINUE
        KEY1 = 1.D0
        KEY3A = 0.D0
        KEY3B = 1.D0
70      CONTINUE
90      CONTINUE
      RETURN
    END

C
*****
      SUBROUTINE VOLFRAC(ILAY,IRAD,ISEG,GEND,GTERM,RNUM,PHI,BULK)
C      Subroutine to calculate the chain end distribution function
C      of grafted chains. Composition Law is then used to generate
C      the segment density distribution.
*****
      IMPLICIT REAL*8 (A-H,O-Z)
      REAL*8 L, L1, L0, LR, LR0, LR1, KEY1, KEY2A, KEY2B, KEY3A, KEY3B
      PARAMETER (MAXZ=50,MAXR=20,MAXS=500)
      DIMENSION GEND(MAXZ,MAXR,MAXS), GTERM(MAXZ,MAXR,MAXS), LR(MAXR),
1      LR0(MAXR), LR1(MAXR), PHI(MAXZ,MAXR), L(MAXR)
      COMMON/STEPPROB/L1,L0,LR,LR0,LR1
      COMMON/SITES/PI,L

C
      ISMO = ISEG - 1
      IF ( ISMO .NE. 0 ) THEN
        DO 150 N = 1, ISMO
          NPO = N + 1
          KEY1 = 0.D0
          KEY2A = 0.D0
          KEY2B = 1.D0
          KEY3A = 0.D0
          KEY3B = 1.D0
          DO 140 I = 1, ILAY
            IPO = I + 1
            IMO = I - 1
            IF (I .EQ. ILAY) THEN
              KEY2A = 1.D0
              KEY2B = 0.D0
            END IF
            DO 130 J = 1, IRAD
              JPO = J + 1
              JMO = J - 1
              IF (J .EQ. IRAD) THEN

```

```

        KEY3A = 1.D0
        KEY3B = 0.D0
        END IF
        GTERM(I,J,NPO) = GEND(I,J,1) * ((L1 * KEY1 * (LR(J) *
1      GTERM(IMO,JMO,N) + (LR0(J) + KEY3A * LR1(J)) *
2      GTERM(IMO,J,N) + LR1(J) * KEY3B * GTERM(IMO,JPO,N))) +
3      ((L0 + KEY2A * L1) * (LR(J) * GTERM(I,JMO,N) + (LR0(J)
4      + KEY3A * LR1(J)) * GTERM(I,J,N) + LR1(J) * KEY3B *
5      GTERM(I,JPO,N))) + (L1 * KEY2B * (LR(J) * GTERM(IPO,JMO,N)
6      + (LR0(J) + KEY3A * LR1(J)) * GTERM(IPO,J,N) + LR1(J) *
7      KEY3B * GTERM(IPO,JPO,N))))
130      CONTINUE
        KEY1 = 1.D0
        KEY3A = 0.D0
        KEY3B = 1.D0
140      CONTINUE
150      CONTINUE
        END IF
C
C      Calculate the normalization constant for grafted molecules.
C
        SUM = 0.D0
        DO 170 J = 1, IRAD
            JMO = J - 1
            DO 160 I = 1, ILAY
                SUM = SUM + L(J) * GTERM(I,J,ISEG)
160          CONTINUE
170        CONTINUE
        GR1 = SUM
        C = RNUM / GR1
        BULK = ISEG * C
C
C      Calculate the volume fraction profile of the brush.
C
        DO 200 I = 1, ILAY
            DO 190 J = 1, IRAD
                SUM = 0.D0
                DO 180 N = 1, ISEG
                    SUM = SUM + GTERM(I,J,N) * GEND(I,J,ISEG-N+1) /
1          GEND(I,J,1)
180          CONTINUE
                PHI(I,J) = C * SUM
190          CONTINUE
200        CONTINUE
C
        RETURN
        END
C
*****
        SUBROUTINE HCPOT(U,ISTART,ILAY,IRAD,PHI1,PHI2,CHI1,CHI2,CHIS,
1          UHARD)
C      Subroutine to calculate the hard core potential for a given
C      segment type. The interaction potential for is subtracted
C      from the total potential, u' = u - u(int)

```

```

      IMPLICIT REAL*8 (A-H,O-Z)
      REAL*8 L1, L0, LR, LR0, LR1, KEY1, KEY2A, KEY2B, KEY3A, KEY3B
      PARAMETER (MD=2000,MAXZ=50,MAXR=20)
      DIMENSION U(MD), UHARD(MAXZ,MAXR), LR(MAXR), LR0(MAXR),
1      LR1(MAXR), PHI1(MAXZ,MAXR), PHI2(MAXZ,MAXR)
      COMMON/STEPPROB/L1,L0,LR,LR0,LR1

```

C

```

      KEY1 = 0.D0
      KEY2A = 0.D0
      KEY2B = 1.D0
      KEY3A = 0.D0
      KEY3B = 1.D0
      DO 230 I = 1, ILAY
        IMO = I - 1
        IF (I .EQ. ILAY) THEN
          KEY2A = 1.D0
          KEY2B = 0.D0
        END IF
        DO 220 J = 1, IRAD
          IF (J .EQ. IRAD) THEN
            KEY3A = 1.D0
            KEY3B = 0.D0
          END IF
          PHI1V1 = AVGPHI(I,J,PHI1,KEY1,KEY2A,KEY2B,KEY3A,KEY3B)
          PHI1V2 = AVGPHI(I,J,PHI2,KEY1,KEY2A,KEY2B,KEY3A,KEY3B)
          UINT = CHI1 * PHI1V1 + CHI2 * PHI1V2
          IF (I .EQ. 1) UINT = UINT + CHIS * L1
          UHARD(I,J) = U(ISTART+IMO*IRAD+J) - UINT
220      CONTINUE
          KEY1 = 1.D0
          KEY3A = 0.D0
          KEY3B = 1.D0
230      CONTINUE
      RETURN
      END

```

C

```

      SUBROUTINE ENERGY(U,ILAY,IRAD,ISEG_B,ISEG_P,PHIO,PHIB,
1      PHIP,DELS,DELU,DELA)

```

C This subroutine calculates the entropy change and Helmholtz
 C energy change based on the reference state of unmixed
 C components. The equations are derived from the statistical
 C mechanics of the lattice model. ("Polymers at Interfaces")

```

      IMPLICIT REAL*8 (A-H,O-Z)
      PARAMETER (MD=2000,MAXZ=50,MAXR=20)
      REAL*8 L, L1, L0, LR, LR0, LR1, KEY1, KEY2A, KEY2B, KEY3A, KEY3B
      COMMON/PARAMS/CHIBO,CHIBP,CHIBS,CHIPO,CHIPS,CHIOS,BRUSH,
1      PARTICL,NSEGS
      COMMON/POSITION/IPOS1,IPOS2,IPOS
      COMMON/INDEX/ISTAR1,ISTAR2,ISTAR3
      DIMENSION U(MD), PHIB(MAXZ,MAXR), PHIO(MAXZ,MAXR), L(MAXR),
1      PHIP(MAXZ,MAXR), LR(MAXR), LR0(MAXR), LR1(MAXR)

```

```

COMMON/STEPPROB/L1,L0,LR,LR0,LR1
COMMON/SITES/PI,L
COMMON/BULK/BULKO,BULKB,BULKP

C
C Calculation of the entropy part of the partition function.
C
SUM = 0.D0
ISTART = ISTAR1
DO 30 I = 1, ILAY
    IMO = I - 1
    DO 20 J = 1, IRAD
        SUM = SUM + L(J)*PHIO(I,J)*( LOG(BULKO) -
1          U(ISTART+IMO*IRAD+J) )
20    CONTINUE
30    CONTINUE
    IF ( BULKB .NE. 0.D0 ) THEN
        ISTART = ISTAR2
        DO 50 I = 1, ILAY
            IMO = I - 1
            DO 40 J = 1, IRAD
                SUM = SUM + L(J)*PHIB(I,J)*( LOG(BULKB)/ISEG_B -
1              U(ISTART+IMO*IRAD+J) )
40        CONTINUE
50        CONTINUE
    END IF
    IF ( BULKP .NE. 0.D0 ) THEN
        ISTART = ISTAR3
        DO 70 I = 1, ILAY
            IMO = I - 1
            DO 60 J = 1, IRAD
                SUM = SUM + L(J)*PHIP(I,J)*( LOG(BULKP)/ISEG_P -
1              U(ISTART+IMO*IRAD+J) )
60        CONTINUE
70        CONTINUE
    END IF
DELS = SUM

C
C Calculation of the energy part of the partition function.
C
TERM3 = 0.D0
KEY1 = 0.D0
KEY2A = 0.D0
KEY2B = 1.D0
KEY3A = 0.D0
KEY3B = 1.D0
DO 110 I = 1, ILAY
    IF (I .EQ. ILAY) THEN
        KEY2A = 1.D0
        KEY2B = 0.D0
    END IF
    DO 100 J = 1, IRAD
        IF (J .EQ. IRAD) THEN
            KEY3A = 1.D0
            KEY3B = 0.D0

```

```

      END IF
      PHIOAV = AVGPHI(I,J,PHIO,KEY1,KEY2A,KEY2B,KEY3A,KEY3B)
      PHIBAV = AVGPHI(I,J,PHIB,KEY1,KEY2A,KEY2B,KEY3A,KEY3B)
      PHIPAV = AVGPHI(I,J,PHIP,KEY1,KEY2A,KEY2B,KEY3A,KEY3B)
C
      SUM = CHIBO * PHIBAV
      SUM = SUM + CHIPO * PHIPAV
      IF ( I .EQ. 1 ) SUM = SUM + 2.D0 * CHIOS * L1
      TERM3 = TERM3 + L(J) * PHIO(I,J) * SUM
C
      SUM = CHIBO * PHIOAV
      SUM = SUM + CHIBP * PHIPAV
      IF ( I .EQ. 1 ) SUM = SUM + 2.D0 * CHIBS * L1
      TERM3 = TERM3 + L(J) * PHIB(I,J) * SUM
C
      SUM = CHIPO * PHIOAV
      SUM = SUM + CHIBP * PHIBAV
      IF ( I .EQ. 1 ) SUM = SUM + 2.D0 * CHIPS * L1
      TERM3 = TERM3 + L(J) * PHIP(I,J) * SUM
100  CONTINUE
      KEY1 = 1.D0
      KEY3A = 0.D0
      KEY3B = 1.D0
110  CONTINUE
      DELU = TERM3
      DELA = DELS + DELU
C
      RETURN
      END
C
*****
      DOUBLE PRECISION FUNCTION AVGPHI(I,J,PHI,KEY1,KEY2A,KEY2B,
1      KEY3A,KEY3B)
C      Calculates the layer average volume fraction for use in
C      energy calculations. Boundary conditions are handled by the
C      KEY values again.
*****
      IMPLICIT REAL*8(A-H,O-Z)
      PARAMETER(MAXZ=50,MAXR=20)
      REAL*8 L1, L0, LR, LR0, LR1, KEY1, KEY2A, KEY2B, KEY3A, KEY3B
      DIMENSION PHI(MAXZ,MAXR), LR(MAXR), LR0(MAXR), LR1(MAXR)
      COMMON/STEPPROB/L1,L0,LR,LR0,LR1
C
      IPO = I + 1
      IMO = I - 1
      JPO = J + 1
      JMO = J - 1
C
      AVGPHI = ((L1 * KEY1 * (LR(J) *
1      PHI(IMO,JMO) + (LR0(J) + KEY3A * LR1(J)) *
2      PHI(IMO,J) + LR1(J) * KEY3B * PHI(IMO,JPO))) +
3      ((L0 + KEY2A * L1) * (LR(J) * PHI(I,JMO) + (LR0(J)
4      + KEY3A * LR1(J)) * PHI(I,J) + LR1(J) * KEY3B *
5      PHI(I,JPO))) + (L1 * KEY2B * (LR(J) * PHI(IPO,JMO)

```

```

6      + (LR0(J) + KEY3A * LR1(J)) * PHI(IPO,J) + LR1(J) *
7      KEY3B * PHI(IPO,JPO)))
C
      RETURN
      END
C
*****
      SUBROUTINE OUTPUT(ILAY,IRAD,ISEG_B,ISEG_P,U,PHIB,PHIP,PHIO,
1          I_MIN,I_SEC,ITVAR,ENTR,ENGY,TOTENG)
C      Volume fractions, free segment potentials, and energy changes
C      based on particle position are printed to an output file.
C      The output format facilitates 3D plotting using Origin.
*****
      IMPLICIT REAL*8(A-H,O-Z)
      PARAMETER (MD=2000,MAXZ=50,MAXR=20)
      REAL*8 L
      DIMENSION U(MD), PHIB(MAXZ,MAXR), PHIP(MAXZ,MAXR), L(MAXR),
1          PHIO(MAXZ,MAXR), ENTR(MAXZ), ENGY(MAXZ), TOTENG(MAXZ)
      COMMON/PARAMS/CHIBO,CHIBP,CHIBS,CHIPO,CHIPS,CHIOS,BRUSH,
1          PARTICL,NSEGS
      COMMON/POSITION/IPOS1,IPOS2,IPOS
      COMMON/INDEX/ISTAR1,ISTAR2,ISTAR3
      COMMON/SITES/PI,L
      COMMON/BULK/BULKO,BULKB,BULKP
C
      WRITE(14,*)
      WRITE(14,'(2X,A39,I4)')
1      'VALUE FOR GRAFTED CHAIN LENGTH          ', ISEG_B
      WRITE(14,'(2X,A39,I4)')
1      'VALUE FOR PARTICLE CHAIN LENGTH          ', ISEG_P
      WRITE(14,'(2X,A39,I4)')
1      'VALUE FOR CYLINDRICAL LATTICE LENGTH      ', ILAY
      WRITE(14,'(2X,A39,I4)')
1      'VALUE FOR CYLINDER RADIUS                  ', IRAD
      WRITE(14,'(2X,A39,I4)')
1      'START POSITION FOR PARTICLE                  ', IPOS1
      WRITE(14,'(2X,A39,I4)')
1      'END POSITION FOR PARTICLE                    ', IPOS2
      WRITE(14,'(2X,A39,I4)')
1      'CENTER POSITION OF CENTER OF PARTICLE        ', IPOS
      WRITE(14,'(2X,A39,G12.4)')
1      'BRUSH-SOLVENT INTERACTION PARAMETER        ', CHIBO
      WRITE(14,'(2X,A39,G12.4)')
1      'BRUSH-SURFACE INTERACTION PARAMETER        ', CHIBS
      WRITE(14,'(2X,A39,G12.4)')
1      'BRUSH-PARTICLE INTERACTION PARAMETER        ', CHIBP
      WRITE(14,'(2X,A39,G12.4)')
1      'PARTICLE-SOLVENT INTERACTION PARAMETER      ', CHIPO
      WRITE(14,'(2X,A39,G12.4)')
1      'PARTICLE-SURFACE INTERACTION PARAMETER      ', CHIPS
      WRITE(14,'(2X,A39,G12.4)')
1      'NUMBER OF BRUSH MOLECULES IN LATTICE        ', BRUSH
      WRITE(14,'(2X,A39,G12.4)')
1      'NUMBER OF PARTICLE MOLECULES                ', PARTICL

```



```

        WRITE(14, '(2X,A39,I4)')
1      'NUMBER OF ITERATION VARIABLES'          ', ITVAR
C
        WRITE(14,*)
        WRITE(14,*) 'BRUSH DISTRIBUTION '
        WRITE(14,*) 'LAYER    RADIAL    VOLFRAC          POTENTIAL'
        ISTART = ISTAR2
        DO 50 I = 1, ILAY
            IMO = I - 1
            DO 30 J = IRAD, 1, -1
                WRITE(14,60) I, (ABS(J-1-IRAD)), PHIB(I,J),
1              U(ISTART+IMO*IRAD+J)
30      CONTINUE
            DO 40 J = 1, IRAD
                WRITE(14,60) I, (J+IRAD), PHIB(I,J),
1              U(ISTART+IMO*IRAD+J)
40      CONTINUE
50      CONTINUE
60      FORMAT(3X,I2,5X,I2,3X,G15.5,3X,G15.5)
        WRITE(14,*)
C
        WRITE(14,*) 'PARTICLE DISTRIBUTION (VOL FRAC)'
        WRITE(14,*) 'LAYER    RADIAL    VOLFRAC          POTENTIAL'
        ISTART = ISTAR3
        DO 80 I = 1, ILAY
            IMO = I - 1
            DO 70 J = IRAD, 1, -1
                WRITE(14,60) I, (ABS(J-1-IRAD)), PHIP(I,J),
1              U(ISTART+IMO*IRAD+J)
70      CONTINUE
            DO 75 J = 1, IRAD
                WRITE(14,60) I, (J+IRAD), PHIP(I,J),
1              U(ISTART+IMO*IRAD+J)
75      CONTINUE
80      CONTINUE
        WRITE(14,*)
C
        WRITE(14,*) 'SOLVENT DISTRIBUTION (VOL FRAC)'
        WRITE(14,*) 'LAYER    RADIAL    VOLFRAC          POTENTIAL'
        ISTART = ISTAR1
        DO 100 I = 1, ILAY
            IMO = I - 1
            DO 90 J = IRAD, 1, -1
                WRITE(14,60) I, (ABS(J-1-IRAD)), PHIO(I,J),
1              U(ISTART+IMO*IRAD+J)
90      CONTINUE
            DO 95 J = 1, IRAD
                WRITE(14,60) I, (J+IRAD), PHIO(I,J),
1              U(ISTART+IMO*IRAD+J)
95      CONTINUE
100     CONTINUE
        WRITE(14,*)
C
        WRITE(14,*)

```

```

WRITE(14,*) '          BULK (SOLV)          (BRUSH)          (PARTICLE) '
WRITE(14,110) IPOS,BULKO,BULKB,BULKP
C
WRITE(14,*)
WRITE(6,*)
WRITE(14,*) 'POSITION      (S-S*)/kT      (U-U*)/kT      (A-A*)/kT'
WRITE(6,*) 'POSITION      (S-S*)/kT      (U-U*)/kT      (A-A*)/kT'
DO I = IPOS2, IPOS, -1
    WRITE(14,110) I, ENTR(I), ENGY(I), TOTENG(I)
    WRITE(6,110) I, ENTR(I), ENGY(I), TOTENG(I)
END DO
WRITE(14,*)
WRITE(6,*)
WRITE(14,*) 'POSITION      dS(int)/kT      dU(int)/kT      dA(int)/kT'
WRITE(6,*) 'POSITION      dS(int)/kT      dU(int)/kT      dA(int)/kT'
DO I = IPOS2, IPOS, -1
    DENTR = ENTR(I) - ENTR(IPOS2)
    DENGY = ENGY(I) - ENGY(IPOS2)
    DTOT = TOTENG(I) - TOTENG(IPOS2)
    WRITE(14,110) I, DENTR, DENGY, DTOT
    WRITE(6,110) I, DENTR, DENGY, DTOT
END DO
110  FORMAT (I7,3(G15.6))
C
WRITE(14,120) I_MIN, I_SEC
WRITE(6,120) I_MIN, I_SEC
120  FORMAT ('          CPU time:',I6,1H:',I2,9H [min:s] )
C
RETURN
END
C
*****
SUBROUTINE MATINV(A,N,AINV,IERROR)
C  Matrix inversion subroutine, using partial pivoting.
*****
IMPLICIT REAL*8 (A-H,O-Z)
PARAMETER (MD=2000)
INTEGER PIVOT
DIMENSION A(MD,MD), AINV(MD,MD), B(MD), PIVOT(MD),
1      QUOT(MD,MD)
C
C  WRITE(6,*) 'IN MATINV'
NMO = N - 1
IERROR = 0
C
C  Carry out standard Gauss elimination with partial pivoting
C
DO 50 K = 1, NMO
    KPO = K + 1
    BIGGEST = DABS(A(K,K))
    PIVOT(K) = K
    DO 10 I = KPO, N
        AIK = DABS(A(I,K))
        IF (AIK .GT. BIGGEST) THEN

```

```

        BIGGEST = AIK
        PIVOT(K) = I
    END IF
10    CONTINUE
    IF (PIVOT(K) .NE. K) THEN
        DO 20 J = K, N
            TEMP = A(PIVOT(K), J)
            A(PIVOT(K), J) = A(K, J)
            A(K, J) = TEMP
20    CONTINUE
    END IF
    IF (A(K, K) .EQ. 0.D0) THEN
        IERROR = 1                ! ZERO PIVOT FOUND
        RETURN
    END IF
    DO 40 I = KPO, N
        QUOT(I, K) = A(I, K) / A(K, K)
        A(I, K) = 0.D0
        DO 30 J = KPO, N
            A(I, J) = A(I, J) - QUOT(I, K) * A(K, J)
30    CONTINUE
40    CONTINUE
50    CONTINUE
    IF (A(N, N) .EQ. 0.D0) THEN
        IERROR = 1                ! ZERO PIVOT FOUND
        RETURN
    END IF

C
C    Carry out the elimination process as above, and then back
C    substitution to determine the elements of the inverse matrix.
C

    DO 90 L = 1, N
        DO 60 I = 1, N
            B(I) = 0.D0
60    CONTINUE
        B(L) = 1.D0
        DO 70 K = 1, NMO
            IF (PIVOT(K) .NE. K) THEN
                TEMP = B(PIVOT(K))
                B(PIVOT(K)) = B(K)
                B(K) = TEMP
            END IF
            DO 65 I = K+1, N
                B(I) = B(I) - QUOT(I, K) * B(K)
65    CONTINUE
70    CONTINUE
        AINV(N, L) = B(N) / A(N, N)
        DO 80 I = NMO, 1, -1
            SUM = 0.D0
            DO 75 J = I+1, N
                SUM = SUM + A(I, J) * AINV(J, L)
75    CONTINUE
            AINV(I, L) = (B(I) - SUM) / A(I, I)
80    CONTINUE

```

```

90    CONTINUE
      RETURN
      END

C
*****
      REAL*8 FUNCTION  F_TIME( )
C      This function returns the CPU time in seconds.
*****
      IMPLICIT REAL*8 (A-H,O-Z)
      INTEGER*2 hour, minute, second, hundredth
      CALL GETTIM( hour, minute, second, hundredth )
      F_TIME = ((DBLE( hour ) * 3600.) + (DBLE( minute) * 60.) +
1          DBLE( second) + (DBLE( hundredth ) / 100.))
      RETURN
      END

```